Altered brain high-energy phosphate metabolism in mild Alzheimer's disease: A 3-dimensional 31P MR spectroscopic imaging study

Anne Rijpma,1*, Marinette van der Graaf,1, Olga Meulenbroek,2,3, Marcel G.M. Olde Rikkert,2,3, Arend Heerschap,4

1. Introduction

Alzheimer’s disease (AD) is the main cause of dementia in the elderly, responsible for about half of the nearly 47 million dementia cases worldwide (Report, 2015). Although the disease is defined by the accumulation of amyloid beta plaques and neurofibrillary tangle tangles in the brain (Braak and Braak, 1991), other pathological processes can be identified such as oxidative stress, vascular dysfunction, and inflammation (Akiyama et al., 2000; de la Torre, 2004; Marksbery, 1997). Additionally, defects in essential metabolic processes for energy supply and membrane function have been implicated in AD (Lynn et al., 2010; Nitsch et al., 1992).

The human brain is highly vulnerable to disturbances in energy metabolism, due to its relatively large energy consumption. Previous AD studies demonstrated alterations in global and cellular energy metabolism. FDG-PET studies have shown glucose hypometabolism in the retrosplenial cortex (RSC) and medial temporal lobe in people with mild cognitive impairment (MCI) and AD patients, as well as in cognitively normal carriers of the APOE ε4 allele (Nestor et al., 2003; Pietrini et al., 2000; Reiman et al., 2001; Reiman et al., 2005). Furthermore, the enzyme creatine kinase (CK), obtained from post-mortem AD tissue, shows reduced activity compared with samples that are free from neurological disease (Aksenov et al., 2000; David et al., 1998). The CK reaction, key to balance brain energy metabolism, can quickly replenish adenosine triphosphate (ATP) from the energy buffer phosphocreatine (PCr), when local energy demands suddenly increase. This reaction also enhances the efficiency of mitochondrial oxidative phosphorylation (OXPHOS) by keeping adenosine diphosphate (ADP) sufficiently available (Schlattner et al., 2006) and prevents acidification by maintaining pH for a review see

Abbreviations: 1H, proton; 31P-MRS, phosphorus magnetic resonance spectroscopy; AC, anterior commissure; ACC, anterior cingulate cortex; AD, Alzheimer’s disease; ADP, adenosine diphosphate; ATP, adenosine triphosphate; CK, creatine kinase; Cr, creatine; CSF, cerebrospinal fluid; GM, grey matter; GPEth, glycerophosphoethanolamine; HL, left hippocampus; HR, right hippocampus; LS, least square; MCI, mild cognitive impairment; MMSE, Mini Mental State Examination; MRSI, magnetic resonance spectroscopic imaging; NADH, nicotinamide adenine dinucleotide; OXPHOS, oxidative phosphorylation; PC, posterior commissure; PCh, phosphocholine; PCr, phosphocreatine; PDE, phosphodiesterase; PETH, phosphoethanolamine; Pi, inorganic phosphate; PME, phosphomonoester; ROI, region of interest; RSC, retrosplenial cortex; WM, white matter

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One of the earliest pathological changes in AD is synaptic dys-function, which correlates well with cognitive dysfunction and disease severity (Terry et al., 1991). Alterations in neuronal membrane composition, vital for synaptic transmission, have been linked to synaptic dysfunction in AD (Pomponi et al., 2008). For instance, post mortem studies found reduced levels of the major membrane components phosphatidylcholine, phosphatidylethanolamine and phosphatidylino-sitol (Nitsch et al., 1992; Pettigrew et al., 2001), as well as altered activity of catabolic and anabolic enzymes, suggesting compensatory metabolic changes to reduce the rate of neuronal membrane loss (Ross et al., 1998).

High energy phosphates, such as ATP and PCr, and metabolites of phospholipid membrane metabolism can be assessed in vivo by phos-phorus magnetic resonance spectroscopy (31P-MRS). This technique has been applied in AD (e.g. Forlenza et al., 2002; Mandal et al., 2012; Pettigrew et al., 1994; Smith et al., 1995), but previous studies, essentially focusing on single brain regions, were severely hampered by small sample sizes and low spectral resolution, resulting in a wide disparity in findings. Furthermore, differences in the control groups that were used, in the brain regions that were studied and in the disease stages and medication statuses of the patients, may have contributed to apparent inconsistencies in the literature.

The aim of the current study was to investigate whether abnormal phospholipid and energy metabolism can be detected non-invasively in early stage AD patients by 31P MR spectroscopic imaging (31P-MRS). This investigation was designed to overcome the limitations of previous studies. First, we performed the measurements at 3 T field strength with a dual-tuned 1H/31P volume head coil (Rapid Biomedical, Wuerzburg, Germany). High resolution MR images were acquired with a T1-weighted magnetisation-prepared rapid gradient-echo sequence (TR = 2300 ms, TE = 3.16 ms, TI = 1100 ms, 15° flip-angle, 176 sagittal slices, slice-matrix size = 256 × 256 mm, slice thickness = 1 mm, voxel-size = 1 × 1 × 1 mm, TA = 6:25 min).

31P-MR spectra were acquired with whole brain 3D MRSI (a pulse-acquire sequence with 40° flip-angle, acquisition delay of 0.7 ms in including 0.3-ms gradient phase encoding time, 512 ms acquisition duration with WALTZ41H decoupling during the first 256 ms with γB1 = 250 Hz ensuring (γ/2B1) 2 > (JPH)2, TR = 2000 ms, FOV 260 × 260 × 260 mm; matrix size = 10 × 10 × 10, acquisition time 13:08 min). Prior to acquisition, an automatic procedure was applied to optimize the magnetic field homogeneity of a rectangular shim volume maximizing brain coverage while bound by the skull. Subsequently, if necessary, the field homogeneity was further adjusted manually until a value of < 25 Hz was obtained for the full width at half maximum of the absolute-value 1H MR water signal. K-space was sampled with a weighted elliptical phase-encoding scheme with four averages. The volume of interest was centered on the midline and parallel to the line from the anterior commissure to the posterior commissure. Spatial post-processing consisted of zerofilling to a matrix size of 16 × 16 × 16. The nominal volume of the measured voxels is about 17.5 cm3, the effective voxel at 64% of the spatial response function has a spherical shape with a volume of about 40 cm3 (Pohmann and von Kienlin, 2001).

2.2. MR acquisition

MRI and MRS were performed on a Magnetom Tim Trio 3T MR system (Siemens, Erlangen, Germany) with a dual-tuned 1H/31P volume head coil. High resolution MR images were acquired with a T1-weighted magnetisation-prepared rapid gradient-echo sequence (TR = 2300 ms, TE = 3.16 ms, TI = 1100 ms, 15° flip-angle, 176 sagittal slices, slice-matrix size = 256 × 256 mm, slice thickness = 1 mm, voxel-size = 1 × 1 × 1 mm, TA = 6:25 min).

2.3. MRS and MRI data analyses

Four regions of interest (ROI) were selected for analysis from the 3D 31P-MRSI data: ACC, RSC, and left and right hippocampus (HL and HR). Guided by the T1-weighted images, the MRSI grid was shifted in the x, y and z dimension to position voxels in the ROIs (by AR; Fig. 1). For the ACC, a voxel was selected anterior to the genu of the corpus callosum, with the inferior border aligned with the line from the anterior commissure to the posterior commissure (AC-PC line), and on the mid-sagittal plane. For the RSC, a voxel on the mid-sagittal plane was selected posterior to the splenium of the corpus callosum, with the inferior border aligned with the AC-PC line. For the HL and HR, a voxel was selected at the anterior end of each hippocampus, with the inferior and lateral border of the voxel aligned with the inferior and lateral side of the hippocampus.

The software package Metabolite Report (Siemens Healthcare, Erlangen, Germany) was used for post-processing (i.e. 100 ms exponential filter, zero-filling, phase correction, baseline correction) and for automatic fitting of the spectra in the time-domain using prior knowledge appropriate for 31P MR spectra (own spectral data and from de Graaf (2008)). Eleven well-resolved resonance peaks were fitted: the phospholipid metabolites phosphoethanolamine (PEth), phosphocho-line (PCh), glycerophosphoethanolamine (GPEth) and glycerophospho-sphingophosphocholine (GPCh), the high-energy phosphorus molecules PCr, ATP (α-ATP, β-ATP and γ-ATP), nicotinamide adenine dinucleotide (NAD (H)) and inorganic phosphate (Pi), and membrane-bound phospholipid (details of this procedure are described in the Appendix).

Both a quantitative evaluation of the fitting results and a visual quality control were performed. Quantitatively, only metabolite fits
with a Cramer–Rao lower bound of $\leq 30\%$ were considered reliable. Qualitatively, two MR spectroscopists (AR and MvdG) independently checked the spectra by visual inspection of the original spectra and the fitting results. If a metabolite peak was visually present, and its fit was assigned to the correct resonance—giving a minimal residue in the subtraction spectrum—the fitting result was accepted.

The integral of each metabolite resonance was expressed as a percent area of the total phosphorous signal in the corresponding spectrum. Hereby, the data were normalized, and corrected for cerebrospinal fluid (CSF) content and thus for differences in local atrophy. Phosphomonoesters (PME) and phosphodiesters (PDE) from GPEth and GPCh and total ATP (tATP) from the sum of $\alpha$-ATP, $\beta$-ATP and $\gamma$-ATP. In addition, the ratios PME/PDE, PE/GPE, PC/GPC and PCr/Pi were computed. Intracellular pH was determined from the chemical shift difference between the PCr and Pi resonance peaks (Petroff et al., 1985).

The T$_1$-weighted images were segmented into grey matter (GM), white matter (WM) and CSF using automatic segmentation software (by AR; SPm8, Welcome Trust Centre for Neuroimaging, London, UK; VBM8, Structural Brain Mapping Group, Jena, USA). Binary tissue maps (matrices) of GM, WM, CSF were convolved with the, digitally sampled, mathematically-modelled three dimensional point-spread function of the MRSI, using Matlab 2012b (The Mathworks, Inc., Natick, MA), to obtain theoretically correct values of the contribution of tissue type to each ROI (each consisting of one MRS voxel). GM-to-WM ratio (GM/WM) was calculated for each ROI for each subject.

### 2.4. Statistical analyses

Two-factorial mixed ANOVAs were used to test differences in tissue content (GM, WM, and CSF) and GM/WM in each ROI between mild AD patients and controls. Group and brain region (ROI) differences were analyzed for each spectroscopy outcome parameter using a mixed model with group (AD or control), sex, brain region and its interaction with group as fixed factors, considering brain region as a within subject factor, and adjusting for age. An unstructured variance-covariance matrix for brain region was selected. The group-by-brain region interaction was only kept in the model if $p < 0.10$. In the covariate analysis, GM/WM in each ROI was added to the final primary model of each parameter, to investigate the effect of tissue composition on the effects of group and brain region. Although the inclusion of GM/WM in the final model led to a small change (10–20%) in many parameter estimates, this was mainly without a change in main and/or interaction effects. Therefore we report the primary model in tables and figures and refer to the effect of GM/WM only where it led to a change in the main and/or interaction effects, and with $> 20\%$ change in the parameter estimates of group or brain region. Goodness of fit was assessed by comparing Bayesian Information Criteria (BIC) and homoscedasticity and normality of residuals were assessed by visual inspection. Statistical analyses were performed using SAS 9.2 Software for Windows (SAS Institute Inc., Cary, NC, USA). Statistical significance was set at $p < 0.05$ without correction for multiple testing.

### 3. Results

#### 3.1. Subjects
A total of 33 mild AD patients and 35 healthy control subjects were enrolled in the study and subjected to MRI and MRS measurements. Two AD patients had MR spectra of low quality (due to severe motion and a dental implant) and four control subjects were found to meet an exclusion criterion during or after the visit (two subjects took nutritional supplements, two subjects presented with structural neurological damage from ischemic infarcts and trauma). Therefore, 31 AD patients and 30 controls were included in the final analysis. The groups were similar with respect to age and gender (see Table 1 for subject characteristics).

#### 3.2. ROI tissue contribution
The interaction between group and brain region for GM and CSF contributions to the total volume of each ROI was not significant, but GM and CSF differed significantly between groups, and between brain regions (all $p < 0.001$). GM was lower and CSF was higher in AD patients than in healthy control subjects (mean $% \pm SD$, GM:36.3 $\pm$ 4.7 vs. 40.5 $\pm$ 4.0; CSF: 22.5 $\pm$ 4.7 vs. 18.1 $\pm$ 3.5). Overall, GM was highest in the right hippocampus, followed by left hippocampus, and then followed by equal amounts in RSC and ACC (data not shown). CSF in RSC and ACC was higher than in both hippocampi. There was a significant interaction between group and brain region for WM.
### 3.6. Differences in phosphorus metabolites and pH between brain regions

Brain region significantly affected all outcome parameters (all \( p < 0.05 \), except PCh and PME (\( p > 0.05 \)). The normalized signals of total ATP, \( \alpha \)ATP, \( \beta \)ATP, \( \gamma \)ATP, NAD(H), PEth, GPEtn, GPCh, and PDE were lower in the RSC than in the ACC and both hippocampi (all \( p < 0.05 \)), while the pattern was reversed for the ratios PCh/GPCh and PME/PDE (\( p < 0.001 \)). We found no difference between the left and right hippocampus for any of the energy and phospholipid metabolites or pH (\( p > 0.05 \)), except for \( \alpha \)ATP (LS mean difference = 0.65, SEM = 0.26, \( p = 0.015 \)). See Table 3 for an overview of the differences between brain regions.

### 3.7. Influence of tissue content

In the covariate analysis GM/WM was added to the final model. This did not change the effects of group, brain region or the interaction between group and brain region on PCr, Pi, total ATP, \( \alpha \)ATP, \( \beta \)ATP, \( \gamma \)ATP, NAD(H), pH or any of the phospholipid metabolite signals. However, for PCr/Pi the main effect of brain region was reduced to a trend (\( p = 0.062 \)) and the parameter estimates changed substantially, when GM/WM was included in the model. There was no change in the effect of group on PCr/Pi.

### 4. Discussion

In this study we acquired high-quality \( ^{31} \)P-MRSI data of the brain in a large group of mild AD patients and in a well-matched healthy elderly population. High spectral resolution enabled us to gather information on high-energy phosphates, as well as on specific phospholipid metabolites. MR spectra of the four brain regions that are among the most studied in AD were investigated and for the first time, these areas were measured simultaneously by \( ^{31} \)P-MRSI. We detected increased phosphocreatine and pH, but no changes in phospholipid metabolite signals in mild AD patients. Interestingly, the increase in Pcr was observed in the RSC and in the hippocampi, regions that both show early pathological changes in AD, but not in the ACC, a region known to be involved in the disease at a later stage. This suggests that the Pcr abnormality expands across brain regions in a similar fashion as other AD pathologies, such as tau (Braak and Braak, 1991). Furthermore, in both groups pH, high energy phosphates, and most phospholipid metabolites differed across brain regions.

As in vivo human \( ^{31} \)P MRS brain studies are nearly always performed under signal saturating conditions, changes in T1 relaxation time may affect metabolite signal intensities (Longo et al., 1993). Although we cannot exclude that such an effect has contributed to the increased Pcr signal, it would require a rather drastic decrease in Pcr's T1 value from about 3 to 2 s. Moreover, no increases in PME and PDE signals were detected, while those would be affected more severely by a T1 decrease (Klomp et al., 2008). A potential cause for relaxation enhancement is a higher brain iron accumulation in AD patients (Tao et al., 2014), but this would increase the signal linewidth, which was not observed. Thus, the most likely explanation for the increased Pcr signal is a higher tissue concentration of this compound.

Elevated Pcr signals have been reported before for AD patients in comparison with young controls (Mandal et al., 2012), but as Pcr also increases with age in healthy persons (Chiu et al., 2015; Forester et al., 2010; Longo et al., 1993) it is unclear whether this finding was due to an aging effect. The current results showed increased Pcr, and Pcr/Pi, in AD patients compared with elderly controls of the same age. In contrast, two earlier studies showed a decrease in prefrontal Pcr in mild, but not severe, AD (Pettegrew et al., 1994) and decreased Pcr/Pi in the frontal lobe (Smith et al., 1995). However, these studies were performed at 1.5T with only surface coil localization and involved small sample sizes.

As the concentration of high energy phosphates depends on the

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**Table 1**

<table>
<thead>
<tr>
<th></th>
<th>AD n = 31</th>
<th>Controls n = 31</th>
</tr>
</thead>
<tbody>
<tr>
<td>Age (years)</td>
<td>73.4 (6.8)</td>
<td>73.5 (6.3)</td>
</tr>
<tr>
<td>Gender (%)</td>
<td>13 males (42%)</td>
<td>15 males (48%)</td>
</tr>
<tr>
<td>MMSE</td>
<td>23.2 (2.0)</td>
<td>28.1 (1.4)</td>
</tr>
<tr>
<td>Time since AD diagnosis</td>
<td>1.6 months [0.2–15.3]</td>
<td>–</td>
</tr>
<tr>
<td>BMI</td>
<td>25.4 kg/m² (3.8)</td>
<td>26.3 kg/m² (4.5)</td>
</tr>
<tr>
<td>Smoking (never/past/current)</td>
<td>13/17/1</td>
<td>6/22/3</td>
</tr>
<tr>
<td></td>
<td>≤1 relatives with AD (n)</td>
<td>19</td>
</tr>
</tbody>
</table>

MMSE, mini mental state examination; AD, Alzheimer’s disease; BMI, body mass index. Data are presented as mean (standard deviation) or median [range] unless otherwise indicated.

(p = 0.004) and GM/WM (p = 0.021). WM was higher in AD patients compared with controls in the right hippocampus (41.5 ± 3.0 vs. 40.0 ± 2.6), but not in the other brain regions. GM/WM was lower in AD patients than in controls in ACC, and both hippocampi, but not in RSC (data not shown).

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**3.4. Differences in energy metabolites and pH between groups**

A significant interaction between group and brain region was found for Pcr, showing that normalized Pcr signals were higher in mild AD patients compared with healthy control subjects in the RSC (Least Square (LS) mean difference = 0.86, SEM = 0.29, \( p = 0.004 \)), HL (LS mean difference = 1.52, SEM = 0.52, \( p = 0.005 \)) and HR (LS mean difference = 1.47, SEM = 0.38, \( p < 0.001 \)), but not in the ACC (\( p = 0.947 \)) (Fig. 3A). The interaction between group and brain region was not significant for \( \gamma \)ATP and \( \beta \)ATP. A main effect of group was found for Pcr/Pi, showing that this ratio was higher in mild AD patients compared with controls (LS mean difference = 0.22, SEM = 0.11, \( p = 0.046 \)) (Fig. 3B). Also pH was increased in AD patients compared with controls (LS mean difference = 0.008, SEM = 0.004, \( p = 0.032 \)) (Fig. 3C). No group differences were found for \( \gamma \)ATP, \( \beta \)ATP, \( \alpha \)ATP, total ATP, Pi, and NAD(H) (all \( p > 0.05 \)). For a summary of group effects see Table 2.

**3.5. Differences in phospholipid metabolites between groups**

No interaction or group difference between mild AD patients and healthy control subjects were found for any of the phospholipid metabolites (PEth, PCh, GPEtn, GPCh, PME, and PDE; Table 2) or their ratios (PEth/GPEtn, PCh/GPCh, and PME/PDE) (all \( p > 0.05 \)).

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**Table 2**

<table>
<thead>
<tr>
<th></th>
<th>AD n = 31</th>
<th>Controls n = 31</th>
</tr>
</thead>
<tbody>
<tr>
<td>Smoking (never/past/current)</td>
<td>13/17/1</td>
<td>6/22/3</td>
</tr>
<tr>
<td></td>
<td>≤1 relatives with AD (n)</td>
<td>19</td>
</tr>
</tbody>
</table>

### References

Chiu et al., 2015; Forester et al., 2010; Longo et al., 1993; Smith et al., 1995.
balance between energy production and energy utilization, increases in steady state PCr levels and PCr/Pi reflect a redistribution in the content of metabolites involved in the connected CK and ATPase pseudo-equilibria (Du et al., 2007). This may be the consequence of reduced utilization of ATP (Forester et al., 2010), caused by synaptic dysfunction or loss of other energy requiring functionalities (Chandrasekaran et al., 1996; Rapoport et al., 1996). Although these changes are expected to lower ATP production and thus PCr, the final balance between reduced energy production and consumption may still result in a higher PCr level. To maintain equilibrium, the increased PCr should be accompanied by changes in the levels of other substrates of the CK reaction, such as a higher ATP concentration. Previous studies reported an increase in (γ)ATP (Mandal et al., 2012; Mecheri et al., 1997; Pettegrew et al., 1994), although no alterations in ATP levels were found in the current nor in several other studies (e.g. Forlenza et al., 2002; Gonzalez et al., 1996; Smith et al., 1995). Alternatively, a higher PCr may result from an increased total amount of cellular creatine (Cr). However, in vivo measurements of total Cr content in MCI and AD patients provide no clear evidence that Cr is increased in the disease (Graff-Radford and Kantarci, 2013; Tumati et al., 2013). Finally, decreases in ADP and/or H⁺ concentration may accompany the PCr increase. Indeed, a slight increase in pH was detected in mild AD patients, but it does not fully compensate for the increase in PCr when equilibrium is assumed. Changes in PCr levels have also been associated with decreased CK activity in the AD brain (Forester et al., 2010; Mandal et al., 2012). However, it is unlikely to be a direct effect of this decrease as even in cytosolic CK knockout mice the remaining CK activity (< 20%) is sufficient to preserve equilibrium (in ’t Zandt et al., 2004). Clearly, a strongly affected reaction rate will affect processes that require rapid (local) energy supply, and a higher PCr level may represent a flux adaptation to this condition.

There is some evidence for involvement of PCr in processes beyond the PCr-CK system. Since glutamate uptake by synaptic vesicles is stimulated by PCr, independent of ATP or CK (Xu et al., 1996), increased PCr may prevent glutamate excitotoxicity (Bender et al., 2005). Furthermore, PCr may be able to bind to and stabilize phospholipid membranes (Tokarska-Schlattner et al., 2005) and may function as an osmolyte (Bothwell et al., 2001) and a neurotransmitter (Almeida et al., 2006). In addition, differences in metabolite levels may be explained by variations in tissue and cell type (Griffin et al., 2002; Urenjak et al., 1993), although our results remained unchanged when adjusting for grey and white matter. A prominent neuropathological feature in AD is astrogliosis (Osborn et al., 2016). As this alters the neuron-to-glia ratio within grey and white matter (Beach et al., 1989), it is possible that morphological differences between AD patients and healthy aged controls play a role in the alterations in PCr and pH. Furthermore, atrophy may introduce slight differences in the brain area that the measured volumes encompass, which effect may not be entirely captured by

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**Fig. 2.** Representative spectra from the anterior cingulate cortex (ACC), retrosplenial cortex (RSC), left hippocampus (HL) and right hippocampus (HR) of an Alzheimer’s disease patient (73 years old). Zero filling to 4096 data points and an 8 Hz Gaussian filter were applied for display purposes. PEth, phosphoethanolamine; PCh, phosphocholine; Pi, inorganic phosphate; GPEth, glycerophosphoethanolamine; GPCh, glycerophosphocholine; MP, membrane phospholipids; PCr, Phosphocreatine; ATP, adenosine triphosphate; NAD(H), nicotinamide adenine dinucleotide; ppm, parts per million.
adjusting for grey and white matter. However, ROIs were placed such that volume of the actual area of interest was maximized and the measured signals are dominated by the reported brain regions of interest.

Contrary to our expectation, we did not observe differences between mild AD patients and controls in any of the phospholipid metabolites, although preclinical and post-mortem studies show alterations in membrane function and lipid composition in AD (Nitsch et al., 1992; Ross et al., 1998). No previous in vivo studies have reported on PEth, although preclinical and post-mortem studies show alterations in mild AD patients and controls in any of the phospholipid metabolites, nor total PME. However, changes in the complex phospholipid cycle may be too small at this disease stage to be detected.

The current study only reports on relative metabolite levels, as obtaining absolute quantifications requires several assumptions, which adds complexity and reduces reliability. Moreover, when the variation in atrophy between and within groups is large, relative measurements are preferred over absolute. A second limitation may be that our results indicate that the investigated regions are metabolically different from each other. It also underlines that regional differences should be taken into account in any cross-sectional or longitudinal metabolic study. Moreover, as shown here for PCr, changes in metabolite levels in disease may not be the same for all brain regions.

MRSI revealed that high energy phosphates, pH and most phospholipid metabolites vary extensively across brain regions that are of interest in AD. These differences existed in both mild AD patients and controls, and were not explained by regional variation in grey and white matter content, with the ratio PCr/Pi as the sole exception. This indicates that the investigated regions are metabolically different from each other. It also underlines that regional differences should be taken into account in any cross-sectional or longitudinal metabolic study. Moreover, as shown here for PCr, changes in metabolite levels in disease may not be the same for all brain regions.

The current study only reports on relative metabolite levels, as obtaining absolute quantifications requires several assumptions, which adds complexity and reduces reliability. Moreover, when the variation in atrophy between and within groups is large, relative measurements are preferred over absolute. A second limitation may be that our results have not been corrected for multiple testing, because of the exploratory nature of this study. Replication of these results in an independent population would strengthen our findings. In future research it would be valuable to include preclinical AD patients or an at-risk population to clarify the disease stage in which abnormalities in PCr and pH appear, as well as perform longitudinal (intervention) studies to follow these abnormalities. In addition, magnetization transfer experiments to determine the CK and ATPase reaction rates with measurements of absolute concentrations of PCr and ATP to determine fluxes (Du et al., 2007), would elucidate whether the dynamics of the PCr-CK and ATP-ases systems are affected in AD.

14. Conclusion

To the best of our knowledge, this is the largest study to date investigating brain phospholipid and energy metabolism in AD by 31P MRS. Increased PCr levels were found in regions that show early degeneration in AD, but not in the ACC, a region known to be involved in this disease at a later stage. Together with an increased pH, this indicates that energy metabolism is altered in mild AD. Although most

### Table 2

Main effect of group (healthy controls vs Alzheimer’s disease) on phosphorus metabolite signals and tissue pH for all investigated regions.

<table>
<thead>
<tr>
<th></th>
<th>AD</th>
<th>Control</th>
<th>p-Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>PCr*</td>
<td>19.04 ± 0.18</td>
<td>18.08 ± 0.18</td>
<td>&lt; 0.001</td>
</tr>
<tr>
<td>n = 124</td>
<td>n = 124</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Pi</td>
<td>5.30 ± 0.11</td>
<td>5.47 ± 0.11</td>
<td>0.240</td>
</tr>
<tr>
<td>n = 121</td>
<td>n = 123</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PCr/Pi</td>
<td>3.71 ± 0.09</td>
<td>3.49 ± 0.09</td>
<td>0.046</td>
</tr>
<tr>
<td>n = 121</td>
<td>n = 123</td>
<td></td>
<td></td>
</tr>
<tr>
<td>total ATP</td>
<td>42.88 ± 0.27</td>
<td>43.17 ± 0.27</td>
<td>0.445</td>
</tr>
<tr>
<td>n = 124</td>
<td>n = 124</td>
<td></td>
<td></td>
</tr>
<tr>
<td>NAD(H)</td>
<td>3.96 ± 0.11</td>
<td>4.09 ± 0.11</td>
<td>0.388</td>
</tr>
<tr>
<td>n = 103</td>
<td>n = 96</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PEth</td>
<td>8.19 ± 0.11</td>
<td>8.33 ± 0.11</td>
<td>0.375</td>
</tr>
<tr>
<td>n = 119</td>
<td>n = 122</td>
<td></td>
<td></td>
</tr>
<tr>
<td>PCh</td>
<td>3.90 ± 0.07</td>
<td>3.93 ± 0.07</td>
<td>0.757</td>
</tr>
<tr>
<td>n = 112</td>
<td>n = 114</td>
<td></td>
<td></td>
</tr>
<tr>
<td>GPEth</td>
<td>4.32 ± 0.11</td>
<td>4.31 ± 0.11</td>
<td>0.942</td>
</tr>
<tr>
<td>n = 109</td>
<td>n = 117</td>
<td></td>
<td></td>
</tr>
<tr>
<td>GPCh</td>
<td>5.96 ± 0.15</td>
<td>6.08 ± 0.15</td>
<td>0.526</td>
</tr>
<tr>
<td>n = 108</td>
<td>n = 109</td>
<td></td>
<td></td>
</tr>
<tr>
<td>pH</td>
<td>7.037 ± 0.003</td>
<td>7.028 ± 0.003</td>
<td>0.032</td>
</tr>
<tr>
<td>n = 121</td>
<td>n = 123</td>
<td></td>
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LS means ± SEM of metabolite levels, as percentage of total phosphorus signal in the corresponding spectrum, in patients with Alzheimer’s disease and healthy control subjects. Significant group effects (p < 0.05, AD versus Control) indicated in bold. *PCr also has a significant interaction between group and brain region. LS, least squares; SEM, standard error of the mean; n, number of observations; AD, Alzheimer’s disease; HC, healthy control; PCr, Phosphocreatine; Pi, inorganic phosphate; ATP, adenosine triphosphate; NAD(H), nicotinamide adenine dinucleotide; PEth, phosphoethanolamine; PCh, phosphocholine; GPEth, glycerophosphoethanolamine; GPCh, glycerophosphocholine.
phospholipid metabolites, like the high energy phosphates, differed between the investigated brain regions in both groups, no alterations in phospholipid metabolism were found specific to mild AD.

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Declaration of interest

Conflicts of interest: none

Appendix A. Supplementary data

Supplementary data to this article can be found online at https://doi.org/10.1016/j.nicl.2018.01.031.

References


