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White matter integrity in small vessel disease is related to cognition

Anil M. Tuladhara, Anouk G.W. van Norden, Karlijn F. de Laat, Marcel P. Zwiers, Ewoud J. van Dijk, David G. Norris, Frank-Erik de Leeuw

1. Introduction

Cerebral small vessel disease (SVD) manifests on conventional MR images (i.e., T1 and Fluid Attenuated Inversion Recovery (FLAIR)) as white matter hyperintensities (WMH) and lacunes of presumed vascular origin (Wardlaw et al., 2013). These SVD markers are commonly observed in the elderly population. SVD is related to cognitive impairment and may, in some, ultimately lead to dementia (de Groot et al., 2000; Vermeer et al., 2003). This is supposedly due to the disruption of important white matter (WM) tracts. Despite the high prevalence of SVD (de Leeuw et al., 2001; Vernooij et al., 2007), relatively few develop evident cognitive decline or dementia (Vermeer et al., 2003). Other factors, apart from WMH and lacunes, presumably play a role in the transition from relative intact cognitive performance to severe cognitive decline in these few individuals. One of these factors could be the (loss of) microstructural integrity of the largest part of the WM; the on FLAIR imaging normal-appearing white matter (NAWM) surrounding the SVD. Pathological studies have demonstrated loss of microstructural integrity in the NAWM (Grafton et al., 1991) that cannot be visualized with conventional imaging, but can be investigated with diffusion tensor imaging (DTI).

DTI provides information on the microstructural integrity of the WM. DTI measures the local water diffusion profiles by: fractional anisotropy (FA), which represents a normalized ratio of diffusion directionality; mean diffusivity (MD), which reflects the overall magnitude of water diffusion; and axial diffusivity (AD), which reflects the diffusivity parallel to the WM tracts and radial diffusivity (RD), which is the diffusivity perpendicular to these tracts (Pierpaoli et al., 1996). Loss of
microstructural integrity is typically reflected by a reduction in FA and/or an increase in MD (Sen and Basser, 2005); the latter can result from different combinations of changes in AD and RD. Few studies in patients with cerebral SVD demonstrated a relation between higher MD and lower FA and loss of cognitive function (Della Nave et al., 2007; Nikkunan et al., 2008; O’Sullivan et al., 2001b; O’Sullivan et al., 2004; Xu et al., 2010). These studies had, however, small sample sizes and were not able to properly adjust for possible confounders. One large population-based cohort study demonstrated relation between microstructural integrity of both WMH and NAWM and cognitive function. However, the regional differences of microstructural integrity were not taken into account (Vernooij et al., 2009).

We hypothesized that cognitive performance in subjects with SVD would not only be related to loss of WM microstructural integrity within the WMH, but also to specific areas within the NAWM. We conducted DTI using tract-based spatial statistics (TBSS) analyses to investigate the location of microstructural WM loss related to cognitive disturbances. Also, additional adjustments for the WMH and lacunes were made to examine whether the associations in the WM were primarily explained by the typical manifestations of SVD on conventional MRI.

2. Methods and materials

2.1. Study population

The Radboud University Nijmegen Diffusion tensor and Magnetic resonance imaging Cohort (RUN DMC) study prospectively investigates the risk factors and clinical consequences of brain changes among 503 non-demented elderly with cerebral SVD. The selection procedure of the participants and study protocol were described previously in detail (van Norden et al., 2011). In short, on the basis of established research criteria SVD was defined as the presence of lacunes and/or WMH on neuroimaging (Erkinjuntti, 2002). Symptoms of SVD include acute symptoms, such as TIs or lacunar syndromes, or subacute manifestations, such as cognitive and motor (gait) disturbances and/or depressive symptoms (Roman et al., 2002). Inclusion criteria were: (a) age between 50 and 85 years; and (b) cerebral SVD on neuroimaging. The main exclusion criteria were dementia (American Psychiatric Association, 2000), (psychiatric) disease interfering with cognitive testing or follow-up, WMH or SVD mimics and MRI contraindications or known claustrophobia. Consecutive patients referred to the Department of Neurology between October 2002 and November 2006 were selected for participation. Participants were selected for participation in the study by a three-step approach. After reviewing the medical history, 1004 individuals were invited by letter. Of those 1004, 7 these numbers seem odd the way they are displayed. Is this correct??27 were eligible after contact by telephone and 525 agreed to participate. In 22 individuals exclusion criteria were found during their visit to our research center, yielding a response of 71.3% (503/705). For the present study, 59 subjects were additionally excluded because of territorial infarcts (n = 55) and inadequate quality of the MRI image (n = 4), resulting in a final population of 444 participants. All participants signed an informed consent form. The Medical Review Ethics Committee region Arnhem-Nijmegen approved the study.

2.2. Measurement of cognitive function

Cognitive function was assessed by a standardized neuropsychological test battery and has been described in detail elsewhere (van Norden et al., 2011). Performance across tests was made comparable by transforming raw test results in z-scores. We calculated compound scores for seven cognitive domains. Global cognitive function was evaluated by the Mini Mental State Examination (MMSE) and the cognitive index. The cognitive index is a compound score that was calculated as the mean of the z-scores of the 1-letter subtask of the Paper–Pencil Memory Scanning Task, the mean of the reading subtask of the Stroop test, the mean of the Symbol–Digit Substitution Task and the mean of the added score on the three learning trials of the Rey Auditory Verbal Learning Test and the delayed recall of this last test (Vermeer et al., 2003). Verbal memory is a compound score of the mean of two z-scores from the Rey Auditory Verbal Learning Test; one for the added scores of the three learning trials of this test, and one for the delayed recall of this test. Visuospatial memory is a compound score of the mean of the z-scores of the immediate recall trial and the delayed recall trial of the Rey’s Complex Figure Test. Psychomotor speed was calculated as the mean of the z-scores of the 1-letter subtask of the Paper–Pencil Memory Scanning Task, the reading subtask of the Stroop test and the Symbol–Digit Substitution Task. Fluency was calculated from the mean of the z-scores of both verbal fluency tasks. Concept shifting was calculated as the z-score of the third subtask of the Stroop. Attention is a compound score of the z-score of the total time of the Verbal Series Attention Test (de Groot et al., 2000).

2.3. Magnetic resonance imaging scanning protocol

MRI scans of all participants were acquired on a single 1.5-T MRI. The protocol included, among other sequences, the following whole brain scans: 3D T1 magnetization-prepared rapid gradient echo (MPRAGE) sequence (TR/TE/TI 2250/3.68/850 ms; flip angle15°; voxel size 1.0 × 1.0 × 1.0 mm), a fluid-attenuated inversion recovery (FLAIR) sequence (TR/TE/TI 9000/84/2200 ms; voxel size 1.0 × 1.2 × 5.0 mm, interslice gap 1 mm) and DTI sequences (TR/TE 10,100/93 ms; voxel size 2.5 × 2.5 × 2.5 mm; 4 unweighted scans, 30 diffusion weighted scans with b-value 900 s/mm²).

2.4. Conventional magnetic resonance imaging analysis

WMH were manually segmented on FLAIR images and the number of lacunes was rated according to a standardized protocol (van Norden et al., 2011). In addition, the visual Fazekas scale was used on the FLAIR images to rate the severity of changes in the white matter (Fazekas et al., 1987). All imaging analyses were performed by two trained raters blinded to clinical information. In a random sample of 10%, interrater variability for total WMH volume yielded an intra-class correlation coefficient of 0.99. The probability map of the white matter hyperintensities were created using a method previously described by de Laat and colleagues (de Laat et al., 2011). In short, we registered the WMH maps to the T1 images using the transformation matrix from the registration parameters of skull-striped FLAIR images to the T1-images that were obtained using Functional MRI of the Brain linear image registration tool (http://www.fmrib.ox.ac.uk/fsl/flirt). Next, we normalized the WMH maps non-linearly to the group-specific template using the transformation parameters of T1 images to the group-specific template obtained from Functional MRI of the Brain non-linear registration tool (http://www.fmrib.ox.ac.uk/fsl/flirt). Finally, we averaged the normalized WMH maps to create a probability map of the WMH of the study population (Fig. 1).

We computed gray (GM) and WM tissue and cerebrospinal fluid (CSF) probability maps using SPM 5 unified segmentation routines on the T1 MPRAGE images (Ashburner and Friston, 2005). Total GM, WM and CSF volumes were calculated by summing all voxel volumes that had a p > 0.5 for belonging to that tissue class. Total brain volume (TBV) was taken as the sum of total GM and WM. Intracranial volume (ICV) was a summation of all tissue classes. To normalize for head size, TBV was expressed as percentage of total ICV.

2.5. DTI analysis

Tract-based spatial statistics (TBSS) is a relatively new method that mitigates the limitations of VBM analysis (Smith et al., 2006). This analysis is restricted to those WM voxels that constitute the skeleton (core) of the brains connectional architecture. This skeleton can be matched
more accurately (compared to whole-brain normalization) across subjects, enabling robust voxel-wise analysis of the microstructural WM integrity across subjects.

Diffusion data were first preprocessed to detect and correct head and cardiac motion artifacts, using an in-house developed iteratively re-weighted-least-squares algorithm named ‘PATCH’ (Zwiers, 2010). FA, MD, AD and RD images were then calculated using DTIFit within the Functional MRI of the Brain diffusion toolbox, which were fed into the TBSS pipeline (Smith et al., 2006). The thinning procedure was conducted on the mean FA image to create a common skeleton, which represents the core-structure of the WM tract. This skeleton was thresholded at the FA-value 0.3 to include the major WM tracts and to account for the inter-subject variability. All normalized FA data were then projected onto this skeleton. These skeleton projection factors were then applied to the MD, AD and RD images. These data were then fed into the voxel-wise cross-subject statistics. In addition, we obtained FA, MD, AD and RD for three parts of the corpus callosum by performing region-of-interest analyses. The corpus callosum provides interhemispheric connections between cortical and subcortical regions and might play an important role in cognitive function (Bloom and Hynd, 2005). We created masks for genu, body and splenium of the corpus callosum by applying the WM atlas (Johns Hopkins University WM labels, provided by Functional MRI of the Brain Software Library (FSL)) on the mean FA skeleton. The masks were visually inspected and miscellaneous voxels that belonged to other regions, such as the cingulum bundle, were excluded.

2.6. Other measurements

Age, sex and level of education, depressive symptoms and normalized TBV were considered possible confounders. Depressive symptoms were assessed using the Center for Epidemiologic Studies on Depression Scale (CES-D) (Radloff, 1977). Functional independence was assessed using the Barthel Index (range 0–20) (Mahoney and Barthel, 1965). For assessment of vascular risk factors, structured questionnaires were used together with measurements of blood pressure taken on separate occasions. The risk factors included presence of hypertension (mean blood pressure ≥140/90 mm Hg and/or use of anti-hypertensive medications) (Rosendoff, 2007), diabetes (treatment with antidiabetic drugs), hypercholesterolemia (treatment with lipid-lowering drugs) and smoking status.

2.7. Statistical analysis

Baseline characteristics were presented as mean ± standard deviation (SD) and for the skewed parameters the median and interquartile ranges were calculated.

For the TBSS analyses, we assessed voxel-wise correlations between the skeletal DTI parameters (FA and MD) and cognitive performance on several cognitive domains, while adjusting for age, sex, education, depressive symptoms and normalized TBV. To test whether these associations were independent of WMH and lacunes, we adjusted for WMH volume and number of lacunes in a second model. For the voxel-wise statistical analyses, we applied permutation-based statistical interference tool for non-parametric approach, with number of permutation tests set to 5000 (Nichols and Holmes, 2002). Significant clusters were identified using the threshold–free cluster enhancement with a p-value < 0.05, corrected for multiple comparisons (Smith and Nichols, 2009).

For the ROI analyses, we computed regression coefficients of the mean FA, MD, AD and RD of the three ROI in the corpus callosum with cognitive performance, while adjusting for age, sex, education, depressive symptoms, normalized TBV, white matter hyperintensities and number of lacunes. Regression coefficients were presented as standardized β-values. Bonferroni corrections were applied.

3. Results

Demographic and neuroimaging characteristics are shown in Table 1. Mean age of the population (n = 444) was 65.3 years (SD 8.9) and 54.7% were male. Mean WM volume was 467.4 ml (SD 65.4). The largest part of the WM consisted of NAWM, with a median percent volume and number of lacunes in a second model. For the voxel-wise statistical analyses, we applied permutation-based statistical interference tool for non-parametric approach, with number of permutation tests set to 5000 (Nichols and Holmes, 2002). Significant clusters were identified using the threshold–free cluster enhancement with a p-value < 0.05, corrected for multiple comparisons (Smith and Nichols, 2009).

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### Table 1: Baseline characteristics of the study population.

<table>
<thead>
<tr>
<th>Characteristics</th>
<th>n = 444</th>
</tr>
</thead>
<tbody>
<tr>
<td>Demographics</td>
<td></td>
</tr>
<tr>
<td>Age (years)</td>
<td>65.3 (8.9)</td>
</tr>
<tr>
<td>Male*</td>
<td>243 (54.7)</td>
</tr>
<tr>
<td>Only primary education*</td>
<td>44 (10)</td>
</tr>
<tr>
<td>CES-D scale</td>
<td>11.2 (9.5)</td>
</tr>
<tr>
<td>Mini mental state examination</td>
<td>28.1 (1.6)</td>
</tr>
<tr>
<td>Hypertension*</td>
<td>320 (72.1)</td>
</tr>
<tr>
<td>Diabetes*</td>
<td>61 (13.7)</td>
</tr>
<tr>
<td>Hypercholesterolemia*</td>
<td>194 (43.7)</td>
</tr>
<tr>
<td>Smokers, current*</td>
<td>69 (15.5)</td>
</tr>
<tr>
<td>Smokers, former*</td>
<td>239 (53.8)</td>
</tr>
<tr>
<td>Neuroimaging</td>
<td></td>
</tr>
<tr>
<td>TBV, ml</td>
<td>1098.0 (1205)</td>
</tr>
<tr>
<td>ICV, ml</td>
<td>1673.8 (1582)</td>
</tr>
<tr>
<td>WMH volume, ml†</td>
<td>6.4 (3.3; 16.8)</td>
</tr>
<tr>
<td>White matter volume, ml</td>
<td>467.4 (65.4)</td>
</tr>
<tr>
<td>Lacunes*</td>
<td>102 (23.6)</td>
</tr>
</tbody>
</table>

Data represent N of subjects* (%), mean (SD), or median (interquartile range). TBV: total brain volume; ICV: intracranial volume; WMH: white matter hyperintensities.
were predominately located in the frontal periventricular regions (Fig. 1). 13 participants (2.9% of the study population) were diagnosed with mild cognitive impairment.

Fig. 2 shows the relation between FA and the cognitive domains tested ($p < 0.05$, FWE-corrected for multiple comparisons). FA in the frontal, parietal, occipital, temporal but also in the infratentorial voxels of the skeleton was positively related to the cognitive index, attention and verbal memory performance. A lower FA in almost all regions was associated with higher scores on psychomotor speed and concept shifting (indicating lower performance). We found a similar distribution for the inverse association with MD and the cognitive domains. With regard to MMSE, visuospatial memory and fluency, no significant associations were found for FA and MD. A significant ($p$-corrected < 0.01) association was identified in almost all voxels of the skeleton in the relation between FA and cognitive index and concept shifting. The strongest significant ($p$-corrected < 0.01) relation between MD and psychomotor speed and cognitive index was located in the frontal lobe and the corpus callosum. The relation between FA and MD and verbal memory was most outspoken along the whole course of the corpus callosum and the cingulum bundle ($p$-corrected < 0.01).

Additional adjustment for WMH and lacunes (Fig. 2B) weakened the relations between the FA and cognitive index, psychomotor speed, verbal memory and concept shifting, but remained present ($p$-corrected < 0.05). There were no associations between for FA and attention after additional adjustment for WMH and lacunes. There were no associations between MD and attention after additional adjustment for WMH and lacunes, while the associations between MD and psychomotor speed and concept shifting weakened but remained significant. Voxels with the highest significance for FA in relation to cognitive index, psychomotor speed, verbal memory and concept shifting were located in the corpus callosum ($p$-corrected < 0.01). In addition, FA in the cingulum bundle and corpus callosum remained highly associated with verbal memory performance ($p$-corrected < 0.01).
chomotor slowing due to impaired executive function, de
clinical manifestations of cognitive impairment are usually of a charac-
ters, such as hypertension or diabetes, as they were considered a part
The abnormalities in microstructural integrity of the NAWM are par-
tial SVD-related, as our results showed that the presence of WMH and
 Structural abnormality of the white matter tracts has been found in
Alzheimer’s disease and mild cognitive impairment and has been dem-
our results suggest a disruption of cortical–cortical and cortical–subcortical connections, and a subsequent ‘disconnection-syndrome’ accounting for cognitive disturbances in patients with SVD (O’Sullivan et al., 2001a). In concordance with the findings from previous studies (van Norden et al., 2012; Vernooij et al., 2009), this suggests that microstructural integrity of the NAWM should also be taken into account when investigating the relation between SVD and cognitive function and that DTI should be considered part of the imaging protocol in future studies on cognitive performance.
In conclusion, our study showed that cognitive disturbances in el-
attention, planning and set-shifting and forgetfulness (Roman et al.,
We showed that WM integrity at specific locations was related to
cognitive performance. The strongest significant relations be-
tween microstructural integrity and verbal memory performance
were located in the cingulum bundle. This bundle, which connects the
medial temporal lobe and the posterior cingulate cortex, is an important
structure in verbal memory performance (Sepulcre et al., 2008; van der Holst et al., 2013). We also found verbal memory to be associated with
the anterior parts of the corpus callosum. Episodic memory is partially
dependent on interhemispheric interaction (Christman and Propper, 2001). Loss of microstructural integrity of the corpus callosum can lead to impaired interhemispheric interaction, resulting in impaired (verbal) memory performance. With regard to psychomotor speed, we found that the strongest significant relation with microstructural in-
tegrity was located in the corpus callosum and frontal lobe. The
As post-hoc analysis we analyzed the corpus callosum in more ana-
tomical detail by segmenting it in three regions (Table 2). We found that
microstructural integrity of genu and splenium of the corpus callosum
related to cognitive index, but also with executive domains, psychomo-
tor speed and concept shifting (p < 0.05 after Bonferroni corrections).
The microstructural integrity of body was associated with verbal mem-
ory. We found no relations between microstructural integrity in corpus
callosum and attention, visuospatial memory, MMSE and fluency. The associations with MD and cognitive performance were mainly driven
by changes in RD, and not by changes in AD.
4. Discussion
In this study, we examined the relation between the microstructural
integrity of the WM and cognitive performance in subjects with cerebral
SVD. We demonstrated that low FA and high MD in multiple regions of
the WM were associated with lower scores on cognitive performance.
The corpus callosum showed the highest significant relation with cogni-
tive function, especially in the genu and splenium. The microstructural
integrity of the cingulum bundle showed the highest significant relation
with verbal memory performance and the frontal WM with psychomo-
tor speed.
A limitation is the cross-sectional nature of our study, which limits
causal inference. The RUN DMC study has a longitudinal design and
follow-up is currently being executed to evaluate the effect of progres-
sion of SVD on (changes in) cognitive performance (van Norden et al.,
2011). In addition, we did not intentionally adjust for vascular risk fac-
tors, such as hypertension or diabetes, as they were considered a part
of the causal chain between SVD and cognitive performance. Major
strengths of the study included the large sample size, the single center
design, the use of a single scanner and the high response rate. Further-
more, we manually segmented the WMH. Extensive neuropsychological
assessment was performed by two investigators and all analyses were
adjusted for potential confounders.
Table 2
Association between the microstructural integrity of the corpus callosum and cognitive performance.

<table>
<thead>
<tr>
<th>Cognitive index</th>
<th>Verbal memory</th>
<th>Psychomotor speed</th>
<th>Concept shifting</th>
</tr>
</thead>
<tbody>
<tr>
<td>Genu FA</td>
<td>.19*</td>
<td>.12</td>
<td>.16*</td>
</tr>
<tr>
<td>MD</td>
<td>−.19</td>
<td>−.13</td>
<td>−.14*</td>
</tr>
<tr>
<td>AD</td>
<td>−.12</td>
<td>−.10</td>
<td>−.06</td>
</tr>
<tr>
<td>RD</td>
<td>−.19</td>
<td>−.12*</td>
<td>−.16*</td>
</tr>
<tr>
<td>Body FA</td>
<td>.14</td>
<td>.13*</td>
<td>.09</td>
</tr>
<tr>
<td>MD</td>
<td>−.16</td>
<td>−.14*</td>
<td>−.10</td>
</tr>
<tr>
<td>AD</td>
<td>−.08</td>
<td>−.05</td>
<td>−.05</td>
</tr>
<tr>
<td>RD</td>
<td>−.16</td>
<td>−.14*</td>
<td>−.10</td>
</tr>
<tr>
<td>Splenium FA</td>
<td>.19*</td>
<td>.09</td>
<td>.18*</td>
</tr>
<tr>
<td>MD</td>
<td>−.15</td>
<td>−.09</td>
<td>−.13</td>
</tr>
<tr>
<td>AD</td>
<td>−.02</td>
<td>−.04</td>
<td>−.01</td>
</tr>
<tr>
<td>RD</td>
<td>−.18</td>
<td>−.09</td>
<td>−.17*</td>
</tr>
</tbody>
</table>

Standardized β-values adjusted for age, sex, education, depressive symptoms, normalized TIV, white matter hyperintensities and number of lacunes. FA: fractional anisotropy. MD: mean diffusivity. AD: axial diffusivity. RD: radial diffusivity.
* p < .05 (Bonferroni corrected).


