A Biomaterial Composed of Collagen and Solubilized Elastin Enhances Angiogenesis and Elastic Fiber Formation Without Calcification

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ABSTRACT

Elastin is the prime protein in elastic tissues that contributes to elasticity of, for example, lung, aorta, and skin. Upon injury, elastic fibers are not readily replaced, which hampers tissue regeneration. Incorporation of solubilized elastin (hydrolyzed insoluble elastin fibers or elastin peptides) in biomaterials may improve regeneration, because solubilized elastin is able to promote proliferation as well as elastin synthesis. Porous biomaterials composed of highly purified collagen without and without elastin fibers or solubilized elastin were prepared by freezing and lyophilization. Solubilized elastin formed spherical structures that were incorporated in the collagenous part of the scaffolds and that persisted after chemical crosslinking of the scaffolds. Crosslinked scaffolds were subcutaneously implanted in young Sprague Dawley rats. Collagen-solubilized elastin and collagen scaffolds showed no calcification in this sensitive calcification model, in contrast to scaffolds containing elastin fibers. Collagen-solubilized elastin scaffolds also induced angiogenesis, as revealed by type IV collagen staining, and promoted elastic fiber synthesis, as shown with antibodies against rat elastin and fibrillin-1. It is concluded that scaffolds produced from collagen and solubilized elastin present a non-calcifying biomaterial with a capacity for soft-tissue regeneration, especially in relation to elastic fiber synthesis.

INTRODUCTION

Elastin is the major insoluble protein present in elastic tissue, contributing to the elasticity of lung, aorta, ligaments, and skin. Elastic fibers are not readily replaced upon injury,1 probably because of difficulties in recapitulating normal developmental expression patterns of tropoelastin and associated molecules.2,3 This seriously hampers tissue regeneration.

Solubilized elastin (obtained by hydrolyzing insoluble elastin) may markedly improve tissue regeneration, because it exhibits multiple biological effects. These include enhanced cell migration,4 cell proliferation,5 and elastin synthesis.6,7 Solubilized elastin interacts with the elastin-laminin receptor, which is composed of 3 subunits: 2 transmembrane subunits of 61 and 55 kDa and 1 extracellular subunit of 67 kDa, the latter binding tropoelastin and other elastin-like molecules. The receptor is present on a large number of cells, including fibroblasts, vascular smooth muscle cells, endothelial cells, chondrocytes, monocytes, lymphocytes, and polymorphonuclear leukocytes, and its signal transduction pathway is mediated through a pertussis toxin–sensitive G-protein.8–11 In

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addition to the elastin-laminin receptor, other receptors may play a role as well (e.g., integrins).12 Biomaterials containing solubilized elastin may thus exert biological effects on a wide variety of cell types.

We have previously prepared biomaterials composed of highly purified type I collagen and elastin fibers and studied their tissue reaction.13,14 In young Sprague Dawley rats (but not in adult rats), implantation of these scaffolds resulted in calcification of elastin fibers. Although initiation of tissue calcification does not require a cellular response,15 the in vivo milieu can accelerate the process16 (e.g., through the extracellular release of enzymes by macrophages and giant cells involved in elastin degradation).17-20

We here hypothesize that porous scaffolds containing solubilized elastin may improve synthesis of elastin through interaction with the elastin-laminin receptor.6 Furthermore, if enzymes involved in elastin degradation play a role in increasing calcification, application of solubilized elastin may reduce the presence of macrophages and giant cells and thus reduce calcification. In addition, solubilized elastin is less hydrophobic and more charged than insoluble elastin. Negative charges from C-terminal carboxylic groups may prevent positively charged calcium ions from precipitating in the same way, because negatively charged sulfate groups have been shown to suppress calcium binding to, for example, polyurethane.21 In this study, we therefore prepared and characterized collagen, collagen–elastin fibers, and collagen-solubilized elastin scaffolds and studied calcification, angiogenesis, and elastin synthesis after subcutaneous implantation.

MATERIALS & METHODS

Materials

Mouse anti-bovine elastin immunoglobulin (Ig)G clone BA-4 was purchased from Sigma Chemical Co. (St Louis, MO); goat anti-rat alpha-elastin from Elastin Products Co. (Owensville, MO); rabbit anti-bovine type I collagen, rabbit anti-rat type I collagen, and rabbit anti-rat type III collagen IgGs from Chemicon (Temecula, CA); and goat anti-human type IV collagen IgG from Southern Biotechnology Inc. (Birmingham, AL). Rabbit anti-human fibrillin-1 (pAb-rF6H) and rabbit anti-human fibrillin-2 (anti-rFBN2-1) anti-sera were prepared as described previously.22,23 Alexa488- and Alexa594-labeled secondary antibodies were from Molecular Probes Europe (Leiden, The Netherlands), and rabbit anti-goat peroxidase and 3,3-diaminobenzidine tetrahydrochloride (DAB) were from DAKO (Glostrup, Denmark).

Isolation of scaffolds components

Insoluble type I collagen was purified from bovine Achilles tendon. Briefly, tendons were cleaned from non-collagenous tissue, pulverized under liquid nitrogen conditions using a Pulverisette 19 with a 0.5-mm sieve (Fritsch, Idar-Oberstein, Germany), and consecutively rinsed extensively with 0.1 M sodium chloride (NaCl) in 50 mM Tris-hydrochloric acid (HCl) pH 7.2, 1.0 M NaCl in 50 mM Tris-HCl pH 7.2, 4 M urea in 0.5 M acetic acid, 0.5 M acetic acid, aceticone, and demineralized water.24

Insoluble elastin fibers (EL-fiber) were isolated from equine ligamentum nuchae. Non-elastinous tissue was removed, and ligaments were pulverized under liquid nitrogen conditions through a 1.0 mm sieve. The pulverized ligament was then washed and treated with 1 M NaCl in 10 mM phosphate buffer pH 7.4 (PB), various organic solvents, formic acid with cyanogen bromide, 4 M urea plus 1 M 2-mercaptoethanol in 0.1 M PB, trypsin, and 1 M NaCl in 10 mM PB.25 Solubilized elastin (EL-sol) was prepared from insoluble elastin fibers using oxalic acid hydrolysis.

Briefly, 10 g of elastin was hydrolyzed for 1 h with 75 mL 0.25 M oxalic acid at 95°C. Then the preparation was quickly cooled on ice and centrifuged, and the supernatant was collected. The pellet was hydrolyzed again for 1 h with oxalic acid, followed by cooling and centrifuging. This procedure was repeated until all insoluble material was solubilized (generally after a total of 14 steps). Supernatants were pooled, dialyzed against 10 mM PB, and subsequently dialyzed against MilliQ water using Amicon Ultra-15 10 kDa MWCO filter tubes (Millipore, Billerica, MA).

Characterization of solubilized elastin preparation

The amount of solubilized elastin in the elastin pool was determined according to the method develop by Lowry,27 size of elastin using 1-dimensional gel electrophoresis (4% polyacrylamide gel with silver staining),28 and gel permeation chromatography29 [column material: Sephacryl S-500, reference samples: ferritin (0.88 MDa), dextran blue (2 MDa), and Helix pomatia hemocyanin (9 MDa)], size-charge distribution using 2-dimensional gel electrophoresis,30 amine group content after reaction with 2,4,6-trinitrobenzene sulfonic acid,31 and amino acid composition using a Biochrom 20 amino acid analyser (Amersham Pharmacia Biotech, Uppsala, Sweden).32

Preparation of scaffolds

Various scaffolds were prepared composed of collagen only (COL); collagen plus insoluble elastin fibers in a 1:1 ratio (COL-EL-fiber); and collagen with solubilized elastin in 97:3, 9:1, and 1:1 ratios (COL-EL-sol).

Briefly, a 2% (w/v) protein suspension (collagen without or with elastin fibers) was shaken overnight in 0.5 M acetic acid at 4°C. If appropriate, EL-sol was added and the suspension diluted to 1% (w/v) with cold MilliQ water and homogenized on ice using a Potter-Elvehjem homogenizer. Air-bubbles were removed by centrifuging at 250 g for 10 min at 4°C. The suspension was then slowly poured into a plastic mould, frozen in a bath of ethanol and solid carbon
dioxide (CO₂) (–80°C) and lyophilized in a Zirbus lyophilizer (Bad Grund, Germany). For scaffolds composed of collagen plus ELsol in a 1:1 ratio, a suspension with a final concentration of 1.6% was used as well.

Scaffolds were applied as such (non-crosslinked) or crosslinked. For crosslinking, 200 mg of scaffold was incubated for 4 h at 22°C with 20 mL 33 mM 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide (EDC) and 6 mM N-hydroxysuccinimide (NHS) in 50 mM 2-morpholinoethane sulfonic acid (pH 5.0) containing 40% ethanol. EDC/NHS crosslinked scaffolds were then washed with 0.1 M disodium hydrogen phosphate (twice for 1 h), 1 M NaCl (twice for 2 h), 2 M NaCl (once overnight, 5 times for 30 min), and MilliQ water (6 times for 30 min). The scaffolds were then frozen in ethanol/CO₂ again and lyophilized. For in vivo experiments, EDC/NHS-crosslinked COL and COL-EL₁₁ fibre scaffolds from a 1:1 ratio suspension were used along with COL-ELsol 1:1 scaffolds from a 1.6% suspension.

Characterization of scaffolds

The amine group content was measured to evaluate the degree of crosslinking. The amount of ELsol bound to collagen was established by estimating the protein content in the solution after crosslinking. Proteins in this solution were precipitated with 10% 2,4,6-trichloroacetic acid on ice for 2 h and centrifuged. The pellet was then dissolved in 10 mM sodium hydroxide and the protein amount assayed according to the method developed by Lowry. The same procedure was applied to evaluate the in vitro release of ELsol from the scaffolds. Neither non-crosslinked nor EDC/NHS-crosslinked collagen scaffolds gave any release of protein from the scaffolds after 24 h or 7 days in PBS, and therefore the protein release from COL-ELsol scaffolds could be attributed to ELsol only. Water-binding capacity of scaffolds was determined as previously described. Scanning electron microscopy was used to analyze the morphology of the scaffolds, transmission electron microscopy to determine the ultrastructure of the scaffolds, and immunofluorescence microscopy to study the distribution of ELsol in the scaffolds using mouse anti-bovine elastin (1:1000) as a primary antibody.

In vivo evaluation of scaffolds

The Ethics Committee of the Radboud University Nijmegen Medical Centre approved the study. Sprague-Dawley rats (male, 3 weeks old) were purchased from Harlan (Zeist, The Netherlands) and housed 2 per cage. The animals were fed pelleted diet and water ad libitum. Scaffolds were washed in 70% (v/v) ethanol and sterile PBS. Rats were anesthetized with isoflurane, and subcutaneous pockets were made to the right and left of 2 midline incisions on the back.

Punches (ø 6 mm) of the scaffolds were implanted in the pockets at a distance of approximately 1 cm from the incisions (4 implants/rat). In this study, 6 COL, 6 COL-EL₁₁ fibre, and 12 COL-ELsol scaffolds were implanted (2 COL, 2 COL-EL₁₁ fibre, and 4 COL-ELsol per time point), and a total of 6 rats was used. Lower numbers of COL and COL-EL₁₁ fibre scaffolds were used because these were compared with previous results. All scaffolds were crosslinked using EDC/NHS. Implants with surrounding tissue were harvested at 3, 7, and 21 days after implantation. Immediately after explantation, scaffolds were divided in half. One half was processed for conventional histology and the other half for immunohistochemistry.

For conventional histology, explants were fixed in 4% (v/v) formaldehyde in PB for at least 24 h at 4°C and embedded in paraffin. Five-µm sections were stained with hematoxylin-eosin, Elastin Van Gieson (visualization of elastin and collagen), or Von Kossa (visualization of calcium deposits). The total area of calcification in the scaffold was determined using Neulucida software (MBF Bioscience, Williston, VT) and expressed as a percentage of the total implant size. Values were compared using the Student t-test, and p < 0.05 was considered to be statistically significant. At least two persons performed histological evaluation independently.

Immunohistochemistry (immunofluorescence and DAB staining) was used to study the biodegradation of scaffold components and the formation of extracellular matrix by the host. Scaffolds were frozen in liquid nitrogen, and 5-µm cryosections were mounted on super frosted slides and air-dried. Immunofluorescence assay was performed as previously described. Primary antibodies used were mouse anti-bovine elastin (1:1000), rabbit anti-bovine type I collagen, goat anti-rat elastin, rabbit anti-rat type I collagen, rabbit anti-rat type III collagen (all 1:100), rabbit anti-human fibrillin-1, and rabbit anti-human fibrillin-2 (both 1:500). Antibodies were visualized with Alexa488- or Alexa594-conjugated secondary antibodies diluted in PBS containing 5% normal rat serum. The antibody to bovine elastin also reacted with equine elastin, the antibodies against human fibrillin also reacted with rat fibrillin, and the antibody to bovine type I collagen did not substantially cross-react with rat type I collagen or vice versa. For immunohistochemistry with the DAB-staining method, cryosections were fixed with 4% paraformaldehyde in PBS for 20 min. Endogenous peroxidase was inhibited with 0.3% hydrogen peroxide (H₂O₂) for 10 min. After blocking for 30 min with 2% bovine serum albumin in PBS containing 0.1% Tween (PBST), sections were incubated with goat anti-human type IV collagen (1:50) for 1 h, washed, incubated for 1 h with rabbit anti-goat IgG peroxidase (1:100), and washed. Antibodies were diluted in PBST containing 5% normal rabbit serum; washings were with PBST. Sections were washed with 50 mM Tris-HCl (pH 7.6) and incubated for 10 min with DAB (0.5 mg/mL) and ammonium nickel sulfate (7.5 mg/mL) in Tris-HCl. Finally, the reaction substrate was added (0.2 µl 30% H₂O₂/mL). Sections were washed, counterstained with hematoxylin, dehydrated, and embedded. The antibody to human type IV collagen cross-reacted with rat type IV,
collagen. The total area of blood vessels (including the lumen) in the scaffold was determined and expressed as a percentage of the total implant size using Neurolucida software. Values were compared using the Student t-test, and p<0.05 was considered to be statistically significant.

RESULTS

Analysis of solubilized elastin preparation

The solubilized elastin preparation was analyzed using sodium dodecyl sulfate polyacrylamide gel electrophoresis, which revealed that the molecular mass of the solubilized elastin ranged from 70 to over 880 kDa. Gel permeation chromatography gave a mean molecular mass of the solubilized elastin of approximately 1100 kDa. Two-dimensional gel electrophoresis showed that the elastin peptides had an isoelectric point of approximately 6. The mean amine group content ± standard deviation of the solubilized elastin was 292 ± 5 nmol amine groups per mg of protein. Amino acid composition of solubilized elastin was similar to that of elastin fibers for all amino acid residues, including desmosine and isodesmosine (both 0.5 ± 0.0 per 1000 amino acid residues).

Analysis of scaffolds containing solubilized elastin

Porous scaffolds were prepared using various ratios of collagen with ELsol. After 4 h of crosslinking, less than 5% of ELsol could be retrieved from the remaining crosslinking solution. Hence, the crosslinking efficiency of ELsol to the scaffolds was at least 95%. The biochemical characteristics of the scaffolds are summarized in Table 1. EDC/NHS crosslinking coupled ELsol firmly to the scaffolds, because the in vitro release was only 2% after 7 days in the case of EDC/NHS-crosslinked collagen plus ELsol scaffolds, whereas it was 60% after only 24 h when crosslinking was omitted.

Collagen and ELsol each possessed approximately 300 nmol amine groups per mg. Therefore, scaffolds made from these components had the same amount of amine groups for all ratios before crosslinking. After EDC/NHS crosslinking, approximately 60% of the amine groups remained for all scaffolds, indicating that 40% of the amine groups was used in the crosslinking reaction.

ELsol did not contribute to the water-binding activity of scaffolds. At a higher percentage of ELsol, the water-binding capacity of COL-ELsol scaffolds was lower.

Using scanning electron microscopy (Fig. 1), non-crosslinked COL-ELsol scaffolds showed spherical structures attached to collagenous fibrils or sheets. Spheres of different sizes (ranging from ~200 nm to 10 µm) were found throughout the scaffolds. After crosslinking, these spheres deformed to some extent. COL and COL-ELfiber scaffolds did not show this spherical organization. Immunofluorescence staining using an antibody against bovine elastin demonstrated that the spheres in COL-ELsol scaffolds were composed of ELsol (Fig. 2A). The same was found based on the autofluorescence of elastin (Fig. 2B). Transmission electron microscopy showed that ELsol spheres in EDC/NHS-crosslinked COL-ELsol scaffolds had a wide size distribution and were mostly incorporated into the collagen.

### Table 1. Biochemical Characteristics of Scaffolds Prepared from Collagen, Collagen + Elastin Fibres and Collagen + Solubilised Elastin

<table>
<thead>
<tr>
<th>Scaffold</th>
<th>Crosslinked with EDC/NHS</th>
<th>Release after 24 h in PBS [% of total ELsol]</th>
<th>Release after 7 days in PBS [% of total ELsol]</th>
<th>Amine group content [nmol/mg scaffold]</th>
<th>Water-binding capacity [# times dry weight]</th>
</tr>
</thead>
<tbody>
<tr>
<td>ELsol*</td>
<td>–</td>
<td>0 ± 0.0</td>
<td>ND</td>
<td>292 ± 5</td>
<td>20 ± 1</td>
</tr>
<tr>
<td>COL</td>
<td>–</td>
<td>ND</td>
<td>ND</td>
<td>297 ± 14</td>
<td>16 ± 2</td>
</tr>
<tr>
<td>COL-ELfiber 1:1</td>
<td>–</td>
<td>ND</td>
<td>ND</td>
<td>160 ± 9</td>
<td>16 ± 2</td>
</tr>
<tr>
<td>COL-ELsol 97:3</td>
<td>–</td>
<td>58.0 ± 11.8</td>
<td>ND</td>
<td>300 ± 3</td>
<td>19 ± 2</td>
</tr>
<tr>
<td>COL-ELsol 9:1</td>
<td>–</td>
<td>59.3 ± 9.4</td>
<td>ND</td>
<td>290 ± 13</td>
<td>19 ± 1</td>
</tr>
<tr>
<td>COL-ELsol 1:1</td>
<td>–</td>
<td>62.3 ± 53.3</td>
<td>ND</td>
<td>298 ± 18</td>
<td>13 ± 1</td>
</tr>
<tr>
<td>COL-ELsol 1:1(1.6)**</td>
<td>–</td>
<td>66.2 ± 7.2</td>
<td>ND</td>
<td>290 ± 10</td>
<td>12 ± 1</td>
</tr>
<tr>
<td>COL</td>
<td>+</td>
<td>ND</td>
<td>0 ± 0.0</td>
<td>189 ± 5</td>
<td>20 ± 2</td>
</tr>
<tr>
<td>COL-ELfiber 1:1</td>
<td>+</td>
<td>ND</td>
<td>ND</td>
<td>98 ± 6</td>
<td>16 ± 1</td>
</tr>
<tr>
<td>COL-ELsol 97:3</td>
<td>+</td>
<td>ND</td>
<td>2.4 ± 1.5</td>
<td>190 ± 15</td>
<td>19 ± 2</td>
</tr>
<tr>
<td>COL-ELsol 9:1</td>
<td>+</td>
<td>ND</td>
<td>1.0 ± 0.8</td>
<td>171 ± 4</td>
<td>18 ± 2</td>
</tr>
<tr>
<td>COL-ELsol 1:1</td>
<td>+</td>
<td>ND</td>
<td>0.8 ± 0.7</td>
<td>163 ± 5</td>
<td>14 ± 1</td>
</tr>
<tr>
<td>COL-ELsol 1:1(1.6)**</td>
<td>+</td>
<td>ND</td>
<td>0.5 ± 0.3</td>
<td>154 ± 12</td>
<td>12 ± 1</td>
</tr>
</tbody>
</table>

*No scaffolds could be prepared of ELsol alone.

**COL-ELsol 1:1 (1.6) scaffold was prepared from a 1.6% suspension of collagen and ELsol, whereas all other scaffolds were prepared from a 1.0% protein suspension.
network (Fig. 2C, D). The latter figure also shows a sphere with a less-dense outer core. Crosslinking does not occur instantaneously, which may cause this effect.

Tissue response to implanted scaffolds

All animals remained in good condition, and no infections were observed. Macroscopically, a thin capsule was seen around the scaffolds at explantation. In Table 2, an overview of calcification behavior and cellular response is given for the 3 different scaffolds. Tissue response to COL and COL-EL_fiber scaffolds was consistent with previous results.\textsuperscript{13}

Calcification of scaffolds

In young Sprague-Dawley rats, COL-EL_sol and COL did not calcify at all in the time span investigated, in contrast to COL-EL_fiber (Fig. 3). In COL-EL_fiber especially, elastin fibers calcified from day 7 on. At day 7, 3.5% \pm 0.1% of the total scaffold surface had calcified, whereas at day 21, it was 11.5% \pm 0.7%, which was statistically significant (\(p < 0.05\)).
Cellular response to scaffolds

At day 3, cellular response to COL-ELsol showed moderate infiltration of neutrophilic granulocytes throughout the scaffold, whereas at day 7, fibroblasts and other mononuclear cells and few giant cells were found. At day 21, a greater number of phagocytic cells was observed, with strong proliferation of fibroblasts. Cellular reactions to COL and COL-ELfiber were considerably less. COL gave the mildest reaction; after 21 days, some macrophages and giant cells were present, mainly at the periphery of the scaffolds. At day 3, cellular response to COL-ELfiber included some neutrophilic granulocytes that had entered the outer part of the scaffold. At day 7, fibroblasts and other mononuclear cells were found in the scaffold, with some giant cells at the periphery of the scaffold, and at day 21, phagocytic cells like macrophages and giant cells dominated the scaffold, whereas the number of non-phagocytic cells had increased at the periphery. Although more macrophages were found in COL-ELsol, the number of giant cells in COL-ELsol and COL-ELfiber was similar.

Vascularization of scaffolds

Type IV collagen (present in endothelial basement membranes) was used as a marker for blood vessels (Fig. 4). At day 3, no blood vessels were observed in the scaffolds, although they were found in the surrounding tissue. At day 7, COL-ELsol showed more blood vessels than COL-ELfiber and COL, but differences were not statistically significant. At day 21, blood vessels were also most abundant in COL-ELsol, both at the periphery and within the scaffold, accompanied by more large blood vessels. COL-ELsol now contained a significantly larger area of blood vessels than COL-ELfiber and COL. At this time, COL-ELfiber also had statistically significantly more blood vessels than COL. In this scaffold, vascularization was also present at the periphery, but considerably fewer vessels were found within the scaffold. In COL, blood vessels were found mainly at the periphery of the scaffolds.

Table 2. General Overview of Calcification and Cellular Events after Subcutaneous Implantation of the Scaffolds in Young Sprague Dawley Rats

<table>
<thead>
<tr>
<th>Scaffold</th>
<th>Implantation time (days)</th>
<th>Calcification</th>
<th>PMNs</th>
<th>Phagocytic cells</th>
<th>Non-phagocytic cells*</th>
<th>Blood vessels**</th>
</tr>
</thead>
<tbody>
<tr>
<td>COL</td>
<td>3</td>
<td>–</td>
<td>sp</td>
<td>±</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>7</td>
<td>–</td>
<td>–</td>
<td>±</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>21</td>
<td>–</td>
<td>–</td>
<td>+</td>
<td>±</td>
<td>–</td>
</tr>
<tr>
<td>COL-ELfiber</td>
<td>3</td>
<td>–</td>
<td>±</td>
<td>±</td>
<td>sp</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>7</td>
<td>±</td>
<td>sp</td>
<td>±</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>21</td>
<td>+</td>
<td>–</td>
<td>+±</td>
<td>+</td>
<td>–</td>
</tr>
<tr>
<td>COL-ELsol</td>
<td>3</td>
<td>–</td>
<td>+±</td>
<td>±</td>
<td>sp</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>7</td>
<td>–</td>
<td>sp</td>
<td>±</td>
<td>–</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>21</td>
<td>–</td>
<td>–</td>
<td>++</td>
<td>++</td>
<td>++</td>
</tr>
</tbody>
</table>

* Absolute numbers of non-phagocytic cells were lower than of phagocytic cells, e.g. + for phagocytic and giant cells refers to more cells than ++ for non-phagocytic cells.

** Blood vessels were assessed by immunostaining for rat type IV collagen, present in vascular basement membranes. PMNs = polymorphic nuclear cells, i.e. granulocytes; phagocytic cells include macrophages, giant cells and monocytes; non-phagocytic cells include fibroblasts, lymphocytes and plasma cells. Events were scored ranging from sporadic (sp) to abundant (+++). -: not present.
FIG. 3. Light microscopy evaluation of calcification of scaffolds 21 days after implantation in young Sprague-Dawley rats. (A) Collagen alone (COL), (B) collagen plus insoluble elastin fiber (COL-Elfiber), (C) collagen with solubilized elastin (COL-ELsol) scaffold. Calcium deposits have an intense black color due to Von Kossa staining and are only found in COL-ELfiber. Bar is 50 μm.

FIG. 4. Light microscopical evaluation of angiogenesis in scaffolds 21 days after implantation in young Sprague-Dawley rats. Sections were stained for type IV collagen as a marker for blood vessels. (A) Collagen alone (COL), (B) collagen plus insoluble elastin fiber (COL-Elfiber), (C) periphery of collagen with solubilized elastin (COL-ELsol), (D) within COL-ELsol scaffold. Bar is 50 μm. (E) Quantification of the blood vessels in the scaffold using type IV collagen and expressed as a percentage of the total scaffold area. At day 21, COL-ELsol had significantly more blood vessels than COL and COL-Elfiber.* p < 0.05.
Scaffold degradation and new matrix synthesis

Table 3 gives an overview of the immunostaining for scaffold components and newly formed extracellular matrix molecules at different times.

### Scaffold degradation

Scaffold degradation was studied using conventional histology and immunohistochemistry with antibodies for scaffold elastin and collagen. From day 7, elastin staining in COL-ELsol decreased, and after 21 days, elastin staining was reduced even more. Elastin spheres were still present at this time, especially in the central part of the scaffolds (Fig. 5A, B). At the periphery of the scaffolds, staining intensity was less, and spheres were smaller, suggesting resorption and degradation. Collagen gradually decreased with time. Elastin fiber fragments (smaller than the implanted elastin fibers) were found from day 7 on in COL-ELfiber. At day 21, less elastin staining and more elastin fragments were observed in these scaffolds. In the same scaffold, thinner and fragmented collagen structures were visible mainly at the periphery of the scaffolds from day 7 on.

At day 21, degraded collagen was also found more centrally, whereas only minor amounts of fragmented collagen were found in COL. Elastin and collagen degradation in COL-ELfiber and COL was consistent with that found in previous studies.\(^{13}\)

### Collagen formation

Generally, most staining for rat type I and type III collagen was found in COL-ELsol, somewhat less in COL-ELfiber, and least in COL. In all scaffolds, staining for type I and III collagen started in the fibrous capsule and at the periphery of the scaffolds from day 7 on (results not shown). In general, new rat collagen fibers aligned with original scaffold components. In COL-ELsol, flattened cells aligned with the lamellar scaffold structures, and this was accompanied by extracellular matrix formation (Fig. 5C). Type IV collagen staining was present in blood vessels as shown under vascularization of scaffolds (Fig. 4).

### Elastic fiber formation

At day 21, COL-ELsol showed most new rat elastin, not only in blood vessels, but also as thread-like structures within the scaffold (Fig. 6). In COL-ELfiber, rat elastin was found mainly in blood vessels present in the capsule around

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**Table 3. Overview of Immunostaining Results of Explants for Scaffold and Rat Extracellular Matrix Components**

<table>
<thead>
<tr>
<th>Scaffold</th>
<th>Days after implantation</th>
<th>Scaffold elastin</th>
<th>Scaffold collagen</th>
<th>Rat elastin</th>
<th>Rat type I collagen</th>
<th>Rat type III collagen</th>
</tr>
</thead>
<tbody>
<tr>
<td>COL</td>
<td>3</td>
<td>–</td>
<td>++</td>
<td>–</td>
<td>sp</td>
<td>–</td>
</tr>
<tr>
<td></td>
<td>7</td>
<td>–</td>
<td>++</td>
<td>sp</td>
<td>±</td>
<td>±</td>
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<tr>
<td></td>
<td>21</td>
<td>–</td>
<td>+±</td>
<td>sp</td>
<td>±</td>
<td>±</td>
</tr>
<tr>
<td>COL-ELfiber</td>
<td>3</td>
<td>++</td>
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Events were scored ranging from sporadic (sp) to abundant (++). -: not present.

**FIG. 5.** (A–B) Elastin Van Gieson–stained paraffin sections of collagen with solubilized elastin (COL-ELsol) scaffolds shows that ELsol spheres from the scaffold are still present 21 days after implantation in young Sprague-Dawley rats. Within the scaffolds, elastin spheres (arrows) are still quite large (A), but at the periphery of the scaffolds, the elastin spheres are smaller (B). Elastin Van Gieson stains elastin black and collagen pink or red. Bars represent 20 μm. (C) Semi-thin epon sections of crosslinked COL-ELsol scaffolds that were implanted for 7 days in young Sprague-Dawley rats stained with toluidine blue and basic fuchsin. Flattened cells aligned with the scaffold lamellar structures and were accompanied by extracellular matrix formation. Cells stain blue, new extracellular matrix stains light pink, and scaffold material stains dark pink. Bars represent 10 μm. Color images available online at www.liebertpub.com/ten.
the implant, and small amounts of thin elastic fibers were found sporadically at the periphery of the scaffolds. In COL, rat elastin was present only in blood vessels in the capsule.

In blood vessels, rat elastin colocalized with fibrillin-1 and fibrillin-2 staining. Fibrillin-2 staining was mainly present in blood vessels (Fig. 6J–L), but not all blood vessels contained newly formed elastin (Fig. 6G–I). Thin fibrillin-1 fibers were formed mainly in COL-ELsol, to a lesser extent in COL-ELfiber, and scarcely in COL (Fig. 6D–F). To some extent, these thin fibers showed colocalization with rat elastin (Fig. 6C, F). Fibrillin-1 staining was found earlier in time than newly synthesized elastin (results not shown) and was more abundant than rat elastin staining (Fig. 6C, F).

**DISCUSSION**

In biomaterials, some principal difficulties are observed, including limited vascularization and poor elastogenesis.2,35

With regard to the application of elastin as a biomaterial, another difficulty arises because elastin tends to calcify.13,36

To induce vascularization and tissue formation, an initial tissue reaction seems to be necessary. COL scaffolds show less reaction than COL-ELfiber or COL-ELsol, and little tissue formation was observed after 3 weeks. Tissue reaction is also dependent on the animal model used. In a previous study, we showed that (young and adult) Sprague-Dawley rats showed more tissue reaction to subcutaneously implanted scaffolds than (adult) Wistar rats.13 As a consequence, more vascularization and collagen production was observed in the Sprague-Dawley rats.13,37 In this study, COL-ELsol gave more tissue reaction than COL-ELfiber, and vascularization and tissue formation was even better in COL-ELsol scaffolds. For example, in normal wound healing of the skin, chemotactic signals recruit inflammatory cells to the wound site, initiating the process of reepithelialization and connective tissue contraction and stimulating the angiogenic response. It is important that this tissue reaction, including the presence of neutrophiles, does
not persist over time, because it is an indication of a grossly infected wound. In COL-EL_{sol} scaffolds, neutrophiles were found only sporadically at day 7. Soluble elastin seems to be able to trigger a cascade for angiogenesis and tissue regeneration. Robinet et al. recently demonstrated that κ-elastin (solubilized elastin prepared using potassium hydroxide treatment) triggered angiogenesis by promoting cell migration and tubulogenesis of human vascular endothelial cells through the elastin receptor.

Elastin synthesis is often an obstacle in tissue engineering (e.g., dermal substitutes). In this study, COL-EL_{sol} scaffolds were, in particular, able to stimulate the synthesis of elastic fibers in vivo, especially as thread-like structures to which fibrillin-1 staining colocalized. Additional fibrillin-1 staining was found surrounding these structures, suggesting that fibrillin-1 synthesis preceded elastin deposition and that elastin deposition was still in progress. Fibrillin-2 colocalized mainly with newly formed elastic fibers in blood vessels and not with loose thread-like elastic fibers found in COL-EL_{sol}. From mice experiments, it has been suggested that fibrillin-2 directs elastogenesis during embryogenesis, whereas fibrillin-1 is more important in tissue homeostasis. Our experimental setup may resemble tissue regeneration rather than embryogenesis. Furthermore, our results indicate that fibrillin-2 may be more involved in cardiovascular aspects, whereas fibrillin-1 may be more significant in skin. Another study in which skin biopsies were taken from healthy volunteers suggests a similar phenomenon; fibrillin-1 was the major contributor to dermal elastic fiber formation during acute wound repair, whereas fibrillin-2 was expressed only in wounds of the aged, and expression was confined to areas proximal to dermal blood vessels. Raghunath et al. also found fibrillin-1 preceding elastin deposition in new skin developing from keratinocyte autografts. Fibrin-1 may be the template for elastic fiber synthesis in thread-like (skin-like) elastic fibers, whereas fibrillin-2 may be the template for elastogenesis in blood vessels. However, time-resolved expression patterns of fibrillin-1 and −2 would be necessary to confirm this. Solubilized elastin may be a means to enhance elastic fiber synthesis. It has been suggested that elastin peptides stimulate elastin synthesis through the receptor. In a porcine skin excision model, improved extracellular matrix remodeling (including elastin regeneration) was found with a collagen–solubilized elastin dermal substitute. In a clinical study, such a matrix was used in 10 patients as a dermal substitute in severe burn injuries of the aged, and expression was confined to areas proximal to dermal blood vessels. Raghunath et al. also found fibrillin-1 preceding elastin deposition in new skin developing from keratinocyte autografts. Fibrin-1 may be the template for elastic fiber synthesis in thread-like (skin-like) elastic fibers, whereas fibrillin-2 may be the template for elastogenesis in blood vessels. However, time-resolved expression patterns of fibrillin-1 and −2 would be necessary to confirm this. Solubilized elastin may be a means to enhance elastic fiber synthesis. It has been suggested that elastin peptides stimulate elastin synthesis through the receptor. In a porcine skin excision model, improved extracellular matrix remodeling (including elastin regeneration) was found with a collagen–solubilized elastin dermal substitute. In a clinical study, such a matrix was used in 10 patients as a dermal substitute in severe burn injuries of the aged, and expression was confined to areas proximal to dermal blood vessels. Raghunath et al. also found fibrillin-1 preceding elastin deposition in new skin developing from keratinocyte autografts. Fibrin-1 may be the template for elastic fiber synthesis in thread-like (skin-like) elastic fibers, whereas fibrillin-2 may be the template for elastogenesis in blood vessels. However, time-resolved expression patterns of fibrillin-1 and −2 would be necessary to confirm this. Solubilized elastin may be a means to enhance elastic fiber synthesis. It has been suggested that elastin peptides stimulate elastin synthesis through the receptor. In a porcine skin excision model, improved extracellular matrix remodeling (including elastin regeneration) was found with a collagen–solubilized elastin dermal substitute.

Calcification is an undesirable phenomenon in soft biomaterial application. Young Sprague-Dawley rats have proven to be a sensitive model for studying calcification. With COL-EL_{sol} scaffolds, we could not detect any calcification in the time frame analyzed, whereas COL-EL_{fiber} showed calcification starting at insoluble elastin fibers. This effect was not due to the presence of fewer macrophages and giant cells in COL-EL_{sol} (and therefore a diminished release of extracellular enzymes involved in elastin degradation). Negative charges from C-terminal carboxyl groups may be involved in preventing positively charged calcium ions from precipitating, but other mechanisms cannot be excluded based on this study alone. Others have observed calcification of solubilized elastin preparations. In a similar rat model, Singla and Lee found calcification with collagen–κ-elastin films stabilized using glutaraldehyde fixation, but this treatment increases calcification of biomaterials. In a cranial lesion in adult rats, a polypentapeptide based on elastin with an amino acid sequence of (Val-Pro-Gly-Va-Gly)$_n$, was also able to initiate calcification in vivo, but it only calcified in a rabbit tibial non-union model with $n > 200$. In conclusion, COL-EL_{sol} scaffolds provide a non-calcifying biomaterial that stimulates angiogenesis and extracellular matrix formation (collagens and elastic fibers) and may be useful in soft tissue engineering.

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