RESEARCH ARTICLE

A FRET-based biosensor for measuring Ga13 activation in single cells

Marieke Mastop¹, Nathalie R. Reinhard¹, Cristiane R. Zuconelli², Fenna Terwey¹, Theodorus W. J. Gadella Jr.¹, Jakobus van Unen¹*¹, Merel J. W. Adjobo-Hermans², Joachim Goedhart¹*

¹ Swammerdam Institute for Life Sciences, Section of Molecular Cytology, van Leeuwenhoek Centre for Advanced Microscopy, University of Amsterdam, Amsterdam, The Netherlands, ² Department of Biochemistry, Radboud Institute for Molecular Life Sciences, Radboud University Medical Center, Nijmegen, The Netherlands

¤ Current address: Department of Biology, Institute of Cell Biology, University of Bern, Bern, Switzerland.
* j.goedhart@uva.nl

Abstract

Förster Resonance Energy Transfer (FRET) provides a way to directly observe the activation of heterotrimeric G-proteins by G-protein coupled receptors (GPCRs). To this end, FRET based biosensors are made, employing heterotrimeric G-protein subunits tagged with fluorescent proteins. These FRET based biosensors complement existing, indirect, ways to observe GPCR activation. Here we report on the insertion of mTurquoise2 at several sites in the human Ga13 subunit, aiming to develop a FRET-based Ga13 activation biosensor. Three fluorescently tagged Ga13 variants were found to be functional based on i) plasma membrane localization and ii) ability to recruit p115-RhoGEF upon activation of the LPA2 receptor. The tagged Ga13 subunits were used as FRET donor and combined with cp173Venus fused to the Gγ2 subunit, as the acceptor. We constructed Ga13 biosensors by generating a single plasmid that produces Ga13-mTurquoise2, Gβ1 and cp173Venus-Gγ2. The Ga13 activation biosensors showed a rapid and robust response when used in primary human endothelial cells that were exposed to thrombin, triggering endogenous protease activated receptors (PARs). This response was efficiently inhibited by the RGS domain of p115-RhoGEF and from the biosensor data we inferred that this is due to GAP activity. Finally, we demonstrated that the Ga13 sensor can be used to dissect heterotrimeric G-protein coupling efficiency in single living cells. We conclude that the Ga13 biosensor is a valuable tool for live-cell measurements that probe spatiotemporal aspects of Ga13 activation.

Introduction

G-protein coupled receptors (GPCRs) are members of a large family of membrane located receptors, with around 750 genes encoding a GPCR identified in the human genome [1]. These seven transmembrane containing proteins can perceive a wide variety of signals including light, hormones, ions and neurotransmitters [2]. GPCRs act as Guanine Exchange Factors (GEFs) [3] for heterotrimeric G-proteins. These protein complexes are comprised of a Ga, Gβ
and Gγ subunit. The heterotrimer is a peripheral membrane protein complex due to lipid modification of the Gα and Gγ subunit [4].

The GEF activity is exerted on the Gα subunit, which can be converted from an inactive GDP-bound state to an active GTP-bound state [5]. The activation of the complex results in a conformational change and in some cases the dissociation of the Gα subunit from the Gβγ dimer [2,6,7]. Both the activated GTP-bound Gα subunit and Gβγ dimer are capable of activating downstream effectors [2].

Almost twenty different Gα subunits can be discerned and these are grouped in four classes; Gi/o, Gs, Gq and G12/13 [2]. Throughout this manuscript we will use Gα13 to indicate the subunit and G13 to indicate the heterotrimer, consisting of Gα13, Gβ and Gγ, the same terminology will be used for Gq/Gαq and Gi/Gαi, respectively. Each class of Gα subunits activates different downstream effectors [5]. The best characterized effectors of the Gα12/Gq13 subunits are RhoGEFs that activate RhoA, e.g. LARG, PDZ-RhoGEF and p115-Rho-GEF [8,9]. For quite some time, it was thought that GPCR activation of the Gα12/Gq13 subunits was the predominant way to activate RhoA. This view has changed over the last decade with the identification of RhoGEFs that can be activated by Gαq [9,10]. Nowadays, it is clear that both Gαq and Gα12/Gα13 can rapidly activate RhoA signaling in cells [11,12], albeit by activating different effectors. Since the Gq class and G12/13 class both efficiently activate RhoA, it has been difficult to distinguish which of these two heterotrimeric G-protein complexes is activated when only downstream effects are measured. To further complicate matters, GPCRs that activate G12/13 often activate Gq as well [13,14]. Yet, it is clear that signaling through either Gq or G12/13 has different physiological effects [13,15,16]. Therefore, it is necessary to have tools that can measure activation of the heterotrimeric G-protein itself.

Direct observation of heterotrimeric G-protein activation has classically been performed by quantifying the binding of radiolabeled nucleotides [17]. This approach is labor-intensive, uses disrupted cells and lacks temporal resolution. Moreover, this technique is generally less suitable for Gq, Gs and G12/13, due to their low expression levels compared to Gi [18]. On the other hand, optical read-outs, often based on FRET and Bioluminescence Resonance Energy Transfer (BRET) techniques are well suited to measure signaling activity with high temporal resolution in intact cells [19,20]. Several groups have generated BRET or FRET based biosensors for detecting events immediately downstream of activated GPCRs [20–24]. Optical biosensors that are based on heterotrimeric G-proteins are particularly suited to report on GPCR activation [25]. However, only a few optical biosensors for reporting activation of Gα12 or Gα13 have been reported.

Sauliere et al. reported a BRET based biosensor for detection of activation of Gα13 activation, enabling the detection of biased-agonism via the angiotensin II type 1 receptor (AT1R) [26]. The approach, however, lacks spatial resolution. Improved luciferases, such as Nanoluciferase, enabled single cell BRET measurements, but longer acquisition times are required, so temporal resolution is decreased [27]. In general, FRET-based sensors have higher emission intensities, requiring shorter acquisition times to obtain sufficient spatial and temporal resolution. Thus, development of a FRET based biosensor reporting on the activation of Gα13 would be a real asset for GPCR signaling research. We have previously reported on single plasmid systems that enable the expression of a multimeric FRET based sensor for Gαq and Gαi [28,29]. Here, we report on the development, characterization and application of a single plasmid, FRET based biosensor for the activation of Gα13.
Results

Strategy for tagging \( \alpha_{13} \) with a fluorescent protein

To directly measure the activation of \( \alpha_{13} \) with high spatiotemporal resolution in living cells, we aimed at generating a functional, fluorescent protein (FP) tagged \( \alpha_{13} \) subunit. \( \alpha \) subunits cannot be tagged at the N- or C-terminus since these are required for interaction with the \( \beta\gamma \) subunit and the GPCR [30]. To functionally tag \( \alpha_{13} \), the FP should be inserted in the \( \alpha_{13} \) sequence, as was previously done for other \( \alpha \) isoforms [25,31].

Initially, we used a sequence alignment of the four classes of \( \alpha \)-proteins and identified the residues of \( \alpha_{q} \) [32] and \( \alpha_{i} \) [29] after which we had previously inserted mTurquoise2 (Fig 1B, S1 Fig). Based on sequence homology, we chose to insert mTurquoise2 after residue Q144 of human \( \alpha_{13} \), indicated with a black rectangular box in the alignment. Upon transfection of the plasmid encoding this variant, we observed cytoplasmic fluorescence. This localization probably reflects incorrect folding or targeting of the \( \alpha \) subunit, since well-folded and functionally tagged variants are located at the plasma membrane [31,32]. Inspection of the crystal structure (PDB ID: 1ZCB), revealed that Q144 is part of an \( \alpha \)-helix (\( \alpha_{B2} \)), which is likely to be disrupted after modification or insertion [33].

Next, we used the protein structure to select a number of residues that were nearby previous insertion sites and next to or close to the end of an \( \alpha \)-helix (\( \alpha_{A} \), \( \alpha_{B2} \) or \( \alpha_{B1} \)). We also took along an insertion site (L106) that was previously used to insert a luciferase into \( \alpha_{13} \) [26]. We used a truncated mTurquoise2, deleting the last 9 amino acids, since this worked well in the Gi sensor [29]. The insertion sites are highlighted on the protein structure and in the sequence alignment in Fig 1A and 1B. The different variants are numbered as \( \alpha_{13.1} \), \( \alpha_{13.2} \), \( \alpha_{13.3} \), \( \alpha_{13.5} \) and \( \alpha_{13.6} \) throughout the manuscript.

The plasmids encoding the different tagged variants were transfected into HeLa cells and we observed striking differences in localization. As shown in Fig 1C, variant 1 and 6 showed cytoplasmic localization. In contrast, strong plasma membrane labeling was observed for variant \( \alpha_{13.2} \), \( \alpha_{13.3} \) and to a lesser extent for \( \alpha_{13.5} \). Since native \( \alpha_{13} \) is expected to localize at the plasma membrane by virtue of palmitoylation [4], we decided to continue with the optimization and characterization of variants 2, 3 and 5.

Functionality of the tagged \( \alpha_{13} \) variants

The correct localization of the tagged \( \alpha_{13} \) variants does not necessarily reflect functionality with respect to activity in signaling, i.e. the capacity to exchange GDP for GTP. To determine functionality, we turned to a dynamic cell-based assay. This assay is based on the observation that ectopic \( \alpha_{13} \) expression is required for p115-RhoGEF relocation to the plasma membrane upon GPCR stimulation [34]. To evaluate the functionality of \( \alpha_{13} \), we co-expressed the LPA2 receptor-P2A-mCherry [22], p115-RhoGEF, tagged with SYFP1, and different variants of \( \alpha_{13} \), including an untagged, native variant (Fig 2, S2 Fig). Cells in which \( \alpha_{13} \) was not over-expressed did not show p115-RhoGEF relocation after GPCR activation (Fig 2B and 2C). However, in the presence of native \( \alpha_{13} \), a relocation of p115-RhoGEF was noticed (Fig 2B and 2C). These findings are in agreement with previous findings and show that a functional \( \alpha_{13} \) is required for the recruitment of p115-RhoGEF to the plasma membrane. Next, similar experiments were performed in the presence of \( \alpha_{13} \) variants 2, 3 and 5, tagged with mTurquoise2Δ9. In all three cases a robust relocation of p115-RhoGEF was observed (Fig 2). In contrast, the relocation was not evident when a \( \alpha_{13} \) variant (variant 1) was employed that did not show efficient plasma membrane localization (Fig 2B and 2C). Hence, we observed a correlation between membrane localization and functionality in the recruitment assay. Altogether,
A FRET biosensor for measuring Ga13 activation in single cells

A) Helix:αC

Helix:αB

Helix:αA

B) Ga11 82 IAIIRAMGRKL--IDFGDSARADDARQLFVLAGAAEEGFMT-------ELAGVIKRLWK 132
Gaαq 88 QAMIRAMDTLK--IPYKYEHNKAHAQLVREVDVEKVSAFEN-------FVYDAIKSLWN 137
Gaαs 104 ETIVAAMSNLVPVELNPENGFRVDYILSMVPNVPDFPDPP-------EFYEHAKALWE 155
Ga13 97 RVVDAKREKH--IPWGDNSSNQHGDKMMSFDTERPMAAQMVMETFVFFYAIRALWA 154
Tagged Ga13 variant 1

-------αA-------

---------αB-------

---------αB1-------

---------αB2-------αC-------

C) Ga13.1-mTurquoise2-Δ9 Ga13.2-mTurquoise2-Δ9 Ga13.3-mTurquoise2-Δ9 Ga13.5-mTurquoise2-Δ9 Ga13.6-mTurquoise2-Δ9

3/67

124/134

77/92

78/109

0/17
the results support the notion that the tagged variants 2, 3 and 5 of Gα13 can be activated by a GPCR and are capable of recruiting p115-RhoGEF.

Evaluation of tagged Gα13 variants for measuring Gα13 activation

Having engineered several correctly localizing Gα13 variants capable of recruiting p115-RhoGEF, we examined whether these variants can be used to report on G13 activation. Using a FRET-based approach (as described for Gq [32]), we monitored the interaction between the different generated mTurquoise2-tagged Gα13 constructs and a Gβγ dimer, consisting of untagged-Gβ and 173cpVenus-γγ, on separate plasmids. These constructs allow acceptor (173cpVenus)–donor (mTurquoise2) FRET ratio measurements, where G13 activation results in a change in distance and/or orientation between the FRET pair, thereby inducing a FRET ratio decrease.

Here we co-expressed an untagged LPA2-receptor, with one of the three tagged Gα13 variants, untagged Gβ, and tagged Gγ. Upon LPA2-receptor activation, a FRET ratio change was observed for all three selected Gα13 variants (Fig 3A). The Gα13.2 variant showed the largest FRET ratio change and the Gα13.5 variant the lowest (Fig 3A). Some cells expressing the Gα13.3 variant showed a slower response (Fig 3A).

Recently, a FRET sensor for Gα13 was reported that employed a tagged Gα and a Gβ subunit [35]. Therefore, we also examined if tagging the Gβ subunit instead of the Gγ subunit yields a higher FRET ratio change for the best performing Gα13 variant. From Fig 3B it can be inferred that tagging the Gγ subunit with the FRET acceptor results in the highest FRET ratio change upon activation of the Gα13 via the LPA2 receptor, which is consistent with our previous observations [32].

Construction and characterization of FRET biosensors for Gα13 activity

We have previously shown for Gqα [28] and Gai [29] activation biosensors that a single expression plasmid ensures robust co-expression of the sensor components and simplifies the transfection. Since all three tagged Gα13 variants are able to report on Gα13 activation using 173cpVenus-Gγ as FRET acceptor, we developed single plasmid sensors using each of the Gα13 variants. Fig 4A shows a schematic overview of the plasmid design for a Gα13 sensor. Analysis of CFP and YFP intensities from single cells show a better correlation for the single plasmid system as compared to cells transfected with separate plasmids (Fig 4B).

As can be inferred from Fig 4C, the subcellular localization of the different Gα13 sensors expressed in HeLa cells is similar. The Gα13 variants are mainly located at the plasma membrane and Gγ is located to the plasma membrane and endomembranes, as published [28]. In Hek293T cells, however, transient expression of the Gα13.2 sensor lead to very round cells that easily detach (S3 Fig), suggesting that very high, transient expression of the sensor can result in enhanced basal Gα13 activity.

Fig 1. Insertion of a fluorescent protein at different positions in Gα13. (A) The protein structure of human Gα13 (PDB ID: 1ZCB). The highlighted residues indicate the amino acid preceding the inserted fluorescent protein. Successful sites for inserting mTurquoise2-Δ9 into Gα13 in pink and unsuccessful sites in orange. (B) A partial protein sequence alignment (full alignment see S1 Fig) of different Gα13 variants also localize to structures inside the cell, which are presumably endomembranes. The numbers in the left bottom corner of each picture indicate the number of cells that showed plasma membrane localization out of the total number of cells analyzed. The tagged Gα13 variants also localize to structures inside the cell, which are presumably endomembranes. The width of the images is 76μm.
Next, we evaluated the performance of the sensors in Human Umbilical Vein Endothelial cells (HUVEC). HUVECs are known to respond to thrombin, activating endogenous Protease Activated Receptors (PARs), which results in Gα13-RhoA signaling [11,36]. We observed no effect of ectopic sensor expression in HUVEC. When thrombin was added to HUVECs, the Gα13.2 sensor showed the most pronounced FRET change (Fig 4D). This is in line with previously reported well-defined FRET change of the Gx13.2 sensor upon S1P stimulation in HUVECs [11]. Based on the FRET ratio imaging data in HUVECs and HeLa, we selected the
Gα13.2 sensor as the Gα13 activation biosensor of choice due to its high sensitivity and robust FRET ratio change upon Gα13 activation.

Characterization of Gα13 inhibition by a GTPase activating protein

Our data show that the Gα13.2 sensor is sensitive enough to detect G13 signaling activated by endogenous thrombin receptors in HUVECs. We and others [11,37,38] have used a Regulator of G-protein Signaling (RGS) domain of p115-RhoGEF as an inhibitor of G13 signaling. The
A FRET biosensor for measuring Ga13 activation in single cells
RGS domain exhibits GTPase Activating Protein (GAP) activity [39]. However, it is unclear whether the inhibition by the RGS domain in cells is due to GAP activity or due to competitive binding of the RGS domain and downstream effectors to Go13. In the latter case, we would expect a change in FRET ratio in the presence of the RGS domain. To gain insight in the mechanism of action, we employed the Go13.2 sensor and co-expressed a membrane bound RGS (Lck-mCherry-p115-RGS), which is shown to effectively inhibit RhoA activation [11].

In the presence of the RGS domain, we did not observe a FRET ratio change of the Go13.2 sensor after adding thrombin to HUVECs (Fig 5A and 5B and S1 Movie). In the control sample (Lck-mCherry) we did observe a ratio change of the Go13.2 sensor induced by thrombin (Fig 5A and 5B and S2 Movie), while resting state FRET ratios were similar for both conditions. The lack of a FRET response in presence of the RGS domain, reflecting suppression of active GTP-bound Go13, provides evidence that GAP activity is involved in the inhibitory effect of the RGS domain. Additionally, we looked into thrombin-induced contraction of HUVECs and show that over-expression of the RGS domain prevents cell contraction, even leading to an overall increase in cell area (Fig 5C and S3 Movie). Together, these data show that the RGS domain inhibits the activation of Go13 and the consequent activation of RhoA which effectively blocks cell contraction.

Application of the Go13.2 biosensor in GPCR activation assays

Published data on GPCRs coupling to Go13 is often based on indirect measures and since downstream signaling effects overlap with the downstream signaling effects of Goq, it is difficult to draw solid conclusions about the involvement of either subunit [14]. Our novel FRET sensor enables direct observation of Go13 activation. Therefore, we evaluated the Goq and Go13 responses to the stimulation of a selection of GPCRs published as coupling to Go13 [26,34,40,41]. These experiments were performed in HeLa cells transiently expressing the corresponding GPCR. As a control, cells only expressing the Go13 or Goq sensor were stimulated, which did not elicit a noticeable sensor response (Fig 6A). Upon LPA2 receptor (LPA2R) stimulation, Goq and Go13 were both activated, which corresponds to published data. Of note is that a number of cells (47 out of 60 for Goq and 23 out of 37 for Go13), transiently expressing the LPA2 receptor, failed to show a Go13 or Goq response (Fig 6B). Upon Angiotensin II type 1 receptor (AT1R) stimulation a notable response of the Goq sensor is observed as compared to a minimal response of the Go13 sensor, which is similar to the control (compare Fig 6C and 6A). The Kisspeptin receptor (KissR or GPR54) showed a clear Goq and no Go13 sensor response upon stimulation (Fig 6D). Together, these results indicate that the LPA2R couples to both Goq and Go13, while the AT1R and KissR are coupled to Goq and hardly or not to Go13. Moreover, it shows that our novel Go13 sensor can indeed be used to distinguish between Go13- and Goq-coupled GPCR signaling.

Discussion

The combined activation of different heterotrimeric G-protein classes by a GPCR defines which signaling networks will be activated. For one of the classes of G-proteins, G12/13, it has
A FRET biosensor for measuring Gα13 activation in single cells

A)

YFP/CFP Ratio

1U/ml Thrombin

Control

+ RGS

Normalized Intensity (a.u.)

1U/ml Thrombin

Control

+ RGS

Time (s)

B)

Control

+ RGS

C)

Δt=1230s

ΔArea= -22%

ΔArea= 4%

Cell area change (%)
been notoriously difficult to measure its activation. Here, we report on the development, characterization and application of a FRET based biosensor for \( \text{G}_{\alpha13} \) activation. This novel tool can be used to study the activation of \( \text{G}_{\alpha13} \) by GPCRs in single living cells. We furthermore

Fig 5. Effects of the \( \text{p115-RhoGEF RGS} \) domain on \( \text{G}_{\alpha13.2} \) activity and cell morphology. (A) Normalized ratiometric traces (upper graphs) and corresponding YFP and CFP traces (lower graphs) (dotted lines depict 95% CI) of HUVECs that were transfected with either the \( \text{G}_{\alpha13.2} \) FRET sensor and Lck-mCherry (Control, \( n = 11 \)) or the \( \text{G}_{\alpha13.2} \) FRET sensor and Lck-mCherry-\( \text{RGS} \) (+ RGS, \( n = 13 \)). Cells were stimulated at \( t = 110s \). (B) Ratiometric images of representative cells measured in (A). Cool colors represent low YFP/CFP ratios, corresponding to emission ratios (ERs) on the right. (C) Cell area change of the cells measured in (B), visualized according to the LUT panel on the right. Dotplots on the right represent individual measurements (± 95% CI) of corresponding cells measured in (A). Image width = 54μm.

https://doi.org/10.1371/journal.pone.0193705.g005

Fig 6. Direct observation of \( \text{G}_{\alpha13} \) and \( \text{G}_{\alpha q} \) activation by different GPCRs. Normalized ratio-metric FRET traces of HeLa cells transfected with the \( \text{G}_{\alpha q} \) sensor (grey line) or the \( \text{G}_{\alpha13.2} \) sensor (black line) (dotted lines depict 95% CI). (A) As a control, cells expressing only the \( \text{G}_{\alpha q} \) (\( n = 37 \)) or \( \text{G}_{\alpha13.2} \) (\( n = 20 \)) sensor were measured. Agonists were sequentially added after 50s, 150s and 230s of imaging. (B) Ratio traces of cells transfected with an untagged LPA2 receptor next to the \( \text{G}_{\alpha q} \) (\( n = 13 \) (out of 60 in total)) or the \( \text{G}_{\alpha13.2} \) (\( n = 14 \) (out of 37 in total)), stimulated at \( t = 50s \). (C) Ratio traces of cells transfected with AngiotensinII type 1 receptor-P2A-mCherry next to the \( \text{G}_{\alpha q} \) (\( n = 22 \)) or the \( \text{G}_{\alpha13.2} \) (\( n = 9 \)) sensor, stimulated at \( t = 50s \). (D) Ratio traces of cells transfected with an untagged kiss-receptor next to the \( \text{G}_{\alpha q} \) (\( n = 13 \)) or the \( \text{G}_{\alpha13.2} \) (\( n = 30 \)) sensor, stimulated at \( t = 50s \) (indicated with the arrowhead).

https://doi.org/10.1371/journal.pone.0193705.g006
show that the G13 sensor is sensitive enough to report on the activation of an endogenous receptor in human primary cells (HUVECs).

Thus far, the tools available to study the activation of Gα13 in single living cells have been limited. BRET-based strategies have been used to study activation of the G12 class. To this end, Renilla reniformis luciferase (Rluc) was inserted in Gα13 after residue Ile 108 [42] or Leu 106 [26]. However, we find that insertion of mTurquoise2 after residue Leu 106 (Gα13.1) does not result in a functionally tagged subunit, possibly because Leu106 is part of an α-helix.

Three of the five evaluated mTurquoise2 insertion sites resulted in plasma membrane localized, tagged Gα13, which were able to recruit p115-RhoGEF to the plasma membrane. The cytoplasmic-localized, tagged Gα13.1 variant was not able to recruit p115-RhoGEF, indicating that plasma membrane localization is required for functionality. Since all functional Gα13 variants could report on G13 activation as determined by FRET ratio-imaging, we developed single plasmid sensors for these three variants. In HeLa cells the localization is as expected, Gα13 at the plasma membrane and Gγ at the plasma membrane and endomembranes. The Gα13 activation biosensors were expressed in HUVECs and could report on G13 activation via endogenous Protease Activated Receptors (PARs). The Gα13.2 sensor is the best performing Gα13 biosensor, based on its sensitivity and magnitude of the FRET ratio change upon activation. Further improvement of the sensors might be achieved by varying FRET pairs [43] or changing their relative orientation by circular permutation [44].

While our manuscript was in preparation, another mTurquoise2 tagged Gα13 variant was reported [35]. In that study, the fluorescent protein was inserted after residue 127 of Gα13, closely resembling our Gα13.2 variant, and it showed plasma membrane localization. Moreover, Bodmann et al. observed a FRET change when an YFP tagged Gα13 variant was used in combination with a CFP tagged Gβ subunit to report on the activation of the thromboxane A2 receptor [35]. The independent observation of a FRET change using a similar tagged Gα13 variant, supports our notion that the Gα13.2 FRET based biosensor is a valuable tool for studying the activation of Gα13.

An advantage of our FRET sensor is that a higher ratio change is detected than for the sensor reported by Bodmann et al. 2017. While they detected a maximal FRET ratio change of 10%, we could reach a FRET ratio change of up to 25% (Fig 3). This might be due to using a tagged Gβ instead of Gγ subunit, since we also observe a lower FRET ratio change when a tagged Gβ is employed (Fig 3B). It is remarkable that Bodmann et al. detect a FRET increase upon Gα13 stimulation (increased YFP, decreased CFP intensity) whereas we detect a FRET decrease upon Gα13 stimulation (Fig 3B). All of the G-protein sensors reported by us (Gαq, Gαi1,2,3 and Gα13) show a FRET decrease upon activation under all conditions tested thus far [11,29,32], consistent with a dissociation of Gα and Gβγ subunits. Moreover, Gα13 subunits, tagged at different sites (Gα13.2, Gα13.3 and Gα13.5) all show a FRET decrease (Fig 3). One notable difference is that we use a donor tagged Gα13 and Bodmann et al. use an acceptor (YFP) tagged Gα13. However, it is unclear how this difference would lead to opposite changes in FRET upon activation and as such, we do not have a solid explanation for the differences in FRET change observed by Bodmann et al. [35] and in this study.

An advantage of the sensor that we constructed, is that it enables the simultaneous production of the three proteins that comprise the heterotrimer from a single plasmid and that the donor and acceptor are present at a well-defined stoichiometry [28]. This is evident from the better correlation between CFP and YFP emission intensities as compared to transfection of separate plasmids (Fig 4B). Moreover, the single plasmid system simplifies the distribution and application of the sensor. Especially in primary cells, such as HUVECs, it is more complicated to obtain simultaneous protein expression from multiple plasmids, whereas transient expression of the single sensor plasmid in HUVECs was efficient.
The RGS domain of p115-RhoGEF effectively inhibits GPCR-\(\Gamma_{12/13}\) mediated RhoA activation in endothelial cells [11] and cell contraction as shown in Fig 5C. Under these conditions, the \(\Gamma_{13.2}\) sensor did not display a FRET ratio change, reflecting a lack of activation. The absence of a FRET change is consistent with the idea that the GAP activity of the RGS domain shuts down \(\Gamma_{13}\) activity [39].

Applying the \(\Gamma_{13.2}\) sensor in HeLa cells, we showed that both \(\Gamma_{13}\) and \(\Gamma_q\) are activated via the LPA2 receptor. In contrast, the Kiss receptor and the AT1 receptor elicited predominantly a \(\Gamma_q\) sensor response. From our data it is not possible to judge whether the minor response of \(\Gamma_{13}\) upon AT1 receptor activation is biologically relevant. The GPCRs analyzed in this study, were reported as coupling to \(\Gamma_{13}\) and/or \(\Gamma_q\) in other studies[26,34,40,41]. Of note, transient expression of the LPA2 receptor shows several non-responders in terms of \(\Gamma_q\) or \(\Gamma_{13}\) activity. This could be explained by insufficient levels of receptor to achieve detectable activation.

Strikingly, the Kiss receptor did not activate the \(\Gamma_{13}\) biosensor, indicating that aspecific, promiscuous coupling of a GPCR to an ectopically expressed G-protein biosensor is not detected. Conversely, we previously observed that HUVEC treated with S1P do show \(\Gamma_{13}\) activation, but no \(\Gamma_q\) activation [11]. Together, these observations suggest that our FRET based biosensor toolkit provides a way to determine GPCR coupling selectivity towards heterotrimeric G-proteins in living cells. It would be advisable to complement such studies with more downstream read-outs to verify the possible perturbation by the ectopically expressed G-protein sensors.

In summary, the results obtained in this study point out that the \(\Gamma_{13.2}\) biosensor is a sensitive \(\Gamma_{13}\) activation sensor for live cell imaging, that is suitable for application in primary cells and able to detect endogenous GPCR activation.

**Material & methods**

**Cloning/plasmid construction**

mTurquoise2-\(\Delta 9\) was inserted in the \(\Gamma_{13}\) sequence using a previously reported strategy [29]. A PCR was performed on the mTurquoise2 sequence to truncate it and flank it with AgeI sites using primers Fw 5′-ATACCGGTTCATATCCCTGGGAGACAAC-3′ and Rv 5′-TAAACCGGTGATCCCGGGCGG-3′. To determine at which positions we wanted to insert mTurquoise2 in G\(\alpha\)13, we used Pymol to look at the structure of G\(\alpha\)13 and we used ClustalW to make an alignment of multiple G\(\alpha\) classes. A whole-vector PCR was performed on a pcDNA vector encoding human G\(\alpha\)13 (ordered from cDNA.org) to introduce an AgeI restriction site at the spot where we wanted to insert mTurquoise2, using primers Fw 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ and Rv 5′-ATACCGGTAAAGCTCTCTTGAGCAGCATCAAC-3′ for G\(\alpha\)13.1, primers Fw 5′-ATACCGGTGCCCATGCAACCCCTGAGCC-3′ and Rv 5′-ATACCGGTCCGGGATCAGCGACATACCATTATC-3′ for G\(\alpha\)13.2, primers Fw 5′-ATACCGGTCCGGCCTGGGAGACACAC-3′ and Rv 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ for G\(\alpha\)13.3, primers Fw 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ and Rv 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ for G\(\alpha\)13.4, primers Fw 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ and Rv 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ for G\(\alpha\)13.5 and primers Fw 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ and Rv 5′-ATACCGGTCAATATCCCTGGGAGACACAC-3′ for G\(\alpha\)13.6. The G\(\alpha\)13 pcDNA vector including AgeI site and the mTq2 PCR product were cut with AgeI and ligated, resulting in mTurquoise2 tagged G\(\alpha\)13. Of note, the cloning of variant G\(\alpha\)13.4, with an insertion of mTurquoise2-\(\Delta 9\) after T139, failed.

We used GFP-p115-RhoGEF (a kind gift of Keith Burridge, UNC, Chapel Hill, USA) as a template to amplify p115-RhoGEF with the primers Fw 5′-AACAGATCTCTTGGTACCGCTCTCGGATC-3′ and Rv 5′-AGCGTCGACTCAAGTGCAGCCAGGCTG-3′. The PCR product,
flanked with the restriction sites BglII and Sall, was used to clone p115-RhoGEF into a clon-tech-style C1 vector, generating mVenus-p115-RhoGEF.

The untagged LPA2 receptor was ordered from cDNA.org. To create the clontech-style N1 LPA2 receptor-P2A-mCherry construct, a PCR was performed using primers Fw 5’-AGG TCTATATAAGCAGAGC-3’ and Rv 5’-TAATGCACGTTGGTGGAGCTACATCGTG-3’. The N1-P2A-mCherry construct, described previously [22] and the LPA2 receptor PCR product were digested with EcoRI and Sall and ligation resulted in the LPA2 receptor-P2A-mCherry construct.

The G13 single plasmid sensor variants were constructed as described previously by overlap-extension PCR [29,45]. The first PCRs were performed on the previously published Goq sensor [28] using primerA Fw 5’-GAAGTTTTTCTG TGCCATCC-3’ and primerB Rv 5’-GGGCCATTTATCATCGGT TTTTTCAAAG-3’. The second PCR was performed on a mix of both PCR products using primerA and primerD. This second PCR product and the Goq sensor were digested with SacI and XbaI and the PCR product was ligated into the sensor, resulting in a G13 single plasmid sensor.

Lck-mCherry-p115-RhoGEF-RGS was constructed as described before [11]. The p115-RhoGEF-RGS domain (amino acid 1–252) was PCR amplified using Fw 5’-GATTCTATATAAGCAGAGC-3’ and Rv 5’-GGGCCATTTATCATCGGT TTTTTCAAAG-3’. The PCR product and clontech-style C1 Lck-mCherry vector were digested with BglII and EcoRI and ligation resulted in a clontech-style C1 vector encoding Lck-mCherry-p115-RhoGEF-RGS.

The untagged Kiss receptor was purchased from www.cDNA.org. The rAT1aR-mVenus was a kind gift from Peter Varnai (Semmelweis University, Hungary). The coding sequence of AT1R was inserted into mCherry-N1 with a P2A peptide to obtain AT1R-P2A-mCherry.

Cell culture and sample preparation

HeLa cells (CCL-2, American Tissue Culture Collection; Manassas, VA, USA) were cultured in Dulbecco’s modified Eagle’s medium (DMEM) (Gibco, cat# 61965-059) supplemented with 10% fetal bovine serum (Invitrogen, cat# 10270-106), 100U/ml penicillin and 100 μg/ml streptomycin at 37 °C in 7% CO2. For microscopy experiments, cells were grown on 24mm Ø round coverslips, 0.13–0.16 mm thick (Menzel, cat# 360208) to 50% confluency and transfected with 500ng plasmid DNA, 1 μL Lipofectamin 2000 (Invitrogen, cat# 11668-019) or 4.5 μl PEI (1 mg/ml) in water (pH 7.3) and 100 μl OptiMEM (Gibco, cat# 31985-047) per 35mm Ø dish holding a 24mm Ø coverslip. One day after transfection the coverslip was mounted in a cell chamber (Attofluor, Invitrogen). Microscopy medium (20 mM HEPES (pH = 7.4), 137 mM NaCl, 5.4 mM KCl, 1.8 mM CaCl2, 0.8 mM MgCl2 and 20 mM glucose) was added to the coverslip in the cell chamber. The ratiometric FRET experiments were performed at 37 °C.

Primary HUVECs, acquired from Lonza (Verviers, Belgium) were seeded on fibronectin (FN)-coated culture flasks. HUVECs, grown in EGM-2 medium, supplemented with single-quots (Lonza) at 37 °C in 5% CO2. For microscopy experiments HUVECs were transfected at passage #4 or #5 with a Neon transfection system (MPK5000, Invitrogen) and Neon transfection kit (Invitrogen) and grown on FN-coated 24mm Ø round coverslips, 0.13–0.16 mm thick (Menzel, cat# 360208). Per transfection, 2μg plasmid DNA was used and a single pulse was generated at 1300 Volt for 30 ms. [11]. The ratiometric FRET experiments were performed at 37 °C in EGM-2 medium and in 5% CO2.
Confocal microscopy
To obtain confocal images of live HeLa cells transiently expressing either a tagged Gα13 variant or G13 single plasmid sensor, a Nikon A1 confocal microscope, equipped with a 60x oil immersion objective (Plan Apochromat VC, NA 1.4), was used. The pinhole size was set to 1 Airy unit. To check the localization of tagged Gα13 variants, samples were excited with a 457nm laser line, a 457/514 dichroic mirror was used and the emission was filtered through a 482/35BP filter. To check the localization of the G13 single plasmid sensor constructs, samples were excited with a 440nm (CFP) and a 514nm (YFP) laser line, a 457/514 dichroic mirror was used and the emission was filtered through a 482/35BP (CFP) or 540/30BP (YFP), respectively. Images were acquired with sequential line scanning modus, to avoid bleedthrough.

p115-RhoGEF recruitment assay
For the p115-RhoGEF recruitment assay, HeLa cells were cultivated in RPMI medium supplemented with 10% fetal calf serum and L-Glutamine (2 mM) (PAN Biotech GmbH, Aidenbach, Germany) and kept at 7˚C in a 5% CO₂ atmosphere. Cells were harvested, and 50,000 cells/well were seeded in eight-well μ-slides (Ibidi). After 24 hours, cells were transiently transfected with 0.25 μg of the LPA2receptor-P2A-mCherry, the SYFP1-p115-RhoGEF and the Gα13 variants tagged with mTurquoise2 (Gα13.1, Gα13.2, Gα13.3, Gα13.5). Transfection of HeLa cells was performed using Lipofectamine 3000 and Plus Reagent, according to the manufacturer’s instructions (Invitrogen). Twenty-four hours after transfection, the growth medium was replaced by RPMI phenol red-free medium and measurements were performed after a total incubation time of 48h. Throughout the measurements, cells were kept at 37˚C. Cells were stimulated with Oleoyl-L-α-lysophosphatic acid (10 μM, Sigma) at the indicated time point. Confocal images were taken with a Leica TCS SP5 laser scanning confocal microscope (Leica Microsystems, Mannheim, Germany) equipped with an HCX PL APO 63×, N.A. 1.2, water immersion lens. mTurquoise2 was excited at 458 nm and emission was detected between 465–500 nm; SYFP1 was excited at 514 nm and emission was detected between 520–550 nm; mCherry was excited at 561 nm and emission was detected between 600–670 nm. To avoid bleedthrough, images were acquired in the sequential line scanning modus. Image analysis was performed with Fiji.

Widefield microscopy
Ratiometric FRET imaging HeLa cells. Ratiometric FRET experiments were performed on a wide-field fluorescence microscope (Axiovert 200 M; Carl Zeiss GmbH)[32] equipped with a xenon arc lamp with monochromator (Cairn Research, Faversham, Kent, UK) and Metamorph 6.1 software, for 240s or 288s (controls in Fig 6A) and with a time interval of 2s. The fluorescence intensity of the donor and acceptor were recorded with an exposure time of 200ms per image using a 40x objective (oil-immersion Plan-Neo-fluo 40×/1.30; Carl Zeiss GmbH). HeLa cells were used, expressing cp173Venus-Gγ (or untagged Gγ in Fig 3B), untagged Gβ (or mVenus tagged Gβ in Fig 3B) and one of the mTurquoise2 tagged Gα13 variants from multiple plasmids or expressing the single plasmid Gq-sensor or one of the G13 sensor variants. A GPCR is expressed from a separate plasmid, which was either untagged LPA2 receptor, untagged Kiss receptor or AngiotensinII type 1 receptor-P2A-mCherry. Fluorophores were excited with 420 nm light (slit width 30 nm), mTq2 emission was detected with the BP470/30 filter, YFP emission was detected with the BP535/30 filter and RFP emission was detected with a BP620/60 filter by turning the filter wheel. After 50 s HeLa cells (unless stated otherwise) were stimulated with either a final concentration of 3μM LPA (Sigma), 100nM Kiss-1 (112–121) Amide (Phoenix pharmaceuticals) or 10μM angiotensin (Sigma). The curves were normalized to the average
intensity of the first 5 frames that were recorded. ImageJ was used to perform a background correction and calculation of mean intensity of each cell for each time point. Cells that did not show a visible response were not used for the analysis. The total number of cells imaged and the number of cells analyzed (“the responders”) are indicated in the figure legends.

**Ratiometric FRET imaging HUVECs.** To perform ratiometric FRET experiments on HUVECs we used the same microscopy equipment and filter settings as were used to perform ratiometric FRET imaging of HeLa cells, however there are some differences in the way the data is recorded. The HUVECs are imaged for 1230s with a time interval of 10s and the imaging is performed at 37 °C in EGM-2 medium and in 5% CO₂. After 110s, HUVECs were stimulated with a final concentration of 1U/ml thrombin (Haematologic Technologies). The image processing procedure that was used to display the change in cell area during live cell microscopy of HUVECs is described elsewhere [11]). In order to show the FRET ratio in images of cells, ImageJ was used. We first converted the CFP and the YFP stack to 32-bit type and corrected for background signal. Then the stacks were divided to obtain a YFP/CFP stack. We used the CFP stack to make a binary mask and multiplied this mask with the YFP/CFP stack. Finally, we applied a smooth filter to reduce noise and used the lookup table (LUT) to visualize changes in FRET ratio.

**Supporting information**

**S1 Fig.** Full amino acid alignment of four classes of human Gα subunits of heterotrimeric G-proteins. Note that the amino acid sequence of Gαs is that of the short isoform. The highlighted residues indicate the amino acid preceding the inserted fluorescent protein (or luciferase). In bold, the sites that were previously used to insert Rluc (Saulière et al., 2012). Insertion of mTurquoise2-Δ9 in Gα13 after residue Q144 (black) was based on homology with previous insertions in Gαq and Gαi (black). Successful sites for inserting mTurquoise2-Δ9 (R128, A129 and R140) in pink and unsuccessful sites (L106 and L143) in orange.

(PNG)

**S2 Fig.** Confocal images of HeLa cells expressing both the Gα13.2-mTurquoise2 (left) and LPA2-p2A-mCherry (right) used in p115-RhoGEF recruitment assay (Fig 2). The width of the images is 67μm.

(PNG)

**S3 Fig.** Confocal microscopy images of Hek293T cells (left) or widefield microscopy images of HUVECs, both expressing the G13.2 sensor. The upper images show Gα13.2 localization and the lower images show Gγ localization. Hek293T cells were excited with 457nm (CFP) and 514nm (YFP) light and respectively, a 482/35BP and 540/30BP were used for detection of emission light. The width of the images is 70μm. HUVEC cells were excited with 420nm (CFP) and 490nm (YFP) light and respectively, a 470/30BP and 535/30BP were used for detection of emission light.

(PNG)

**S4 Fig.** The CFP and YFP traces of HUVECs expressing the different G13 biosensors, stimulated with 1 U/ml thrombin at t = 100s (dotted lines depict 95% CI). The number of cells analyzed is: G13.2 sensor n = 16, G13.3 sensor n = 11, G13.5 sensor n = 16.

(PNG)

**S1 Movie.** Dynamics of Gα13 activation in the presence of the Lck-mCherry-RGS, related to Fig 5B.

(AVI)
S2 Movie. Dynamics of Gα13 activation in the presence of the Lck-mCherry (control), related to Fig 5B. (AVI)

S3 Movie. Analysis of the endothelial cell area changes induced by thrombin, related to Fig 5C. (AVI)

Acknowledgments
We thank the members of our labs for their continuous interest and support of this project. The plasmid with rAT1aR-mVenus was a kind gift from Peter Várnai (Semmelweis University, Hungary) and GFP-p115-RhoGEF was provided by Keith Burridge (UNC, Chapel Hill, USA).

Author Contributions
Conceptualization: Marieke Mastop, Jakobus van Unen, Joachim Goedhart.
Funding acquisition: Theodorus W. J. Gadella, Jr., Joachim Goedhart.
Supervision: Theodorus W. J. Gadella, Jr., Joachim Goedhart.
Writing – original draft: Marieke Mastop, Joachim Goedhart.
Writing – review & editing: Joachim Goedhart.

References


