Strategies To Increase the Thermal Stability of Truly Biomimetic Hydrogels: Combining Hydrophobicity and Directed Hydrogen Bonding

Hongbo Yuan,†,§ Jialiang Xu,†,‡,§ Eliane P. van Dam,‖ Giulia Giubertoni,‖ Yves L. A. Rezus,‖ Roel Hammink,§ Huib J. Bakker,‖ Yong Zhan,† Alan E. Rowan,‖,§ Chengfen Xing,‖,‡,§ and Paul H. J. Kouwer†,§,∥

†School of Materials Science and Engineering, Hebei University of Technology, Tianjin 300401, P. R. China
‡School of Chemical Engineering and Technology, Tianjin University, Yaguan Road 135, Tianjin 300350, P. R. China
§Institute for Molecules and Materials (IMM), Radboud University, Heyendaalseweg 135, 6525AJ Nijmegen, The Netherlands
‖AMOLF, Science Park 104, 1098 XG Amsterdam, The Netherlands
∥Australian Institute for Bioengineering and Nanotechnology, The University of Queensland, Brisbane, QLD 4072, Australia

ABSTRACT: Enhancing the thermal stability of proteins is an important task for protein engineering. There are several ways to increase the thermal stability of proteins in biology, such as greater hydrophobic interactions, increased helical content, decreased occurrence of thermolabile residues, or stable hydrogen bonds. Here, we describe a well-defined polymer based on \( \beta \)-helical polysiocyanotripeptides (TriPIC) that uses biological approaches, including hydrogen bonding and hydrophobic interactions for its exceptional thermal stability in aqueous solutions. The multiple hydrogen bonding arrays along the polymer backbone shield the hydrophobic core from water. Variable temperature CD and FTIR studies indicate that, on heating, a better packed polymer conformation further stiffens the backbone. Driven by hydrophobic interactions, TriPIC solutions give fully reversible hydrogels that can withstand high temperatures (80 °C) for extended times. Cryo-scanning electron microscopy (cryo-SEM), small-angle X-ray scattering (SAXS), and thorough rheological analysis show that the hydrogel has a bundled architecture, which gives rise to strain stiffening effects on deformation of the gel, analogous to many biological hydrogels.

INTRODUCTION

To build up its architectures, nature uses well-defined structures as building blocks, such as \( \alpha \)-helices and \( \beta \)-sheets, which are the principal structural components of proteins and of the double helix of DNA. These stable, robust architectural motifs are responsible for the tertiary structure and mechanical strength and thus play a crucial role in the function of all biological systems. The stability of such structural elements is particularly important for hyperthermophilic organisms that need to survive the extra heat in their environments. The architecture of biopolymers is attractive to mimic with synthetic polymers due to their high degree of function and their potential applications in the fields of material and supramolecular sciences. Among many artificial polymers, polysiocyanopeptides (PICs) are particularly interesting because of their stable helical backbones with a high helix inversion barrier. They adopt an \( \sim \)-helical conformation stabilized by a \( \beta \)-sheet-like peptidic hydrogen bond network along the polymer backbone between monomers \( n \) and \( n + 4 \). Moreover, this helical structure plays a vital role in the high stiffness of the polymer. In earlier work, we showed that gels made of polysiocyanopeptides grafted with ethylene glycol side chains mimic biological gels and more complex cytoskeletal composites in nearly all aspects. The ultrasensitive mechanical responses of these gels are responsible for the extraordinary mechanical responses of several biological systems. These systems are responsible for the ultra-sensitive mechanical responses of several biological systems. These systems are responsible for the ultra-sensitive mechanical responses of several biological systems.

Received: August 24, 2017
Revised: November 8, 2017
Published: November 15, 2017
that these gels demonstrate originate from the network architecture of semiflexible bundles that is formed when a polymer solution is heated into the mesophilic region (37°C). Furthermore, these gels decorated with GRGDS peptides can serve as a 3D matrix to manipulate the differentiation of stem cells. To the best of our knowledge, however, very few examples of synthetic biomimetic polymers with high thermal stability have been reported. In this work, we use a truly synthetic polymer based on the helical PIC backbone and mimic thermophilic proteins using biological approaches. This model system will aid in understanding and developing the underlying design principles of thermally stable aqueous biomimetic materials or even thermophilic proteins.

The exceptional stability of oligo(ethylene glycol)-decorated polyisocyanotripeptides (TriPIC, Figure 1) is based on three adjacent alanine groups. The rigid, helical backbone of TriPIC is stabilized by two parallel well-defined hydrogen-bonding arrays between the two amide groups, which run parallel to the polyisocyanide backbone. The amide regions are partially inaccessible to water, and consequently, a hydrophobic core is constructed around the polymer backbone. On heating, the first hydrogen bond (A, NOT H2O accessible) keeps stable which mainly holds the helical architecture, whereas the second one (B) is stretched, endowing the polymer with a better defined helix and stiffer backbone. Beyond a gelation temperature, single polymers assemble and bundle into a network, driven by the hydrophobic interactions of the glycol tails, which induces an unusual thermal stability of the gels, which are stable for many hours at 80°C.

**RESULTS AND DISCUSSION**

**Polymer Synthesis and Characterization.** The synthesis of the oligo(ethylene glycol)-functionalized polyisocyanotripeptide (TriPIC) pursues a standard peptide coupling strategy, followed by subsequent dehydration and polymerization reactions [Scheme 1]. A detailed description of the synthesis and characterization (1H and 13C NMR, MS, HRMS) of the intermediate and final products is given in the Experimental Section and the Supporting Information (Figures S1–S6). The isocyanide monomers were polymerized through nickel(II)-catalyzed polymerization using ethanol as the initiator in freshly distilled chloroform. In the formation of the helix, both hydrogen bonding and steric interactions (from the methyl of the alanine group) play crucial roles. In our hands, polymers with different amino acids such as glycine or valine either did not polymerize or were unable to form self-supporting hydrogels. Here, we use the TriPIC with alanines in the L,D,L-configuration. In fact, we were unable to even polymerize the equivalent diastereomeric D,D,L-isocyanotripeptide monomer, most likely due to unfavorable steric interactions. The polymer length was regulated by adjusting the molar ratio between the catalyst and the monomer. In this way, a series of polymers with different lengths (TriPIC-a–g) were obtained. The molecular weights (M<sub>v</sub>) were estimated by viscometry based on the Mark–Houwink equation, and the apparent polymer contour length (L) was calculated based on M<sub>v</sub>.

**Figure 1.** (a) Molecular structure of the tri(ethylene glycol)-functionalized polyisocyanotripeptides (TriPIC). (b) Schematic representation of the key groups that stabilize the structure against thermal agitation.

**Scheme 1.** (a) Synthetic Route to TriPIC Polymers

<table>
<thead>
<tr>
<th>TriPIC</th>
<th>[M]/[cat.]</th>
<th>M&lt;sub&gt;v&lt;/sub&gt; (kg mol&lt;sup&gt;-1&lt;/sup&gt;)</th>
<th>n</th>
<th>L (nm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>a</td>
<td>500</td>
<td>156</td>
<td>403</td>
<td>42</td>
</tr>
<tr>
<td>b</td>
<td>1000</td>
<td>231</td>
<td>596</td>
<td>63</td>
</tr>
<tr>
<td>c</td>
<td>2000</td>
<td>373</td>
<td>963</td>
<td>101</td>
</tr>
<tr>
<td>d</td>
<td>5000</td>
<td>451</td>
<td>1164</td>
<td>122</td>
</tr>
<tr>
<td>e</td>
<td>8000</td>
<td>548</td>
<td>1404</td>
<td>149</td>
</tr>
<tr>
<td>f</td>
<td>12000</td>
<td>616</td>
<td>1593</td>
<td>167</td>
</tr>
<tr>
<td>g</td>
<td>15000</td>
<td>643</td>
<td>1660</td>
<td>174</td>
</tr>
</tbody>
</table>

Reagents and conditions: (i) HCl, EtOAc, room temperature, 2 h; (ii) L-HO-Ala-Boc, EDC·HCl, HOBt, DIPEA, room temperature, 16 h, yield = 65% for two steps; (iii) HCl, EtOAc, room temperature, 2 h; (iv) HCO$_2$Na/HCO$_2$Et, reflux, 16 h, yield = 68% for two steps; (v) diphosgene, N-methylmorpholine, CH$_2$Cl$_2$, −40 °C, 1 h, yield = 80%; (vi) Ni(ClO$_4$)$_2$·6H$_2$O, EtOH/CHCl$_3$, room temperature, 2−7 days, yield = 85%. [M]/[cat.] = monomer-to-catalyst ratio, M<sub>v</sub> = viscosity-derived molecular weight; degree of polymerization n and the polymer contour length L are calculated based on M<sub>v</sub>.
observed by atomic force microscopy (AFM, Figure S7). The results are consistent with the molecular weights ($M_w$) and the used starting conditions.

**Single Polymer Chain Stability.** The helical backbone conformation is stabilized by hydrogen-bonding arrays, and as such, water will have a large impact on the stability and the rigidity of the helix. We used H/D exchange experiments in conjunction with FTIR and ATR spectroscopy to study the solvent accessibility of the polymer core. Figure 2a shows the FTIR spectrum of TriPIC-b, together with that of its monomer, recorded in D$_2$O solution. The absorption band at 1735 cm$^{-1}$ for the amide I (which is observed for the polymer, and 1645 cm$^{-1}$ for the monomer) is shifted to 1645 cm$^{-1}$ when H$_2$O is added to the solvent whereas the band at 1645 cm$^{-1}$ is unaffected. This leads us to conclude that the two absorption bands correspond to the two types of amide groups (A and B): apparently, the amide groups closest to the helical backbone (A) absorb at 1645 cm$^{-1}$ and are solvent inaccessible, whereas the amide groups further away from the central helix (B) and close to the poly(ethylene glycol) chain, absorb at 1671 cm$^{-1}$ (in D$_2$O), and are accessible to the solvent.

**Hydrogel Formation.** Equivalent to the corresponding dipeptide polysiocyanides, 22 the TriPIC polymers display a lower critical solution temperature (LCST). Heating beyond the LCST causes the oligo(ethylene glycol) tails to dehydrate, which induce bundle formation of the polymers and the formation of hydrogels. The gelation temperature $T_{gel}$ coincides with the LCST of the aqueous polymer solution.

We studied the thermal responsiveness and stability of TriPIC hydrogels using rheological analysis (Figure 3). When an aqueous TriPIC-$f$ solution is heated in a rheometer, the storage modulus $G'$, defined as the ratio between the applied stress $\sigma$ and the measured strain $\gamma$, increases as a network is formed (Figure 3a), even at concentration as low as $c = 0.1$ g L$^{-1}$ (about 0.01 wt %). The gel stiffness is retained when the hydrogel is kept for more than 10 h at elevated temperatures $T = 80 \, ^\circ$C, which demonstrates a remarkable thermal stability. At elevated temperatures, both the storage modulus $G'$ and the loss modulus $G''$ are independent of frequency (Figure S8). We find that gelation is fully reversible (Figure S9a); cooling the sample results in a low viscous solution with minimal thermal hysteresis. Repeated heating and cooling cycles have virtually no effect on the mechanical properties of the TriPIC hydrogels (Figure S9b).

The gelation temperature, $T_{gel}$, defined as the onset point of the increase in the $G'$ as a function of the temperature, was found to be 50 $\, ^\circ$C for TriPIC-$f$, which is identical to those of the gels made of polymers with different molecular weights TriPIC-$a$-g (Figure S10a) and also those of the gels prepared at different polymer concentrations (Figure 3b). The shear modulus in the gel phase, however, increases sharply with both the concentration $c$ and the polymer contour length $L$.

Over the measured concentration regime $c = 0.1-4.0$ g L$^{-1}$, the storage modulus scales as $G' \propto c^2$, which is in line with experimental and theoretical results of the semiflexible networks. 31, 32 For such networks it is expected that at high stresses, i.e., beyond a critical stress level $\sigma_c$, the hydrogel becomes stiffer. Many biological networks, such as actin, collagen, and fibrin, display this so-called strain-stiffening behavior, which plays a key role in tissue protection and cell–cell communication and may influence other cellular functions. The nonlinear regime is readily probed by a prestress protocol, 33 where the rheometer applies a constant stress to the sample and on top of that a small oscillatory stress, yielding the differential modulus defined as $K' = \partial G'/\partial \gamma^2$.

At small deformations, $K' = G'$, but beyond a critical stress $\sigma_c$, the differential modulus scales to the applied stress $K' \propto \sigma^\eta$, where

![Figure 2](https://example.com/fig2.png)

**Figure 2.** (a) FTIR spectra of polymer TriPIC-b (blue line) and the corresponding monomer (red line) between 1300 and 1800 cm$^{-1}$ in D$_2$O at room temperature; $c = 17.0$ g L$^{-1}$. (b) ATR spectra of polymer TriPIC-b in D$_2$O (red line) and in 50/50 D$_2$O/H$_2$O (blue line) at room temperature. The different color coded absorptions are discussed in the main text.
$m$ is the stiffening index that indicates the mechanical responsiveness of the hydrogel.

Indeed, TriPIC hydrogels of different polymer length (Figure S10b) and at different concentrations (Figure 3c) clearly show strain-stiffening. At the highest concentrations (or contour length), the plateau in $K'$ is followed by a nonlinear regime with $m \approx 1$, a value similar to what is experimentally found for collagen but lower than the theoretical limit $m = 3/2$, which was found for the dipeptide PIC gels. At lower concentrations, the critical stress is so low that even below $\sigma < 1$ Pa the network already responds nonlinearly and the gel becomes progressively stiffer. In these samples, the critical stress, i.e., the threshold for the nonlinear regime, is comparable to that of biological hydrogels and are of the order to what cells can apply to their extracellular environments.

A third approach to manipulate the mechanical properties of TriPIC hydrogels is the use of salts. Commonly, the addition of salts has a significant influence on the LCST of thermoresponsive polymers and proteins, an effect known as the Hofmeister effect. In the case of TriPIC gels (Figure 3d), $T_{eq}$ decreases (linearly) with increasing the NaCl concentration, and as a result, the mechanical parameters ($K'$ and $\sigma_c$)
in the linear and the nonlinear regime can be readily tuned by adding the salts (Figure S11). The nature of the salt determines the amplitude of the Hofmeister effect and of the effect on the gel mechanics.37

Architectural Analysis. The biomimetic mechanical properties of TriPIC hydrogels are the direct result of their fibrillar or bundle architecture. Bundle formation is a design criterion in both of mesophilic and thermophilic biological hydrogel networks, which intrinsically gives rise to gels at low concentrations, with large pore sizes and with strong mechanical responses.38,39 We studied the gel architecture in situ by using cryo-scanning electron microscopy (cryo-SEM) and small-angle X-ray scattering (SAXS). Cryo-SEM images (Figure 4a, b) show a homogeneous and branched network of polymer bundles with pore sizes of the order of 100 nm at \( c = 4.0 \text{ g L}^{-1} \). Quantiﬁcation of the bundle diameter is not easy from the SEM images but can be derived from the SAXS patterns. We recorded scattering of the TriPIC-f (4 g L\(^{-1}\)) as a function of temperature (Figure 4c): at low \( T \) molecularly dissolved and beyond the LCST (50 °C) in the gel phase, where the scattering curves start to deviate. Fitting the scattering data with appropriate models allows us to extract the architectural information on the network. In solution (at \( T < T_{\text{gel}} \)), we ﬁtted the data to the semiflexible polymer model of Kholodenko (Figure 4d, red solid line), yielding a polymer diameter \( R = 1.0 \text{ nm} \) and a persistent length \( l_p = 48 \text{ nm} \). The contour length ﬁxed at 160 nm is outside the experimental window. Upon heating the sample to 70 °C, however, the curve of the scattering proﬁle changes because of bundle formation and is ﬁtted excellently by a composite Kholodenko/Ornstein–Zernike (KOZ) model (pink solid line),25 with a bundle radius \( R_B = 2.96 \text{ nm} \). The persistence length of the polymer bundles \( l_p,B \) is now outside the experimental window and is ﬁxed on 800 nm. The Ornstein–Zernike term yields a correlation length \( \xi_{\text{OZ}} = 110 \text{ nm} \) that corresponds to the average pore size of the network. The results agree markedly well to the cryo-SEM images.

Bundling is crucial in the formation of semiflexible networks and their unique properties but is still poorly understood experimentally. To obtain deep insights into the mechanism of the bundling of TriPIC polymers, we carried out temperature-dependent FTIR experiments (Figure 5a) and speciﬁcally followed the vibrations of the two hydrogen-bond-forming amide groups. Note that the hydrogen bonds formed by the amide closest to the isocyanide backbone (amide A) is thought to maintain the helical architecture of the polymer,28 while the hydrogen bonds of the second amide group (amide B) further stabilizes and stiffens the TriPIC polymer backbone. This is consistent with the present results regarding the different solvent accessibilities of these two amide groups. The intensities of the \( \text{C}==\text{O} \) stretch vibrations of both amides and the ester (Figure 5a) change with temperatures, which indicates that the local chemical environment of these groups changes as a function of temperature.

To analyze the data more quantitatively, the spectra were deconvoluted by globally ﬁtting six Gaussian peaks with peak

---

**Figure 5.** (a) FTIR spectra of the TriPIC-b in D\(_2\)O (\( c = 17.0 \text{ g L}^{-1} \)) as a function of temperature. The amide I and ester regions of the spectra were ﬁtted with six Gaussian-curves centered at 1622, 1646, 1661, 1674, 1734, and 1739 cm\(^{-1}\). Inset: the amplitude changes of amide and ester groups with temperature at 1646, 1661, 1674, 1734, and 1739 cm\(^{-1}\). At \( T_{\text{gel}} \) (dashed line), most of the intensities show an inﬁction point. (b) CD spectra of TriPIC-b as a function of temperature. (c) Evaluation of the CD signal at \( \lambda = 315 \text{ nm} \) of TriPIC-b with temperature. The CD measurements were performed in H\(_2\)O (\( c = 0.5 \text{ g L}^{-1} \)).
centers at 1622, 1646, 1661, 1674, 1734, and 1739 cm\(^{-1}\) (Figure S12 shows additional information). We fitted the amide I\(_A\) band with one Gaussian and the amide I\(_B\) band and the ester vibrational band each with two Gaussians as this allows us to model the blue-shift and broadening of the bands with increasing temperature. The areas of the Gaussians are shown in the inset. We observe that there is an inflection point at \(T_{\text{gel}} = 50\) °C, above which the intensity variation of the bands becomes stronger. Interestingly, the ester C=O and the amide I\(_B\) vibrational bands show a blue-shift with increasing temperature while the center position of the amide I\(_A\) band is independent of temperature. The ester C=O groups and part of the amide I\(_B\) groups are hydrogen-bonded to their aqueous solvation shell, and these hydrogen-bonds become weaker with increasing temperature, leading to the observed blue-shift and peak broadening of the amide I\(_A\) and ester bands. The amide A hydrogen-bond strength does not change: by the observed changes in the UV–vis vibrational bands show a blue-shift with increasing temperature of the aqueous TriPIC polymer solution or gel are fully reversible: on cooling the original spectrum is obtained again (Figure S13). As a control, we do not observe any spectral changes when heating a solution of the monomer (Figure S14).

The transition to the gel phase is also readily identified using UV–vis spectroscopy (Figure S15) and circular dichroism (CD) spectroscopy (Figure Sb). Heating the solution shows a clear step in the ellipticity \(\Delta \varepsilon = 315\) nm, right at the transition temperature \(T_{\text{gel}} = 50\) °C, which implies an increased helical content and a better-defined helical architecture are formed as a result of the stretching of the hydrogen bonds and increasingly stiffer backbones on heating. This is also supported by the observed changes in the UV–vis spectra that show a large jump in the absorbance at \(\lambda = 315\) nm. Again, these transitions are completely reversible upon cooling with minimum hysteresis effects. It is interesting to note that the large effects in UV–vis and CD were not observed in the corresponding dipeptide polyisocyanide.\(^27\) Apparently, the introduction of the second hydrogen bond in the polymer has a large effect on its molecular structure and rigidity and, as such, plays a very important role in gelation and thermal stability.

### CONCLUSION

In summary, we presented a thermal stable and well-defined helical polymer based on the \(\beta\)-helix polyisocyanotripeptide that mimics biological features of thermophilic proteins. This exceptional helical architecture is stabilized by a double hydrogen-bonding array between the amide groups, which plays a key role in the bundle formation, gelation, and thermal stability. Consequently, the TriPIC polymers have several significant and unusual characteristics. First, the hydrophobic core, which is constructed by the multiple hydrogen bonds, is partly shielded from water. The increased helical definition on heating the polymer in solution in an important design feature toward its thermal stability. Second, on heating aqueous TriPIC solution, the polymers assemble into bundled networks driven by hydrophobic interactions between the ethylene glycol tails. The formed gels show excellent thermal stability at temperatures as high as 80 °C. Third, the mechanical properties of TriPIC gels in both the linear and nonlinear regimes, including the storage modulus \(G^'\) and critical stress \(\sigma_c\), are readily tailored by the polymer concentration, their length, and by salts present in solution. In short, we have presented a truly synthetic polymer that is able to deal with excessive thermal energy using biological approaches such as hydrogen bonding and hydrophobic interactions, even without the changing of surface electrostatics which is a common natural strategy. This approach can be extended to design principles for future thermophilic proteins and synthetic polymers.

### EXPERIMENTAL SECTION

**Materials and instrumentation.** All chemicals were purchased from Sigma-Aldrich, Acros, or Alfa Aesar and used as received unless specially stated. Dichloromethane and chloroform were distilled over CaCl\(_2\). Tetrahydrofuran and toluene were distilled over sodium in the presence of benzophenone. \(^1\)H and \(^13\)C NMR spectra were recorded on a Varian Inova 400 or a Bruker Avance III 500 MHz. Rheology measurements were measured with stress-controlled and parallel-plate rheometer (Discovery HR-2, TA Instruments). AFM images were taken by a NanoScope IV in tapping mode. The absorption spectra were taken on a JASCO V-630 UV–vis spectrophotometer, and the CD spectra were carried out on a JASCO J-810. Cryo-scanning electron microscopy (cryo-SEM) was performed on a JEOL 6330 cryo-scanning electron microscope. IR spectra were performed on a Bruker VERTEX 80v vacuum FT-IR spectrometer.

**Synthesis of 3EG-L-Ala-d-Ala-L-Ala-Boc.** 3EG-L-Ala-d-Ala-L-Ala-Boc (4.0 g, 9.84 mmol), as synthesized according to the literature,\(^27\) was dissolved in 20 mL of HCl solution in ethyl acetate (2.3 mol/L) and stirred at rt for 2 h. After the Boc-protecting group was totally removed as monitored by TLC (3% of methanol in DCM as eluent), the solvent and the excess HCl were removed by rotary evaporator in vacuo. The crude product was dissolved in 250 mL of distilled DCM, to which \(\varepsilon\)-HA-O-Ala-Boc (1.9 g, 10 mmol) and hydroxybenzotriazole (1.1 g, 10 mmol) were added and N-Ethylisopropylamine (1.3 g, 10 mmol) was added slowly until the reaction mixture was basic and clear in appearance, and 1-\(\varepsilon\)-(dimethylamino)propyl)-3-ethylcarbodiimide hydrochloride (EDC\(_2\)HCl) (1.9 g, 10 mmol) was added. The reaction mixture was stirred at rt overnight. The reaction mixture was washed successively with citric acid solution (6%, 100 mL), water (100 mL), saturated solution of sodium bicarbonate (100 mL), and water (100 mL x 2) and dried over sodium sulfate. The solvent was removed by rotary evaporation, and the crude product was purified by a silica column chromatography (2% of methanol in DCM as eluent). The product was collected as a colorless oil, with a yield of 65%. Analysis: \(^1\)H NMR (500 MHz, CDCl\(_3\)) \(\delta\) 7.36 (d, \(J = 6.6\) Hz, 1H), 7.22 (d, \(J = 5.5\) Hz, 1H), 5.57 (d, \(J = 5.3\) Hz, 1H), 4.53–4.40 (m, 2H), 4.22–4.03 (m, 3H), 3.60–3.56 (m, 2H), 3.55–3.50 (m, 6H), 3.46–3.42 (m, 2H), 3.26 (s, 3H), 1.32 (s, 9H), 1.31–1.23 (m, 9H). \(^13\)C NMR (125 MHz, CDCl\(_3\)) \(\delta\) 173.01, 172.57, 171.96, 155.46, 79.59, 71.77, 70.45, 70.42, 70.36, 68.77, 64.22, 58.81, 50.30, 48.48, 48.05, 28.23, 18.23, 17.89, 17.69. MS (ES\(^+\)): m/z (%): 500.1 [M + Na\(^+\)]. HRMS (ES\(^+\)): calc for \(C_{21}H_{39}N_3O_9Na\): 500.2579, found 500.2585.

**Synthesis of 3EG-L-Ala-d-Ala-L-Ala-For.** 3EG-L-Ala-d-Ala-L-Ala-For (2 g, 4.94 mmol) was dissolved in 10 mL of DCM solution in ethyl acetate (2.3 mol/L) and stirred at rt for 2 h. After the Boc-protecting group was totally removed as monitored by TLC (3% of methanol in DCM as eluent), the solvent and the excess HCl were removed by rotary evaporator in vacuo. The crude product was mixed with 30 mL of ethyl formate, to which mixture sodium formate (1.34 g, 19.76 mmol) was added. The reaction was stirred under reflux overnight, after which it was cooled down to rt, and the solid was filtered off and washed thoroughly with CHCl\(_3\). The solvent was removed from the filtrate, and the crude product was purified with a silica column chromatography (3% of methanol in DCM as an eluent) to yield 3EG-L-Ala-d-Ala-L-Ala-For as a colorless solid, with a yield of 68%. Analysis: \(^1\)H NMR (\(\delta\) ppm, CDCl\(_3\), 500 MHz): 8.18 (s, 1H), 7.04 (d, \(J = 7.1\) Hz, 1H), 6.94 (d, \(J = 6.6\) Hz, 1H), 6.65 (d, \(J = 4.4\) Hz, 1H), 4.51–4.60 (m, 3H), 4.33–4.21 (m, 2H), 3.71–3.67 (m, 2H), 3.67–3.63 (m, 6H), 3.57–3.54 (m, 2H), 3.38 (s, 3H), 1.42 (d, \(J = 7.1\) Hz, 6H), 1.38 (d, \(J = \)
Synthesis of Monomer. 3EG-l-Ala-d-Ala-l-Ala-For (1.215.6 mg, 3.0 mmol) and N-methylmorpholine (NMM; 831 μL, 7.5 mmol) were dissolved in 300 mL of freshly distilled CHCl₃ and cooled down to −40 °C (dry ice and acetone bath) under an argon atmosphere. A solution of diphosgene (185 μL, 1.5 mmol) in 40 mL of freshly distilled CHCl₃ was added dropwise under argon over 1 h with the temperature kept at −40 °C. The reaction was quenched by adding sodium bicarbonate (5 g). The quenched mixture was stirred for 5 min at −40 °C. The reaction mixture was purified by the silica column (CHCl₃/methanol, 2%), to yield monomer as a pale solid, with a yield of 80%. Analysis: H NMR (δ ppm, CDCl₃, 500 MHz): 7.20 (d, 1H), 6.89 (d, 1H), 4.61 (m, 1H), 4.53 (m, 1H), 4.32 (m, 3H), 3.72 (m, 2H), 3.66 (s, 6H), 3.57 (m, 2H), 3.39 (s, 3H), 1.67 (d, J = 7.1 Hz), 1.44 (m, 6H). ¹³C NMR (δ ppm, CDCl₃, 125 MHz): 172.85, 172.38, 170.84, 166.30, 161.05, 71.88, 70.60, 70.54, 70.45, 68.93, 64.45, 58.96, 48.88, 48.35, 19.79, 18.13, 17.87. MS (ES⁺): m/z (%) = 410.2 [M + Na⁺]; HRMS (ES⁺): calcd for C₇₃H₁₂₅N₃O₈Na 428.2003, found 428.2009.

Characterizations of Polymer. The molecular weight (Mₐ) of the polymer was measured by viscometry in acetonitrile at 25 °C, according to the Mark–Houwink equation, and the apparent polymer contour length (Lₐ) was calculated from the measured Mₐ. The polymer was observed by the atomic force microscopy (AFM) in the tapping mode. The solutions of polymers (CHCl₃) were spin-coated onto the freshly cleaved Mica substrate.

Rheology. To prepare the TriPIC hydrogels, 4.0 mg of polymers was dissolved in 1.0 mL of precooled Milli-Q water by stirring for 12 h at 4 °C, resulting in a 4.0 g L⁻¹ transparent gel solution. Rheological measurements were performed on a stress-controlled rheometer (Discovery HR-2, TA Instruments), which was equipped with a parallel-plate geometry (40 mm diameter; aluminum) and temperature controller. In order to minimize sample evaporation at high temperature, an oil sealing was used. For the linear viscoelastic regime, all experiments were performed at a differential modulus K' of the sample over monomer (500:1, 1,000:1, 2,000:1, 5000:1, 8000:1, 12000:1, 15000:1). The reaction mixture was stirred for 2–7 days at room temperature, and the isocyanide peak was monitored by ATR-FTIR. When the reaction was complete, the reaction mixture was precipitated in a large volume of disopropyl ether for three times.

Present Address
R.H.: Department of Tumor Immunology, Radboud Institute for Molecular Life Sciences, Radboud University Medical Center, Geert Grooteplein 26, 6525 GA Nijmegen, The Netherlands.

Notes
The authors declare no competing financial interest.

ACKNOWLEDGMENTS
This work was supported by the National Nature Science Foundation of China (NSFC, 51503143, 21574037, and 21761132007), Tianjin Natural Science Foundation (16JCQNJC05000 and 15JCYBJC17500), Innovation Foundation of Tianjin University (2016XRX0017), China International Science and Technology Project (2016YFE0114900), Natural Science Foundation of Hebei Province (B2015202330 and B2017202051), Tianjin 1000 Youth Talents Plan, and Netherlands Organization for Scientific Research (NWO) with a Veni Grant (680-47-437) and a Gravitation Grant (024.001.035). Y. Duan is acknowledged for preparing some of the intermediate compounds.

REFERENCES