Automated Quantification and Integrative Analysis of 2D and 3D Mitochondrial Shape and Network Properties

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Abstract
Mitochondrial morphology and function are coupled in healthy cells, during pathological conditions and (adaptation to) endogenous and exogenous stress. In this sense mitochondrial shape can range from small globular compartments to complex filamentous networks, even within the same cell. Understanding how mitochondrial morphological changes (i.e. “mitochondrial dynamics”) are linked to cellular (patho) physiology is currently the subject of intense study and requires detailed quantitative information. During the last decade, various computational approaches have been developed for automated 2-dimensional (2D) analysis of mitochondrial morphology and number in microscopy images. Although these strategies are well suited for analysis of adhering cells with a flat morphology they are not applicable for thicker cells, which require a three-dimensional (3D) image acquisition and analysis procedure. Here we developed and validated an automated image analysis algorithm allowing simultaneous 3D quantification of mitochondrial morphology and network properties in human endothelial cells (HUVECs). Cells expressing a mitochondria-targeted green fluorescence protein (mitoGFP) were visualized by 3D confocal microscopy and mitochondrial morphology was quantified using both the established 2D method and the new 3D strategy. We demonstrate that both analyses can be used to characterize and discriminate between various mitochondrial morphologies and network properties. However, the results from 2D and 3D analysis were not equivalent when filamentous mitochondria in normal HUVECs were compared with circular/spherical mitochondria in metabolically stressed HUVECs treated with rotenone (ROT). 2D quantification suggested that metabolic stress induced mitochondrial fragmentation and loss of biomass. In contrast, 3D analysis revealed that the mitochondrial network structure was dissolved without affecting the amount and size of the organelles. Thus, our results demonstrate that 3D imaging and quantification are crucial for proper understanding of mitochondrial shape and topology in non-flat cells. In summary, we here present an integrative method for unbiased 3D quantification of mitochondrial shape and network properties in mammalian cells.

Introduction
Mitochondria play diverse roles in eukaryotic cell physiology in that they serve as producers of ATP and constitute essential hubs of metabolism and signal transduction. The organelle is composed of a mitochondrial outer membrane (MOM) that surrounds an inner membrane (MIM), which is highly folded and encloses the matrix compartment where metabolic enzymes and the mitochondrial genome reside. Mitochondria operate as main transducers of cellular energy and house enzymes systems for β-oxidation, the TCA cycle, ketogenesis, and oxidative phosphorylation (OXPHOS). The OXPHOS machinery is embedded in the MIM, and consists of the electron transport complexes and the ATP synthase. In this system, electron flow drives transmembrane transport of protons, which generates the proton gradient utilized for ATP production by ATP synthase [1]. Although mitochondria are characterized by having some degree of genetic and metabolic autonomy their function is intricately linked to that of the cell. In this sense, evidence has been provided that bidirectional mitochondria-cell communication through major signaling pathways occurs in cellular homeostasis, growth, survival and death. Hence, endogenous and exogenous factors including nutritional status, pharmacological modulation, cytosolic signal transduction and the presence of pathological mutations may (in) directly affect mitochondrial function [2–7].

In living cells, mitochondria can form a large tubular assembly (“a reticulum”) extending throughout the cytosol, which is often close to other cellular compartments like the nucleus, endoplasmatic reticulum (ER) and cytoskeleton [8–10]. The cellular volume fraction occupied by mitochondria varies between cell types and with metabolic condition [11,12]. Mitochondrial morphology is very dynamic and can shift between fragmented structures and filamentous networks, via mitochondrial fission and fusion events [13]. Mitochondrial morphology is directly controlled by the balanced action of fission and fusion proteins including the optic atrophy 1 (OPA1) protein, mitofusins (Mfn1
Cell culture

Materials and Methods

Mitochondrial morphology and physiology demands automated quantitative methods to analyze mitochondrial shape. Mitochondrial shape parameters can be obtained using fluorescent cations that specifically accumulate within mitochondria (e.g., TMRE, TMRM, rhodamine 123, JC-1) or by genetically introducing mitochondria-targeted fluorescent proteins [25,26]. At present, mitochondrial shape analysis is primarily performed by automated computer-assisted analysis of 2-dimensional (2D) fluorescence microscopy images, employing suitable types of software and (custom) algorithms [6,27]. These strategies work best on cultured cells with a relatively flat morphology. For cells displaying a substantial “thickness” in the axial (z) direction, three-dimensional (3D) image acquisition and analysis are required. In principle, confocal microscopy allows acquisition of axial image sequences (“z-stacks”) for 3D quantification. However, relatively few strategies optimized for mitochondrial analysis have been reported [6]. One such strategy involves creation of a semi-3D image by collapsing multiple image-sections from a wide-field or confocal z-stack into a single 2D projection [28,29]. A more advanced method is to generate a 3D representation of the mitochondria from the z-stack and performing a 3D analysis of the mitochondrial objects. Although technically more demanding than 2D procedures, attempts to analyze mitochondria in 3D appeared promising in studies of mitochondrial shape and network properties [6,22,25,30–32]. However, to the best of our knowledge, none of the published 3D strategies involves combined and integrative assessment of mitochondrial shape and network properties. In this study, we established and validated such analysis in z-stacks of human endothelial cells (HUVECs) expressing a mitochondria-targeted green fluorescence protein (mitoGFP). The performance of this 3D approach was compared with our previously described 2D algorithm [6,20,24,27,33–40] in healthy cells and during ROT-induced metabolic stress conditions. Our results demonstrate that 3D imaging and quantification are of crucial importance for proper analysis of mitochondrial dynamics in cells displaying a non-flat morphology. Hopefully, the strategy provided in this study may contribute to clarify new relationships between mitochondrial morphology and physiology.

Materials and Methods

Cell culture

Phoenix A retroviral packaging cells were used for virus production [41]. The cells were maintained in DMEM with 4.5 g/l glucose (Gibco) supplemented with 10% fetal bovine serum (FBS), 2 mM L-glutamine, 100 U/ml penicillin and 100 μg/ml streptomycin (all from Sigma-Aldrich). Human Umbilical Vein Endothelial Cells (HUVECs) were purchased from Lonza, Basel, Switzerland (C2517A). The cells were cultured in EGM-2 (Lonza), and kept at 37°C and 5% CO2. The growth medium was changed every second or third day and the cells were passaged prior to reaching confluence. The maximum passage number used for experiments was 8.

Cloning and retroviral transduction

HUVECs stably expressing mitochondrial targeted GFP (mitoGFP) were produced by retroviral transduction [41]. Generation of a retroviral vector carrying mitoGFP was initiated by exchanging EYFP in the commercial available pEYFP-mito vector (BD Biosciences, Clontech) with EGFP. GFP from pEGFP-N1 and YFP from pEYFP-mito were excised using the restriction enzymes BamHI and BsrGI. The products were separated by gel electrophoresis and the pEGFP insert and the vector with the mitotargeting sequence were gel-purified using GFX columns (GE Healthcare). EGFp was then cloned into the vector fragment, generating the pEGFP-mito vector. Further, pEGFP-mito was cut with NheI before converting overhangs to blunt ends followed by further cutting with NotI. The resultant fragment was cloned into the retroviral vector pCGFP [42] previously cut with BamHI, blunt-ended, and cut again with NotI to remove the existing GFP fragment. The fragments were separated by gel electrophoresis and gel-purified using GFX columns prior to ligation. This resulted in generation of the pCEGFP-mito vector. Correct orientation of the inserts was controlled using restriction enzymes XbaI and NotI, and plasmids with correct promoter orientation were sequenced. All enzymes and buffers used during cloning procedures were from New England Biolabs. Phoenix A packaging cells were transfected by CaCl2 precipitation in presence of chloroquine (Sigma-Aldrich) with the pCEGFP-mito retroviral vector. At 6 h post-transfection, the medium was replaced with fresh DMEM containing 10% FBS and cells were grown for 12 hours. The medium was then replaced with EGM-2 medium and the cells were grown for additionally 24 hours to produce retroviruses. Conditioned media was collected, filtered through 0.45 μm-pore-size polysulfonic filters and added to the HUVEC culture together with protamine sulfate (5 μg/ml) (Sigma-Aldrich). Fresh EGM-2 medium was again added to the Phoenix A packaging cells, and after additional 24 hours virus were harvested and added to the HUVECs for a second round with virus infection. After the first overnight incubation with virus-containing medium, the cells were incubated in fresh EGM-2 for 8 hours, prior to an additional overnight incubation in the presence of the virus vector. After infection, HUVECs were cultured before GFP-positive cells were sorted on a FACSAria Cell Sorter (BD Biosciences).

Confocal microscopy

12,000 HUVECs were seeded onto 18 mm coverslips and were allowed to adhere under routine culturing conditions for 2–4 hours before treatments were added. The cells were then incubated for 72 hours before they were fixed with cold (4°C) 3.7% paraformaldehyde at room temperature for 30 minutes. The coverslips were rinsed in PBS and water before they were dried and mounted onto a cover glass using Vectashield mounting medium with DAPI (Vector Laboratories, California, US). The z-stack images of mitoGFP were acquired on a Zeiss LSM 510 Meta confocal microscope (Carl Zeiss, Oberkochen, Germany) using a Plan-Apochromat 63×1.40 NA oil objective. Excitation wavelength was 488 nm and emission was detected using a long pass filter from...
Multidimensional Analysis of Mitochondria

A

2D Test image, binary

SHAPE

64 pixels

108 pixels

2D vectorized

NETWORK

B

3D Test z-stack

(black + 3x 2D Test image + black)

3D iso-surface

SHAPE

3D vectorized

NETWORK

C SHAPE (Units: Numerical values, pixel/voxel based)

2D Area (Am) vs 3D Volume (Vm)

2D Perimeter (Pm) vs 3D Surface area (Sm)

2D Form factor/Roundness (F) vs 3D Sphericity (SF)

D NETWORK (Units: Numerical values, pixel/voxel based)

2D Branch Length (LBR) vs 3D Branch Length (LBR)

2D Branching points (NBP) vs 3D Branching points (NBP)

2D Branch Diameter (DBR) vs 3D Branch Diameter (DBR)
505 nm. Image pixel size was 0.0845 μm (x and y) and bit depth 8, z-step size 0.364 μm, and pinhole diameter 96 μm.

Image processing and analysis
All image processing and analysis were performed using the Image-Pro Plus software (version 7.0) with the SharpStack Total deconvolution and 3D Constructor modules (Media Cybernetics, Inc., Washington, USA). The blind deconvolution algorithm of this software is the same found in the AutoQuant software (Media Cybernetics, personal communication). The datasets were first calibrated using the acquisition system parameters, and cropped to exclude unnecessary regions, before processing by 3D blind deconvolution. For comparative purposes, the images were excluded processing regions of interest. The Fast Fourier Transform (FFT) processing, a circular area of interest (AOI; radius setting 2, 5 or 10, as specified) was defined in the center of the spectrum in the frequency domain. Projections of multiple z-stack sections into one image were performed either by averaging or by generating a maximum intensity composite (MIC). For 3D analysis, the z-stacks were loaded into the 3D Constructor module using no sub-sampling. A 3D iso-surface was created without further filtering or simplification prior to volumetric shape measurements. Regions of interest (ROIs) were selected stochastically in mitochondria-rich parts of the cytoplasm. With respect to mitochondrial network analysis, the objects were skeletonized using standard processing operations (medial axis transform), which involved an intensity threshold, followed by thinning and then pruning of the objects. The threshold intensity corresponded with the respective threshold used in the parallel shape analysis, as indicated in the individual

Table 1. Parameters of mitochondrial morphology.

<table>
<thead>
<tr>
<th>Analysis modality</th>
<th>Descriptor</th>
<th>Comment</th>
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<tbody>
<tr>
<td>2D Shape analysis</td>
<td>Count</td>
<td>NROI</td>
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<tr>
<td></td>
<td>Area</td>
<td>A_m</td>
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<td></td>
<td></td>
<td>A_m,ROI</td>
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<tr>
<td></td>
<td>Perimeter</td>
<td>P_m</td>
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<tr>
<td></td>
<td></td>
<td>P_m,ROI</td>
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<tr>
<td></td>
<td>Formfactor</td>
<td>F</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Calculated as (P_m/2(4πA_m)). Circular objects will have an F-value close to 1, other shapes will have F&lt;1.</td>
</tr>
<tr>
<td>3D Shape analysis</td>
<td>Count</td>
<td>NROI</td>
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<tr>
<td></td>
<td>Volume</td>
<td>V_m</td>
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<tr>
<td></td>
<td></td>
<td>V_m,ROI</td>
</tr>
<tr>
<td></td>
<td>Surface</td>
<td>S_m</td>
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<td></td>
<td></td>
<td>S_m,ROI</td>
</tr>
<tr>
<td></td>
<td>Sphericity</td>
<td>SF</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Calculated as SF = (6 V_m) / (D_m^2 S_m), where D_m is the equivalent diameter. For a spherical object SF is close to 1, all other shapes have an SF&lt;1.</td>
</tr>
<tr>
<td>2/3D Network analysis</td>
<td>Branch count</td>
<td>N_Br</td>
</tr>
<tr>
<td></td>
<td>Branch points</td>
<td>N_BP</td>
</tr>
<tr>
<td></td>
<td>Branch length</td>
<td>L_Br</td>
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<td></td>
<td></td>
<td>L_Br,ROI</td>
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<tr>
<td></td>
<td>Branch diameter</td>
<td>D_Br</td>
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<tr>
<td></td>
<td>Branch volume</td>
<td>V_Br</td>
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<tr>
<td></td>
<td></td>
<td>V_Br,ROI</td>
</tr>
<tr>
<td></td>
<td>End points</td>
<td>N_EP</td>
</tr>
<tr>
<td>2/3D Network - Shape</td>
<td>Branch (filament) length per mitochondrion</td>
<td>L_Br,ROI / N_ROI</td>
</tr>
<tr>
<td>Integrative analysis</td>
<td>Branch (filament) length per biomass</td>
<td>L_Br,ROI / A_m,ROI (2D); L_Br,ROI / V_m,ROI (3D)</td>
</tr>
<tr>
<td></td>
<td>Branch number per mitochondrion</td>
<td>N_BP / N_ROI</td>
</tr>
<tr>
<td></td>
<td>Branch number per biomass</td>
<td>N_BP / A_m,ROI (2D); N_BP / V_m,ROI (3D)</td>
</tr>
<tr>
<td></td>
<td>Branching point frequency - branch length</td>
<td>N_BP / L_Br,ROI</td>
</tr>
<tr>
<td></td>
<td>Branching point frequency - biomass</td>
<td>N_BP / A_m,ROI (2D); N_BP / V_m,ROI (3D)</td>
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Legend: ROI, region of interest.

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experiments. We used 2 thinning iterations to create the
topological skeleton, and 2 pruning iterations to remove small
extensions due to irregularities in the objects (i.e. noise such as
single-pixel bumps) but not significant parts of the structures. The
resulting mitochondrial skeleton was vectorized to identify and
count/measure branches (skeletal backbone), end points and
branch points as graphic vectors/points. This was also used to
measure distance map values (i.e. how far from the edge of the
object any pixel/voxel lies) in order to determine branch diameter
and volume. All these image operations are conventional and can
be applied in suitable image processing software. In Image-Pro
Plus, these operations have been integrated in a consecutive
manner in the built-in “NeuronAnalyzing” macro, which we
employed in this study.

Figure 2. Image optimization for mitochondrial segmentation in 3D z-stacks. (A) The images show all sections of an unprocessed (“RAW”) z-stack of a HUVEC expressing mitoGFP. (B) The histogram shows the cumulative pixel fluorescence intensity in the individual z-stack sections (RAW). The highest intensity column (section 8) is highlighted in white. (C) The effect of 3D blind deconvolution (“Deconv”) on the S/N ratio. Fluorescence intensity was measured across the indicated line (upper panel) before and after 2, 4, 6, 8 or 10 deconvolution cycles. The figure shows z-stack section 8 (upper panel) and the associated line intensity diagrams (middle panel) derived after 0 (“RAW”), 4 (“4*Deconv”) and 10 (“10*Deconv”) deconvolution cycles. The line intensity peaks and valleys identify mitochondrial objects/filaments and background, respectively. The intensities of five selected peak and background pixels (numbered 1–5, middle panel), before and after 2–10 deconvolution cycles are displayed in the column diagram (bottom panel). (D) Usefulness of Fast Fourier Transform (FFT) filtering following deconvolution. The images (upper panel) show z-stack section 8 after FFT filtering using frequency domain area of interest (AOI) radius setting 10, 5 and 2 (including Hi-Pass filtering). The intensity profiles across the same line (see above) are shown (middle panel), and the selected peak/background pixel intensities are plotted in the column diagram (bottom panel) for comparison with the non-FFT filtered image (n, identical to “10*Deconv” in (C)).

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Results

Analysis of the shape of synthetic objects in 2D and 3D

Our first objectives were to determine: (i) if the previously described principles of 2D analysis [21,27] could be translated into 3D analysis, and (ii) if mitochondrial filament properties could be quantified analogous to neuronal networks (see Materials and Methods). To allow proper interpretation of the parameters describing mitochondrial shape and network properties (“descriptors”) a 2D test image was used. This image contained mitochondria-like synthetic objects of relevant size (Fig. 1A). A 5-section z-stack was generated by layering of 3 copies of the 2D image between an empty (black) image on the top and bottom of the series (Fig. 1B). For the 2D image, descriptors of mitochondrial shape were quantified as previously described in detail [27]. For analysis of the 3D image, an iso-surface 3D (volumetric) model was generated from the z-stack. In addition to the shape analysis, the network analysis algorithm was used to skeletonize objects (in 2D and 3D), to perform vectorization, and to identify and quantify branch properties, branching points and endpoints. To allow faithful quantitative comparison of objects in the 2D and 3D test images, we selected descriptors with a correspondent meaning in 2D and 3D (Table 1). Plotting the numerical value for each shape descriptor and each object in the 2D and 3D image gave similar results (Fig. 1C and D). In this sense, the area of each 2D object ($A_m$) was virtually identical with the volume ($V_m$) of the corresponding 3D object (Fig. 1C; left panel). The 2D object perimeter ($P_m$) and 3D object surface area ($S_m$) also gave similar profiles (Fig. 1C; middle panel). Of note, an increase in length and degree of branching of the test objects induced a greater increase in $P_m$ than in $S_m$. To assess the “complexity” of 2D objects we analyzed the 2D formfactor ($F$), which is a measure of mitochondrial length and degree of branching [27,33]. In the 3D image, the sphericity factor ($SF$) was used as an equivalent measure of object complexity (Fig. 1C; right panel). $F$ and $SF$ gave similar profiles when plotted with inverse scaling in the same diagram (Fig. 1C; right panel). This is expected since there is an inverse relationship between $F$ and $SF$ as descriptors of circular
spherical (3D) objects. Taken together, the above results demonstrate that the shape/volume descriptors can be used to discriminate between objects of different width, objects with simple vs. complex morphologies, and circular (2D) vs. spherical (3D) objects.

Analysis of the network properties of synthetic objects in 2D and 3D

To obtain topological information, network analysis was performed on both the 2D and 3D test datasets (Fig. 1D & Table 1). In case of filamentous objects the profiles of branch length \(L_{br}\), number of branching points \(N_{br}\) and branch diameter \(D_{br}\) were similar in the 2D and 3D case. Numerical data for spherical/non-filamentous objects were only generated by the 2D analysis protocol but not by the 3D analysis algorithm. The latter was caused by the property of the 2D network rendering procedure to generate small and branched structures that did not properly reflect the original objects. Although unrepresentative structures can be easily removed from the analysis using an object filtering strategy (e.g. by discarding objects with a short branch length), they were included here for comparative purposes. We observed that the \(L_{br}\) and \(D_{br}\) descriptors allowed a logical discrimination between objects of different filament length and diameter, respectively (Fig. 1D: left and right panels). Quantification of the \(N_{br}\) parameter yielded similar results for 2D and 3D objects (Fig. 1D, middle panel).

Blind deconvolution improves the quality of quantitative mitochondrial analysis

Confocal microscopy is widely used to acquire 3D image stacks (z-stacks) of cells with fluorescently labeled constituents, including mitochondria. The shape of the fluorescent objects in such images will be blurred due to the point spread function (PSF) of the optics (convolution), leading to difficulties separating nearby mitochondria and their networks. In this sense, “deconvolution” is often applied to remove systemic disturbances including haze, in order to improve image contrast and object segmentation [43]. In this study we performed blind deconvolution with an iterative and constrained algorithm (SharpStack/AutoQuant) which repeats the same computational operations in order to adapt itself to the real PSF of the microscope system. Hence, this method is able to adjust to the specific conditions and specimens, and is designed to perform the best possible deconvolution without exceeding the information available. Due to these capabilities, blind deconvolution (including the algorithm used in this study) has been increasingly employed in cell imaging, and has proven useful in studies of subcellular structures in various contexts [44,43]. Others have confirmed that this blind deconvolution algorithm maintains the linear relationship in object intensities and their relative intensity changes, which validates the use in quantitative analysis [46]. Here we investigated whether 3D blind deconvolution was suited to optimize mitochondrial shape and network analysis. For this purpose we imaged HUVECs that were retrovirally transduced with a mitochondria-targeted variant of the green fluorescent protein (mitoGFP), by confocal microscopy (Fig. 2A). To prevent interference of mitochondrial movement during z-stack acquisition cells were fixed using paraformaldehyde treatment, which preserves well both cellular and mitochondrial structure [32]. The signal-to-noise (S/N) ratio was evaluated using the z-section display showing the maximal fluorescence intensity (i.e. section 8; Fig. 2B). Repeated deconvolution cycles increased the intensity difference between mitochondrial objects and the background, as shown by the intensity plotted across the indicated line profile (Fig. 2C; top and middle panel). Accordingly, increasing the number of deconvolution cycles reduced the background (non-mitochondrial) fluorescence intensity and increased the peak (mitochondria-specific) signal intensities (Fig. 2C; bottom panel with intensities of selected peak and background pixels). Based upon the above analysis we used at least 8 cycles to produce a deconvolved version of the image.

Fast Fourier transform filtering does not improve mitochondrial analysis

FFT filtering has been employed to optimize fluorescence images for segmentation of mitochondria [28]. Therefore we determined how FFT filtering of the deconvolved z-stack (see above) affected the S/N ratio. Frequency selection in the FFT transformed image (frequency domain) was performed by defining a circular AOI in the center of the spectrum. It was confirmed that FFT filtering highlighted high-intensity (mitochondrial) objects and flattened the non-mitochondrial (background) signal (Fig. 2D: top and middle panel). Reducing the AOI radius from 10 to 5 to 2 resulted in a progressive increase in image contrast (Fig. 2D: bottom panel). Next, we determined how FFT filtering affected the quantitation of 3D mitochondrial structure by analysis of a region of interest (ROI) within a deconvolved z-stack with and without FFT filtering (Fig. 3A and B). The analysis revealed that although FFT filtering apparently increased image contrast, its effects on quantitative mitochondrial shape and network parameters were only minor (Fig. 3C). However, careful inspection revealed that FFT filtering somewhat affected the localization of branch points in the mitochondrial network. Given the above results, we decided not to include an FFT filtering step in the image quantification algorithm.

Extracting 2D mitochondrial shape and network parameters from confocal z-stacks

Next, we determined whether image deconvolution affected quantification of mitochondrial shape and network properties. For this purpose quantification was carried out on all signal-containing sections in a ROI from a typical z-stack of mitoGFP expressing HUVECs (Fig. 4A: “unprocessed (RAW)”): Additionally, repre-
sentative 2D projections of the z-stack ROI were obtained by: (i) averaging of the three sections of highest intensity (Fig. 4; “Avg7–9”), (ii) generating a MIC image of the three sections of highest intensity (“MIC7–9”) and, (iii) calculating a MIC image using all sections (“MICall”). For comparison, all images were processed in two ways using: (i) the established spatial filtering 2D technique (Fig. 4; “Spatially filtered”; blue panels) developed for flat cells with fluorescently labeled mitochondria [6,20,21,24,27,33,34,36–40,47], and (ii) the deconvolution approach presented in the paper (Fig. 4; “Deconvolution”; orange panels). Following processing, mitochondrial objects were segmented/binarized (see also the next section) and size-filtered (Fig. 4; “SHAPE”); yellow panels). Similarly, mitochondrial network properties were analyzed by skeletonization and vectorization (Fig. 4; “NETWORK”; pink panels). Relative to the unprocessed situation, the average object pixel intensity in each section was increased by spatial filtering but not by deconvolution (Fig. 4B). However, this differential effect on intensity did not significantly influence the quantified shape (Fig. 4C) and network properties (Fig. 4D).

Visual inspection of the average (Avg7–9), MIC and MICall images revealed that these contained a higher amount of visually inspection of the average (Avg7–9), MIC and MICall quantified shape (differential effect on intensity did not significantly influence the spatial filtering but not by deconvolution (Deconvolution”; orange panels) for the purpose of 3D mitochondrial segmentation and analysis. (B) 3D models of the ROI were generated after spatial filtering, as previously established for 2D mitochondrial analysis [27], and after deconvolution as described in the current paper. The percentages reflect the segmentation thresholds (grey tone values) defining the 10%–35% (as indicated) brightest pixels in the highest intensity section (section 8). The smaller 2D images indicate the effects of threshold setting (MICS created from the processed z-stacks). 3D volume and network models are shown for three of the studied intensity thresholds (10%, 20% and 35%). (C) The diagrams show the quantified data from (B). Descriptor variables are explained in Table 1.

An automated algorithm for 2D and 3D analysis of mitochondria in HUVECs expressing mitoGFP

Based on the results obtained so far, we designed an image processing and analysis algorithm for 2D and 3D analysis of mitochondrial shape and network properties using confocal z-stacks (Fig. 6A). The algorithm applies several modules that need to be tuned carefully based on the qualities of the dataset/experiment, and combined to enable an automated sequence of processing and analysis steps. In brief, confocal z-stacks (“RAW”) are processed by 3D blind deconvolution (10 cycles; as described in Materials and methods). Optionally, the contrast may be stretched e.g. by employing a minimum intensity threshold to remove low intensity background noise and a maximum intensity limit, before the gray values of the pixels are reassigned to range from 0 to 255 (true for a 8-bit image) (as performed in Fig. 6 and Video S1–3). Further processing and analysis is twofold: (i) To enable 2D analysis, the z-stack is projected into a representative 2D MIC image (see previous sections). 2D shape analysis is performed subsequent to binarization of the MIC image, as previously described [27]. For 2D network analysis, the MIC image is skeletonized, vectorized and analyzed using the same threshold level as for the binarization. (ii) To enable 3D analysis, a volumetric model of the z-stack is created, and an isosurface is added to allow mitochondrial shape (3D) measurements. In parallel, 3D network analysis is performed using the same threshold intensity level as for the isosurface.

Integrative shape and network analysis of filamentous and non-filamentous HUVEC mitochondria

To test the performance of the method we analyzed mitochondria displaying two characteristic phenotypes, i.e. filamentous vs. non-filamentous mitochondria. The z-stacks were acquired from a mitoGFP expressing HUVEC (see previous sections). 2D shape analysis is performed subsequent to binarization of the MIC image, as previously described [27]. For 2D network analysis, the MIC image is skeletonized, vectorized and analyzed using the same threshold level as for the binarization. (ii) To enable 3D analysis, a volumetric model of the z-stack is created, and an isosurface is added to allow mitochondrial shape (3D) measurements. In parallel, 3D network analysis is performed using the same threshold intensity level as for the isosurface.

Table 1

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Description</th>
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<tr>
<td>NROI</td>
<td>Number of ROIs</td>
</tr>
<tr>
<td>LRR, NRR</td>
<td>Length and number of elongated mitochondrial segments</td>
</tr>
<tr>
<td>DBR</td>
<td>Diameter of the binarized objects</td>
</tr>
<tr>
<td>LRR, NRR</td>
<td>Length and number of elongated mitochondrial segments</td>
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</table>

Multidimensional Analysis of Mitochondria

To highlight mitochondrial objects, microscopy images were binarized using an intensity-based threshold operation. Obviously, setting a certain threshold intensity value can influence subsequent 3D analysis of mitochondrial shape and volume properties. The impact of threshold intensity was therefore evaluated on a z-stack with mitoGFP expressing HUVECs that was processed using spatial filtering (see previous section) or by deconvolution and subsequently analyzed (Fig. 5A). To allow proper comparison, intensity thresholds were set in such a way that they included a specific fraction (10–35%) of the brightest pixels in the highest intensity section of the z-stack (i.e. section 8). Lowering the threshold intensity level (equivalent to including a higher fraction of pixels), reduced the value of the object count parameter (NROI), increased object-size parameters (VROI, DROI), and increased filament connectivity parameters (LRR, NRR) (Fig. 5B and C). It was also observed that threshold adjustments affected mitochondrial segmentation and shape/network parameters less dramatically in the deconvolved z-stack than in the spatially filtered z-stack. For instance, NROI remained relatively stable (average 2 fold change) in the deconvoluted z-stack when using a threshold between 20%–35%, whereas this parameter changed more than 20 fold for the spatially filtered z-stack in the same threshold intensity range. Similarly, LRR, NRR increased almost 5 fold in the spatially filtered dataset in the 20%–35% threshold range, compared to 1.4 in the deconvolved data. In the spatially filtered z-stack, inclusion of more pixels did not affect DROI, as after deconvolution; but low thresholds (30% and 35%) introduced a significant amount of noise and thereby an increase in NROI. When a 20% threshold setting was applied, similar mitochondrial shape/network data were obtained for the spatially filtered and deconvoluted z-stack.

Figure 5. Threshold setting for mitochondrial segmentation in a HUVEC z-stack. A sample z-stack was acquired from a HUVEC expressing mitoGFP, and a region of interest (ROI) was selected (identical to the sample z-stack and the ROI as shown in Fig. 3). (A) The images show maximum intensity composites (MIC) of the entire unprocessed sample z-stack (“RAW”) and a magnification of the ROI. The figure also displays the comparative effects of spatial filtering (“Spatial filtering”; blue panels) and deconvolution (“Deconvolution”; orange panels) for the purpose of 3D mitochondrial segmentation and analysis. (B) 3D models of the ROI were generated after spatial filtering, as previously established for 2D mitochondrial analysis [27], and after deconvolution as described in the current paper. The percentages reflect the segmentation thresholds (grey tone values) defining the 10%–35% (as indicated) brightest pixels in the highest intensity section (section 8). The smaller 2D images indicate the effects of threshold setting (MICS created from the processed z-stacks). 3D volume and network models are shown for three of the studied intensity thresholds (10%, 20% and 35%). (C) The diagrams show the quantified data from (B). Descriptor variables are explained in Table 1.

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Multidimensional Analysis of Mitochondria

A

2D ANALYSIS

SHAPE | NETWORK

Thresholding  
2D BIN | 2D Skeleton

Thinning Vectorization

Processing

RAW  
3D BD

Thresholding  
3D Surface | 3D Skeleton

Thinning Vectorization

SHAPE | NETWORK

3D ANALYSIS

B

Normal (CTR)

Stressed (ROT)

20 µm

C

Normal

Stressed

Fluorescence Intensity (Numerical value * 10^4)

Section No 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23

Section No 1 2 3 4 5 6 7 8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23 24 25 26 27 28 29 30 31 32

D

2D analysis

Normal (ROI2)

Stressed (ROI4)

Deconv. SHAPE NETWORK

Frame 7 MIC

Frame 12 MIC

E

3D analysis

Normal (ROI2) Stressed (ROI4)

3D model

SHAPE NETWORK
Mitochondrial morphology was studied in normal and metaboli-
cally stressed (250 nM rotenone, 3 days) HUVECs expressing mitoGFP. (A) The figure shows a schematic overview over
the procedure established to analyze mitochondrial shape and network properties in 2D and 3D. The boxes represent image outcome, and the
arrows indicate mathematical operations. "RAW", unprocessed z-stack; "3D BD", z-stack 3D blind deconvolution (10 cycles); "2D BIN", binarized 2D
image (intensity threshold); "2D Network", skeleton based on the 2D image; "3D Surface", iso-surface model (intensity threshold); "3D Network",
skeletonized 3D model. The intensity thresholds were determined to give the best reflection of the source image. (B) The images are maximum
intensity composites (MICs) of the processed z-stacks from an untreated HUVEC ("Normal (CTR)") and a ROT-treated stressed HUVEC ("Stressed
(ROT)"). The z-stacks were processed by deconvolution and a contrast stretch (as described in the current article). Five different regions of interest
(ROIs; numbered 1–5 in the images) were selected in each cell. (C) The histograms show the intensity profile of the two z-stacks. The highest intensity
sections are shown as white columns. (D) 2D analysis was performed on the highest intensity frame, and the z-stack MIC. The panels show shape and
network representations of one ROI selected from each cell. (E) 3D shape and network models were generated and analyzed from each of the ROIs in
both cells. Here, the 3D models of one ROI in each cell type are shown.

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Performance of deconvolution and FFT filtering in 2D and
3D analysis

The performance of deconvolution and/or FFT filtering was evaluated in prototypic non-flat cells (HUVECs) expressing mitoGFP targeted to the mitochondrial matrix of cells. Given the time required for acquisition, cells were fixed to prevent mitochondrial movement. We observed that 3D deconvolution significantly improved the segmentation of mitochondrial objects in the z-stack, and thereby the quality of the shape and network analysis. The characteristics of the z-stack fluorescence intensity histogram were less affected by deconvolution when compared to the spatial filtering procedure. However, subsequent 2D quantification of mitochondrial parameters in the individual z-stack sections yielded similar results for deconvolved and spatially processed images. In the 3D case, deconvolution allowed a more robust mitochondrial segmentation and analysis. These results demonstrate that image optimization by deconvolution constitutes a valid alternative to the 2D spatial filtering strategy prior to 2D

Figure 6. Comparative 2D/3D mitochondrial analysis to detect effects of metabolic stress in HUVECs. Mitochondrial morphology was studied in normal and metabolically stressed (250 nM rotenone, 3 days) HUVECs expressing mitoGFP. (A) The figure shows a schematic overview over the procedure established to analyze mitochondrial shape and network properties in 2D and 3D. The boxes represent image outcome, and the arrows indicate mathematical operations. "RAW", unprocessed z-stack; "3D BD", z-stack 3D blind deconvolution (10 cycles); "2D BIN", binarized 2D image (intensity threshold); "2D Network", skeleton based on the 2D image; "3D Surface", iso-surface model (intensity threshold); "3D Network", skeletonized 3D model. The intensity thresholds were determined to give the best reflection of the source image. (B) The images are maximum intensity composites (MICs) of the processed z-stacks from an untreated HUVEC ("Normal (CTR)") and a ROT-treated stressed HUVEC ("Stressed (ROT)"). The z-stacks were processed by deconvolution and a contrast stretch (as described in the current article). Five different regions of interest (ROIs; numbered 1–5 in the images) were selected in each cell. (C) The histograms show the intensity profile of the two z-stacks. The highest intensity sections are shown as white columns. (D) 2D analysis was performed on the highest intensity frame, and the z-stack MIC. The panels show shape and network representations of one ROI selected from each cell. (E) 3D shape and network models were generated and analyzed from each of the ROIs in both cells. Here, the 3D models of one ROI in each cell type are shown.

PMCID: 3892834

Multidimensional Analysis of Mitochondria

MitoGFP targeted to the mitochondrial matrix of cells. Given

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In contrast, our results revealed that 3D deconvolution is the preferred strategy for z-stack processing prior to 3D analysis. FFT filtering has been successfully applied in other studies that did not use deconvolution [28]. However, we did not include FFT filtering in our image processing scheme since it did not (further) improve the analysis.

Figure 7. Shape and network analysis of normal vs. stressed HUVEC mitochondria. The images from the study in Fig. 6 were analyzed with respect to 2/3D “SHAPE” (A) and “NETWORK” parameters (B). The positions of the different ROIs are shown in Fig. 6B. The data resulting from 2D analysis of the highest intensity frame (“2D single sect.”) and the z-stack MIC (“2D MIC”) where compared with the 3D data (“3D volume”). The descriptor variables are explained in Table 1. *p<0.05 compared to CTR, Student’s t-test, two-tailed.

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**Integrative analysis of filamentous vs. non-filamentous HUVEC mitochondria**

The developed 3D protocol was benchmarked by comparing mitochondrial shape and network parameters between z-stacks of filamentous (“Normal”) and non-filamentous (“Stressed”) HUVEC mitochondria. We also tested several semi-3D strategies by collapsing multiple z-stack sections into a representative 2D image. Clearly, such an approach is technically less demanding and time-consuming than full-scale z-stack 3D analysis. The difference between the MIC projection of all the sections compared with the two 3-sections projections (MIC and Avg) was relatively small. It was, however, evident that some features were lost or rendered in the projected images compared to the 3D analysis. Obviously, projecting an entire z-stack into a single 2D image can lead to excessive merging/shielding of objects, which is undesirable. Analysis of the single highest intensity z-stack section was less reliable compared to the MIC image when examining mitochondrial morphology in normal and stressed cells. This means that although z-stack projection approaches may be employed to study certain aspects of mitochondrial morphology, this analysis should preferably be supported by complementary methods [6].

When applicable, the internal variation within each ROI was also evaluated.

Compatible with visual observations, both 2D and 3D analysis indicated a shift from filamentous network morphology to circular (in 2D) and spherical (in 3D) organelles. This effect was particularly clear from the network analysis, since both 2D and 3D descriptors indicated a reduction in the number of mitochondrial branches ($N_{BR}$), mitochondrial branching points ($N_{BP}$), and total mitochondrial branch length ($L_{BR,ROI}$). 2D mitochondrial shape analysis suggested that stressed cells contained a higher number ($N_{ROI}$) of smaller ($A_m$) and more circular ($F$) mitochondria, accompanied with a loss in mitochondrial biomass ($A_m,ROI$). This indicates that mitochondrial fragmentation and removal occurred in the stressed cells. In contrast, 3D mitochondrial shape analysis revealed a morphological change towards more spherical organelles ($SF$) without alterations in volume of individual mitochondria ($V_m$) and total mitochondrial biomass ($V_m,ROI$). This suggests that mitochondria are swollen but not fragmented in the stressed cell, supported by the increase in mitochondrial branch volume ($V_{BR}$).

The decrease in mitochondrial number ($N_{ROI}$) suggested by the 2D analysis, in contrast to 3D volume analysis, was most likely due to axial branch/object crossing between individual optical z-sections leading to artifactual object merging in the 2D MIC projection (Fig. 7A). This phenomenon will predominantly affect elongated filamentous mitochondria when the 2D projection (i.e. MIC) is created from the z-stack, thereby leading to an erroneous apparent reduction in $N_{ROI}$. Another reason why $A_m$ (2D), but not $V_m$ (3D), was affected, may relate to the fact that the stressed cell was “rounding” up (i.e. became “thicker”). The latter will alter the...
axial mitochondrial distribution, and thereby increase the merging/shielding of organelles in the collapsed 2D MIC image. Our observation that $V_{\text{BRG}}$ and $V_{\text{BRG,ROI}}$ were differently affected is likely explained by the fact that fewer mitochondrial branches were detected and measured in the stressed cell, which reduces total branch volume ($V_{\text{BRG,ROI}}$) but not necessarily branch mean value ($\rho_{\text{BRG}}$). The same reason is valid for explaining the reduction in total branch length ($L_{\text{BRG,ROI}}$), but not the branch mean value ($L_{\rho_{\text{BRG}}}$).

By comparing two characteristic mitochondrial phenotypes (i.e., filamentous vs. non-filamentous mitochondria) we were able to judge in detail the implications of the different processing steps for the mitochondrial quantification. Of note, the effects of ROT on mitochondrial morphology seem to depend on cell type, ROT and 3D analysis led to contradictory conclusions regarding mitochondrial fragmentation. The results confirmed that 3D analysis is the preferred method in studies of mitochondria in non-flat adhering cells. Integrative analysis of object shape and network properties was found to provide new insight into important aspects of mitochondrial dynamics. This strategy may potentially be adapted to other biological contexts and imaging modalities in order to gain new knowledge about mitochondrial (patho)physiology.

Summary and conclusions

This study demonstrates that both 2D and 3D analyses can be employed to discriminate and characterize changes in mitochondrial shape and network properties. In this sense, both types of analysis supported a change from a filamentous to a non-filamentous mitochondrial morphology in normal vs. stressed HUVECs, in agreement with visual observations. However, 2D and 3D analysis led to contradictory conclusions regarding mitochondrial fragmentation. The results confirmed that 3D analysis is the preferred method in studies of mitochondria in non-flat adhering cells. Integrative analysis of object shape and network properties was found to provide new insight into important aspects of mitochondrial dynamics. This strategy may potentially be adapted to other biological contexts and imaging modalities in order to gain new knowledge about mitochondrial (patho)physiology.

References


Supporting Information

Video S1 3D volume model of endothelial mitochondria. The video shows a 3D volume representation of mitochondrial fluorescence in the z-stack analyzed in Figure 2, 3 and 4, which was acquired from a mitoGFP expressing HUVEC by confocal microscopy. The z-stack was processed by 3D blind deconvolution and a contrast stretch (as described in the article).

(WMV)

Video S2 3D surface (shape) model of endothelial mitochondria. The video shows a 3D model of the mitochondrial surface in the same z-stack as Video S1 (i.e. a mitoGFP expressing HUVEC). An intensity threshold value (surface value) was applied to assign the surface.

(WMV)

Video S3 3D network model of endothelial mitochondria. The video shows a 3D model of the mitochondrial network in the same z-stack as Video S1 (i.e. a mitoGFP expressing HUVEC). The mitochondrial filaments were skeletonized and vectorized, and mitochondrial branches (green branches), branch- ing points (purple dots, 3 branches; red dots, 4 branches) and endpoints (green dots) were identified.

(WMV)

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Author Contributions

Conceived and designed the experiments: WJKH KJT. Performed the experiments: JN LIHN IKNP. Analyzed the data: KJT JN LIHN.

Contributed reagents/materials/analysis tools: KJT WJKH JBL PHGMW. Wrote the paper: JN LIHN IKNP PHGMW JBL WJKH KJT.


