Neocortical neuronal activity is characterized by complex spatiotemporal dynamics. Although slow oscillations have been shown to travel over space in terms of consistent phase advances, it is unknown how this phenomenon relates to neuronal activity in other frequency bands. We here present electrocorticographic data from three male and one female human subject and demonstrate that gamma power is phase locked to traveling alpha waves. Given that alpha activity has been proposed to coordinate neuronal processing reflected in the gamma band, we suggest that alpha waves are involved in coordinating neuronal processing in both space and time.

Introduction

Cortical traveling waves have been investigated by intracranial recordings in several species, including turtle, rabbit, cat, dog, and monkey (for review, see Ermentrout and Kleinfeld, 2001; Sato et al., 2012). Traveling waves have also been observed in the scalp EEG, although there is some debate as to whether it reflects the propagation of cortical activity or if it can be explained by volume conduction of the activity from a few neuronal sources (Hughes, 1995; Nunez et al., 2001; Alexander et al., 2013). Recent work has demonstrated cross-frequency interactions in which the amplitude of gamma band activity is coupled to the phase of alpha activity (Osipova et al., 2008; Voytek et al., 2010; Spaak et al., 2012). Here, we investigated whether gamma activity is also linked to the phase of alpha oscillations traveling over cortex. If so, this would create a scenario in which bursts of gamma are propagating with the phase of the alpha wave. Electrocorticography (ECoG) allows us to measure neocortical activity with high temporal and spatial resolution. The relatively high signal-to-noise ratio obtained with ECoG makes it possible to reliably detect alpha and gamma activity and to investigate their spatiotemporal interactions (Freeman et al., 2000; Osipova et al., 2008; Gunduz et al., 2011).

Materials and Methods

Experimental procedures. ECoG data collected from seven participants was used. The experimental design was resting state with either closed or open eyes. There were two groups of participants of either sex. Group 1 included participant numbers 1, 2, 3, 5, and 6, who had their eyes closed during the experiment. Group 2 included participant numbers 4 and 7, who were fixating on a blue “O” in the center of the screen that was located 100 cm ahead. The length of the experiment was between 3 and 12 min. The sampling rate of the recording of data for Group 1 was 1000 Hz and for Group 2 was 512 Hz. Data for Group 1 were collected in New York and data for Group 2 were collected in Utrecht, The Netherlands. The local Ethics Committee approved all relevant aspects of the experimental procedure. All datasets were provided completely anonymously. Data analyses were performed using MATLAB R2009 (MathWorks), either with custom-written scripts or with the Field-Trip toolbox (Oostenveld et al., 2011).

Offline data preprocessing and calculation of the spectra. To remove line noise, a notch filter was used with a band-stop frequency of 58–62 Hz for data from Group 1 and 48–52 Hz for data from Group 2. Next, a common average referencing filter was applied in which all measurement electrodes except the noisy ones were included. Electrodes above the neocortical areas that were considered epileptic and later resected were excluded from further analysis. Furthermore, noisy electrodes were the ones that showed a difference between the maximum and minimum raw voltage over all trials above a subjective threshold.

Frequency analysis was required for computing phase-locking values and phase-amplitude coupling. To estimate instantaneous phase and amplitude, we band-pass filtered the data. We used the magnitude and angle of the Hilbert-transformed band-pass-filtered data as our amplitude and phase estimates, respectively. We applied linear phase, finite impulse response filters. The filter orders were frequency dependent (order = number of cycles × sampling frequency/frequency of interest) as well as the pass-band, which was [f1 – f/4, f + f/4] for the phase estimation and [f1 – f/8, f + f/8] for the amplitude estimation, where f is the frequency of interest. This resulted in a filter
kernel that linearly decreased in length with frequency. When estimating the phase of the slower oscillations, we used three cycles; when estimating the amplitude of the faster oscillations, we used six cycles. These filter settings were used for calculating phase-amplitude couplings and phase-locking values. Bartlett’s method was used to calculate the power spectrum of 2–20 Hz (Bartlett, 1948). For each frequency band, in each window of data, 5 cycles were used, and the centers of windows were located 2.5 s apart. We chose to adapt the time window with frequency because the spectral smoothing increases with increasing frequency as for the filters used for the phase-amplitude coupling. However, the results were similar when Welch’s method was used. For each subject, the spectrum was first log transformed and then averaged over all windows and non-noisy electrodes.

Phase-locking value. To estimate the phase-locking values (PLVs), the average difference between the phases of different electrodes over the course of the experiment was calculated (Lachaux et al., 1999). The PLV quantifies the consistency in phase difference between two electrodes over trials.

Phase-amplitude coupling. For each subject, we calculated the coupling of the power of different frequency bands of each electrode and the phase of the same electrode. To calculate the phase-amplitude coupling, for each phase and power frequency, the distance between the power distribution for each phase and the uniform distribution was calculated as the phase-amplitude coupling index (Tort et al., 2010). To correct the phase-amplitude coupling for noise, we divided the time length of the experiment into two equal parts. Then, we swapped the power of the first and the second parts and estimated the coupling with the original phase distributions. After that, we subtracted the coupling values obtained after swapping from the original coupling values. We then set all the negative values to zero. Subject-specific alpha and gamma central frequencies were selected based on the peak in the phase-amplitude coupling of the most posterior ventral electrode in each subject.

Spatial traveling waves. Traveling waves are observed with respect to a reference location. To identify the reference locations, we performed the following analysis: for a putative reference location, motifs of traveling waves were identified. A motif consisted of four or more consecutive electrodes (horizontal or vertical gridwise directions) in which there was a systematic phase advance (or decay) of <90 degrees between neighboring electrodes. Further, only electrodes with a PLV >0.1 with respect to the putative reference location were considered. We then counted the number of motifs that a given electrode participated in with respect to all reference locations. The resulting counts are shown in Figure 3.

To identify the optimal reference location, we considered the PLV between a putative location and the motif with the highest count (summed over members in a motif). The chosen reference location was the one in which the PLV was the highest for the dominating motif (for each motif, we considered the PLV values of the 4–5 members; the lowest of these was considered the characterizing PLV value of that motif). Further, this PLV was used as the threshold for the significance test.

To assess the robustness of the traveling waves statistically, we performed a permutation test. The null hypothesis was that the phase advance (decay) of the identified traveling wave occurred by random. For example, when testing a motif of five electrodes, we first identified the electrodes exceeding the PLV threshold (see previous paragraph). Then, we permuted the phase values for these locations and counted how many times the systematic phase advance (or decay) occurred for a group of at least five consecutive electrodes. The number of occurrence divided by the permutations (N = 1000) constituted the p-value.
To plot the traveling pattern, the raw time series of the reference location were filtered in the band of 8–12 Hz using a Butterworth infinite impulse response filter of the fourth order. Then, the peaks of the band-pass-filtered reference location were detected. For the selected electrodes, the average of either the raw time series or the gamma power of windows of 300 ms around the alpha peaks of the reference location was calculated. The gamma power was calculated using a window of 100 ms centered at each time point with a 5 ms time step. The average velocity of travel was calculated by dividing the difference of the peak location of first and the last oscillators by the physical distance between them.

Results

ECoG datasets were analyzed from seven participants during the resting state. Four of the subjects showed a peak in the alpha band in the power spectrum and we exclusively focus the analysis on these subjects. Three of the subjects had their eyes closed and one (Subject 3) was fixating on a blue “O” on a screen located ~100 cm ahead.

Gamma power is phase locked to alpha oscillations

The power spectra averaged over all trials and electrodes of the four participants are shown in Figure 1. Note the prominent peaks in the alpha band ranging from 8 to 10 Hz. On average, 330 s of data was used per subject.

To characterize the coupling between the alpha band activity and activity in the other frequency bands, we calculated the modulation index for phase-amplitude coupling (PAC) as developed by Tort et al. (2010). This measure quantifies the distribution of power in a given band with respect to the phase of activity in a lower-frequency band. A highly nonuniform power distribution suggests phase-amplitude coupling. This PAC measure was calculated for each electrode. Figure 2 shows that there is a strong coupling between alpha phase and gamma power in the most posterior-ventral electrode in all subjects. As can be seen in Figure 2, subject-specific dominant alpha frequencies were 8, 11, 10, and 11 Hz and subject-specific dominant gamma modulation frequencies were 105, 100, 110, and 100 Hz, for Subjects 1–4, respectively.

Alpha waves travel over neocortex

Traveling waves were quantified with respect to a reference location. By changing the reference location, different traveling wave patterns can be observed. Figure 3, left, shows the number of times that each group of electrodes (a motif) showed the traveling wave pattern when changing the location of the reference. Results indicate that traveling wave patterns were relatively independent of the reference location.

For each participant, the reference location was chosen to be the one with the highest coupling with the motif with the highest counts (white disc). From the PLVs, we then derived the difference in alpha phase with respect to the reference location (phase difference indicated by color in Fig. 3, right). The maximum PLVs were 0.72, 0.71, 0.58, and 0.55 for Subjects 1–4, respectively. Different traveling directions were observed for different participants.

Gamma bursts propagate with the alpha waves

For the arrays of electrodes identified in Figure 3, we investigated the traveling wave phenomenon in more detail. Figure 4 shows at least 1500 averaged raw traces for either five or six consecutive electrodes. Before averaging, each trace was phase aligned according to the alpha band activity in the reference location (i.e., “peak aligned”) and then mean corrected. To detect the peaks, the signal from the reference location was band-pass filtered in the subject-specific alpha band. The average traces were normalized such that the amplitude per electrode was one. The plots show systematic changes in alpha phase over electrodes reflecting
a traveling wave. The average velocities of traveling waves were 0.73, 1.6, 2.05, and 1.85 m/s for Subjects 1–4, respectively.

For the phase-aligned raw traces, we also calculated the gamma band power over time using a 100 ms sliding time window. The average traces were mean corrected and normalized. The analysis revealed that the gamma power was phase aligned according to the local phase of the alpha oscillations. This illustrates that the gamma bursts systematically travel with the phase of the propagating alpha wave. To further quantify this observation, we calculated the phase difference between the signal from the reference location and the other electrodes. This was done for the individual peak alpha frequencies for at least 1500 traces. The distribution of phase differences for Subject 1 is shown in the rose plots in Figure 4, blue. Next, we quantified the phase difference between the alpha band activity in the reference location and the temporal evolution of gamma power in the other electrodes (Fig. 4, rose plots, green). To better visualize the distribution of gamma power with respect to alpha phase, we subtracted the minimum gamma amplitude of the phase distribution from all of the values in the phase distribution. Note that the gamma band power is in antiphase with the alpha activity. This analysis confirmed the occurrence of the gamma bursts at the troughs of the traveling alpha band activity.

**Discussion**

Based on data from four participants with implanted ECoG grids covering posterior neocortical regions, we demonstrate cases of gamma bursts propagating over neocortex with a velocity of 0.7–2.1 m/s. The gamma bursts were phase locked to traveling alpha waves and occurred at the troughs of the local alpha oscillations.

We propose that traveling alpha waves coordinate neuronal processing in time and space as reflected in gamma band activity. This proposal is based on several recent observations. First, numerous studies have now established that the phase of theta and alpha oscillations is locked to gamma band activity. This was first demonstrated in rat recordings (Bragin et al., 1995) and has more recently been demonstrated in monkey and human data (Lakatos et al., 2005; Canolty et al., 2006; Osipova et al., 2008; Sauseng et al., 2009; Canolty and Knight, 2010; Voytek et al., 2010; Spaak et al., 2012). Whereas gamma band activity has been associated with neuronal processing (Fries et al., 2007; Jensen et al., 2007; Siegel et al., 2012), alpha band activity is typically associated with top-down control (Klimesch et al., 2007b; Foxe and Snyder, 2011; Jensen et al., 2012). The coordination of gamma band activity by traveling alpha waves could play an important computational role. It should be emphasized that alpha band activity typically reflects pulses of inhibition. Therefore, traveling alpha waves in the visual system might serve to leave parts of the visual field unresponsive by preventing gamma band synchronization, and the traveling waves will create sweeps scanning the visual field (Ermentrout and Kleinfeld, 2001). This mechanism is consistent with the searchlight hypothesis (Crick, 1984). Traveling waves might also be involved in more intricate coding schemes. In rats, there is strong evidence that phase-specific firing at the theta cycle carries different information (O’Keefe and Recce, 1993; Lisman and Jensen, 2013). Likewise, alpha oscillations in the visual system have been proposed to coordinate a phase code. It is possible that the traveling waves could serve to tag visual features to different phases of the oscillations (Ermentrout and Kleinfeld, 2001). According to this scheme, simultaneously activated retinotopic visual representations would be organized in a temporal code coordinated by propagating alpha waves. Further experimental work linking perception and single unit firing to traveling waves is required to test these hypotheses.
It has been shown that the traveling waves are absent in the presence of certain experimental paradigms (Ermentrout and Kleinfeld, 2001). Specifically in the visual cortex, traveling waves are mostly engaged when visual stimuli are weak or absent (Sato et al., 2012). In this report, we had three subjects with eyes closed and one with eyes open. We did not observe any systematic difference between the two groups. Indeed, all of them showed the same consistent pattern of traveling waves, as can be seen in Figure 4.

Several mechanisms could account for the propagation of the gamma bursts coordinated by the alpha waves. One possibility is that a given cortical region serves as an alpha rhythm pacemaker. At a certain phase, the network is sufficiently disinhibited and a gamma burst will occur. The gamma burst will then propagate through excitatory connections (Sato et al., 2012). A second mechanism would rely on coupled alpha oscillators extending over neocortex. Through synaptic interactions, these oscillations could self-organize into traveling waves, allowing for propagating gamma bursts (Ermentrout and Kleinfeld, 2001). Finally, traveling waves might be coordinated by thalamic generators (Llinás et al., 1998). The pulvinar is known to generate alpha activity that is phase locked to neocortical areas (Lopes da Silva, 1991; Saalmann and Kastner, 2011; Saalmann et al., 2012). Multielectrode recordings in neocortex and thalamus paired with selective regional ablation of neuronal activity would be required to distinguish between these mechanisms.

One might be concerned that traveling waves are a consequence of volume conduction. Two alpha generators at different locations oscillating at different phases could by volume conduction produce traveling wave phenomena in an array of recording electrodes. Although this might be the case for scalp EEG recordings (Nunez and Srinivasan, 2006), it is not likely to explain traveling waves in the ECoG recordings. Cooper et al. (1965) have shown that electrodes in neuronal tissue a few millimeters away from a stimulation electrode usually show no sign of after discharges. Furthermore, recordings from rabbits showed distinct local differences in phase and shape of neuronal potentials in electrodes 1 mm apart (Petsche and Rappelsberger, 1970). The propagating gamma bursts confirm that volume conduction cannot explain the reported findings. The gamma bursts observed at the different electrodes occur at different instances in time. They can therefore only be explained by activations of different local populations.

The velocity of travel that we observed was between 0.7 and 2.1 m/s. The literature is not clear on traveling speed of oscillatory populations. This velocity should however be interpreted with caution due to the undersampling might result in aliasing artifacts in the spatial domain (Shaw and Roth, 1955; Pocock, 1980). As for the wagon wheel illusion in the temporal domain, both velocity and direction could be misestimated. Indeed, the direction of travel was not consistent over subjects. It is at this stage not clear whether the different travel directions can be explained by spatial undersampling or if it indeed differed over subjects. Furthermore, the placement of the electrode grids was different over subjects, complicating the interpretation. Different travel directions have also been observed in other studies (Rémond et al., 1969; Nunez et al., 2001). Future investigations in relation to task parameters are required to uncover the functional role of travel speed or direction. Importantly, it has been demonstrated in EEG recordings that the direction of traveling alpha waves is informative about cognitive performance (Klimesch et al., 2007a; Fellinger et al., 2012; Patten et al., 2012).

In short, we have demonstrated here that bursts of gamma activity propagate over neocortex and the propagating gamma bursts are locked to the phase of traveling alpha waves. Our findings suggest that not only do alpha oscillations serve to coordinate the gamma activity in time, but also in space. In future work to uncover the functional role of this phenomenon would be of great interest.

References
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